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## Research



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# Biomechanical demands of percussive techniques in the context of early stone toolmaking

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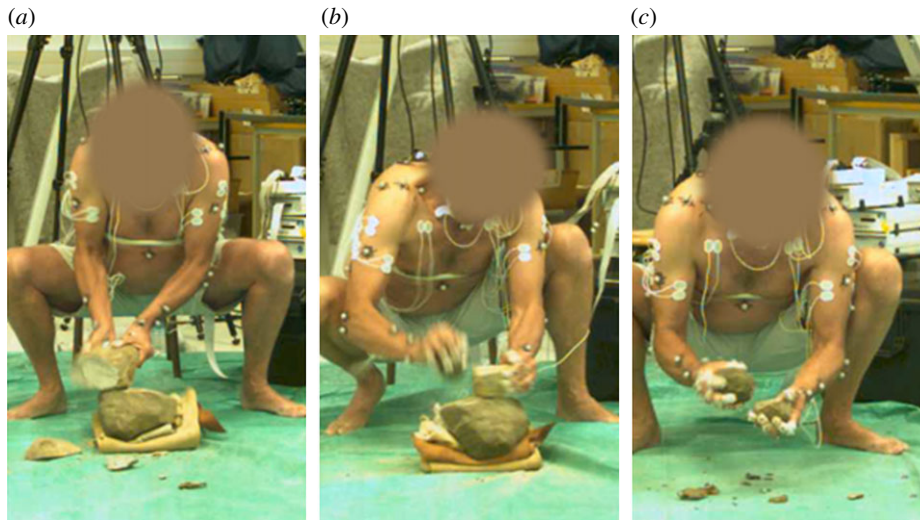
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Recent discoveries in archaeology and palaeoanthropology highlight that stone tool knapping could have emerged first within the genera *Australopithecus* or *Kenyanthropus* rather than *Homo*. To explore the implications of this hypothesis determining the physical demands and motor control needed for performing the percussive movements during the oldest stone toolmaking technology (i.e. Lomekwian) would help. We analysed the joint angle patterns and muscle activity of a knapping expert using three stone tool replication techniques: unipolar flaking on the passive hammer (PH), bipolar (BP) flaking on the anvil, and multidirectional and multifacial flaking with free hand (FH). PH presents high levels of activity for *Biceps brachii* and wrist extensors and flexors. By contrast, BP and FH are characterized by high solicitation of forearm pronation. The synergy analyses depict a high muscular and kinematic coordination. Whereas the muscle pattern is very close between the techniques, the kinematic pattern is more variable, especially for PH. FH displays better muscle coordination and conversely lesser joint angle coordination. These observations suggest that the transition from anvil and hammer to freehand knapping techniques in early hominins would have been made possible by the acquisition of a behavioural repertoire producing an evolutionary advantage that gradually would have been beneficial for stone tool production.

## 1. Introduction

Stone toolmaking is considered a hallmark of humankind and its acquisition represents a major evolutionary advance in hominin evolution. Recent contributions in archaeology, palaeoanthropology and evolutionary biomechanics proposed that the earliest known representatives of the genus *Homo* (2.8 million years ago (Ma), Ledi Geraru, Ethiopia [1]) may not have been the first hominin stone toolmaker as originally proposed by Leakey *et al.* [2]. Indeed, early non-*Homo* hominins between 3 and 4 Ma [3–5] were presumably able to fulfil some of the functional requirements needed for stone toolmaking. Especially, it has been inferred from paleoanthropological analyses that *Australopithecus afarensis* would have been capable of many human-like manipulative capabilities, especially if hammering [3,4,6–9], while biomechanical simulations of hand functions further confirmed that this hominin was capable of human-like grips [10,11], despite local functional limitations [12], validating Marzke's (1983) inferences [7]. Concurrently, the possibility that stone tool knapping could have emerged with the genus *Australopithecus* was suggested from the Oldowan assemblage from Gona, Ethiopia [13], and the possible hammerstone percussion evidence found at Dikika (3.39 Ma, Ethiopia) [14] (but see [15]) both



**Figure 1.** Percussive techniques used for this study: (a) unipolar flaking on the passive hammer (PH), (b) bipolar flaking on the anvil (BP) and (c) multidirectional and multifacial flaking with free hand (FH).

sharing the same geochronological context as, respectively, *Au. garhi* and *Au. afarensis*. The discovery of the stone tools from Lomekwi 3 (3.3 Ma, West Turkana, Kenya) provides evidence of an early emergence of stone tool knapping activities, 500 000 years ago (ka) before the first fossil occurrence of early *Homo* [16] (but see [17]).

As opposed to the Oldowan technocomplex, the Lomekwian stone tools assemblage exhibits exceptionally larger and heavier flakes (around 0.8 kg) and cores (around 3 kg) in addition to recognizable knapping activity marks [16]. From analysis of these technological and morphological features, and stone tool replication experiments, two percussive techniques—the bipolar (BP) flaking on the anvil, and the unipolar flaking on passive hammer (PH) techniques—have been inferred to have been the most frequently used during knapping at the site (figure 1) [16,18]. In the BP technique, the core is rested on an anvil (which itself is likely laying on the ground) and held in place with the non-dominant hand, and struck along its edges with a hammerstone held by the dominant hand [19,20]. In the PH technique, the core is held with both hands and swung down and struck against an anvil (thus, the immobile anvil is acting passively as the hammerstone) [16,19]. These two percussive techniques differ from the free hand (FH) percussive technique dominant in Oldowan technology and correspond with multidirectional flaking. In the latter, the hammerstone is held by the dominant hand and the core maintained by the non-dominant hand without the help of an anvil [19,20]. Inversely, those techniques identified at Lomekwi recall the hammer-on-anvil technique used by common chimpanzees, capuchins and macaques when engaged in nut-cracking and shell crushing. Indeed, it can be performed in a unimanual (like in BP) or bimanual fashion (like in PH) [21–23]. As a result, the three archaeological techniques underline two contrasting conditions, namely ‘with anvil’ versus ‘without anvil’ and ‘unimanual’ versus ‘bimanual’. As such, they are expected to involve specific biomechanical demands including muscle and joint solicitation. The biomechanical demands of some of these knapping activities have been analysed using kinematic and electromyographic approaches. For instance, previous studies of FH percussive techniques emphasized high solicitation of wrist extension during the down-swing [24], suggesting that the flexor–extensor apparatus helps either in stabilizing the elbow joint during the strike [25] or in accelerating the

hammerstone towards the target [26,27]. Thus, the analysis of upper limb movement during stone toolmaking replications provides a means of investigating the functional demands required for making the oldest stone tools and exploring the hypothesis of *Australopithecus* or *Kenyanthropus* being a possible stone tool maker.

Human motor behaviour is highly goal-directed. This requires the central nervous system (CNS) to coordinate different aspects of motion generation to achieve the motion goals. Using the terminology introduced by Latash *et al.* [28], the CNS organizes the control of *elemental variables* to stabilize *performance variables*. Joint degrees of kinematic freedom, activation of muscles and joint torques can all be considered as elemental variables. Performance variables are directly related to the task goal: in the frame of stone tool knapping, point of percussion and angle of blow can be performance variables [29]. The concept of motor synergies (i.e. muscle or kinematic synergies) provides an approach to quantify the covariation of the elemental variables during a task. A motor synergy can be defined as a set of stable spatio-temporal patterns of activity shared across elemental variables that leads to a desirable performance variable. It has been suggested that the CNS may generate motor commands through a linear combination of motor synergies, each controlling a group of elemental variables (see [30] for a review). Such co-activation of elemental variables leads to a reduction in the dimensionality of motor control. Numerous studies have demonstrated that a range of functional tasks can be explained by motor synergies, including stone knapping [31]. Muscle synergies have also been able to discriminate between grasps of differently shaped objects in a non-human primate [32] and, more generally, they are known to be task specific and reflect the biomechanical constraints of the task [33]. To quantify motor synergies, dimensionality reduction methods are used to analyse large sets of muscle activity or joint angle changes observed over the course of motor tasks. Principal component analysis (PCA) allows quantifying complexity as how much variance of the movement can be reduced to single dimension component. Interestingly, similar multivariate methods are used to reconstruct muscle synergy groups based on muscle entheses (i.e. muscle and ligament attachment sites on bone [25] which are the only remains of the musculotendinous unit in fossils) [34–36]. In the case of

the stone knapping task, the variance accounted for by the first principal component (PC1) significantly depends on the conditions of the motor task and can be interpreted as a measure of the complexity of movement control for the CNS [37]. Based on the above-mentioned concepts, stone tool production has been interpreted as being diagnostic of the cognitive and motor skills of extinct hominins [38,39]. Bril *et al.* [40] argue that the transition from anvil and hammer percussive techniques to freehand knapping techniques in early hominins necessitated improved motor control superior to that of non-human primates. Motor skills might have been the most important, as a cognitive development without the ability for execution will not yield an evolutionary advantage [41–43]. While Bril *et al.* [38] showed that nut-cracking and stone knapping implied equivalent skills and rates of success, they also demonstrated highly significant differences. Indeed, both conditions ‘with anvil’ versus ‘without anvil’ and ‘unimanual’ versus ‘bimanual’ influence the manipulative complexity of the task [43] and underline the evolutionary role of the non-dominant (i.e. postural) hand [38].

Consequently, the aim of this study was to compare PH, BP on anvil and FH knapping techniques in terms of biomechanical and motor control demands in an evolutionary perspective. We first hypothesized (H1) that technique output would be comparable so that technique may be reduced to its fundamental striking element [44]. Biomechanical demands of the strikes were assessed through the amplitude of muscle activity and joint mobility of the upper limbs. Based on previous studies we expected, for all three techniques, a high muscle activity of *Extensor* and *Flexor carpi ulnaris*, *Triceps brachii* and *Pectoralis major* muscles [3,11,25,27]. Due to the heavier stone involved, we further hypothesized (H2) that PH technique would elicit greater muscle activity compared to the other techniques.

For all three techniques we expected a high wrist flexion–extension [27] but little joint excursion for the shoulder and elbow joints, especially for BP and FH [31]. Due to the heavier stone manipulated, we hypothesized (H3) that the PH technique involves overall smaller upper limb joint excursions.

As for a motor control point of view, based on interpretations of nut-cracking [38] we expected the PH technique to be less complex than the other two. To address this issue, we relied on data processing techniques based on PCA to detect ‘coordinative structures’, or ‘synergies’ by which the motor system organizes an action [45–47]. We, therefore, used PCA (detailed in the Data analysis and statistics sub-section) as a measure for the complexity of joint and muscle coordination patterns. More precisely, we hypothesized (H4) that the first component will account for a greater percentage of variance for the PH technique and that loading factors would be higher, both in terms of kinematics and muscle activity. This would indicate lesser motor control demands and potentially a less complex technique.

## 2. Material and methods

### 2.1. Participant

One male subject (age = 58 years; height = 1.77 m; mass = 80 kg) participated in the study after giving his written informed consent. He had no previous history of neuropathies or trauma to the upper extremities. The participant (M.B.) is a recognized expert in stone tool replication [48]. Expertise is defined here

as the knowledge of the lithic production schemes and the ability to detach flakes similar to those found in archaeological excavations. This necessitates long-time experience and long-lasting specific training [48–50].

### 2.2. Lithic material

Petrographic variation of raw materials may influence flake production processes, as documented from Pliocene and early Pleistocene sites in the region [51,52]. The raw materials for the replications were sourced directly from the conglomerate located a few hundred metres away from the LOM3 site in West Turkana (see source in Harmand *et al.* [16]) and imported to France. Two anvils (6.7 and 13 kg) and two hammerstones (0.8 and 1.2 kg) were used, consisting of basalt blocks and cobbles. Blocks ( $n = 9$ ) to be reduced were of phonolite and weighted between 0.27 and 5.7 kg.

### 2.3. Experimental design

Three flake production strategies were investigated: unipolar flaking on the PH, BP flaking on anvil and multidirectional–multifacial flaking with FH percussion (figure 1). Originally, four core reduction sessions (each involving a new core) were performed for each technique but, due to synchronization issues, only four, three and two were retained for PH, BP and FH, respectively. The three percussive techniques were randomized to avoid any habituation effect. Thirty-minute rest periods were ensured between each session/trial in order to limit the influence of fatigue. The use of a chair was banned to favour natural postures in accordance with previous observations in humans [53] and chimpanzees [21,54,55]. Despite this postural constraint, the expert had to find a unique posture and keep it throughout the replication sessions. The participant consistently adopted a crouched posture (figure 1) during all sessions, and was free to adapt his pace, reposition the anvil and handle the blocks and/or the hammerstones throughout the sessions. The instruction was to complete a series of strikes until it was no longer possible to detach flakes exceeding 1.5 cm long. Prior to the replication sessions, maximal voluntary isometric contractions (MVCs) were performed.

### 2.4. Kinematics

Joint angle analysis resulted from the following procedure: 55 reflective markers were placed on anatomical landmarks of the trunk and upper limbs. The marker set (adapted from Blache *et al.* [56–58]) is detailed in electronic supplementary material, table S1. The three-dimensional location of the markers was recorded using a 16-camera optoelectronic system (16 MPixels Oqus camera, Qualisys Inc., Sweden). The sample frequency was set to 300 Hz. A least-square optimization-based inverse kinematic algorithm that minimized the distance between theoretical and experimental marker locations was used to compute joint angles with the OpenSim software [59]. The kinematic model originated from Rajagopal [60] and was scaled to the expert’s anthropometry before the calculation of the following joint angles: shoulder, elbow–forearm and wrist flexion/extension (labelled *shoulder\_flex*, *wrist\_flex* and *elbow\_flex*, respectively); shoulder and wrist adduction/abduction angle (labelled *shoulder\_add*, *wrist\_add*, respectively); shoulder medial/lateral rotation (labelled *shoulder\_rot*); and forearm pronation/supination (labelled *forearm\_pron*). Suffix ‘\_d’ or ‘\_nd’ is added to each abbreviation to discriminate between the dominant versus non-dominant limb, respectively (e.g. *shoulder\_flex\_nd*). Negative angles denote extension, abduction, external rotation and supination.



## 2.5. Electromyography

To keep skin impedance low, the site for electrode placement was prepared by shaving, gently abrading the skin using sandpaper and cleaning with 70% isopropyl alcohol. Fourteen surface bipolar electrodes (Ag/AgCl, diameter 8 mm) were placed over the bellies of seven muscles from both upper limbs and aligned parallel to muscle fibres in accordance with Seniam's recommendations [61]. The electromyographic signal (EMG) of the following muscles was recorded: *Pectoralis major*, *Deltoideus*, *Extensor carpi ulnaris*, *Flexor carpi ulnaris*, *Triceps brachii*, *Biceps brachii*, *Infraspinatus*. Again, the suffix '\_d' or '\_nd' is added to discriminate between dominant versus non-dominant limb, respectively. The EMG signal was recorded using a BrainAmpExG MR system (BrainAmp, Brain-Products, Munich) with a sample frequency of 1000 Hz and synchronized to the motion capture system using an external trigger.

## 2.6. Data processing

Data processing was conducted using custom Matlab (Mathworks Inc., Novi, USA) routines. Kinematic data were low-pass (20 Hz) filtered with a second-order Butterworth filter. EMG data were band-pass (20–500 Hz) filtered with a fourth-order Butterworth filter, rectified to the absolute, and EMG envelopes were obtained using a low-pass 5 Hz filter [25]. The maximum EMG value of each muscle obtained during the MVCs was used to normalize the EMG recordings (% MVC). Each trial/session was divided into cycles identified from the vertical displacement of the marker located on the third metacarpal bone (electronic supplementary material, figure S1). Each cycle was intended to detach one flake; there was no preparation of the block toward an ultimate goal that involves a series of cycles related to each other. Therefore, every cycle was accounted for and treated independently. Each cycle was divided into three phases: (i) the analysis phase during which the participant briefly observed and manipulated the block, (ii) the up-swing phase during which he raised his arm and (iii) the down-swing phase during which he executed the strike until the impact of the hammerstone. Technique output (defined here as the percentage of flakes greater than 1.5 cm out of the total number of strikes) was compared.

Physical demands were assessed by using three criteria: (i) joint excursion, (ii) maximal and (iii) overall muscle solicitations. Joint excursions (for all degrees of freedom) were recorded and compared with published normative data [62]. Maximal muscle solicitation was the peak value of %MVC and overall muscle solicitation was evaluated using the averaged integrated EMG (iEMG) envelope using the following formula:

$$iEMG(x) = \frac{1}{n} \sum_{i=1}^n \int_{t_i}^{t_f} EMG(t) dt, \quad (2.1)$$

with  $x$  the muscle considered,  $t_i$  and  $t_f$  the initial and final time of a cycle,  $EMG(t)$  the EMG envelope value at the specific time  $t$ , and  $n$  the number of cycles.

Motor control demands were assessed by using a PCA detailed below. Beforehand, the swing repeatability of standardized cycles was checked using the Sprague and Geers method [63] to ensure representativeness of the mean and for further comparison (electronic supplementary material, table S2).

## 2.7. Data analysis and statistics

The targeted sample size was a minimum of 100 percussive gestures per technique, irrespective of the nature of removals [24]. Given the synchronization issues between motion capture and EMG recordings, some cycles could not be identified for the analysis of muscle activity. Therefore, the analysis of kinematics relies on 138, 120 and 76 strikes for PH, BP and FH, respectively; the analysis of muscle activity was performed on 167, 189 and 89 strikes for PH, BP and FH.

All data are presented as the mean  $\pm$  standard deviation. One-tailed independent  $t$ -tests were performed to determine the statistical significance of technique output and task economy differences between the three techniques' conditions. The effect size was computed using Cohen's  $d$ . The following magnitude scale was used for interpretation [64]: less than 0.2, trivial; 0.2–0.5, small; 0.5–0.8, moderate; greater than or equal to 0.8, large. Statistical significance of averaged iEMG data was tested using an independent two-way ANOVA (with technique and muscle as between-cycles factors).

Statistical parametric mapping (SPM) was used to analyse kinematic and EMG envelopes [65]. SPM analysis was used to identify significant differences between techniques over time. This analysis sets a critical threshold following a random process and computes the  $t$  statistic value for each time [66]. When the  $t$  value exceeds the threshold, the difference between the two curves is significant. For each technique, one PCA was performed on each cycle to analyse the level of kinematics and muscle intra-cycle variation. Time (normalized) was set in rows and joint angles/muscle activations were set in columns. The first principal component (PC1) is a measure of task complexity; the smaller the PC1 value, the more complex the task and vice versa [37]. PCAs were based on the covariance matrix in order to keep angles non-normalized [31]. Statistical significance of the variance of the components was tested using one-way independent measure ANOVA. In addition, the contribution of each muscle and each degree of freedom to PC1 was identified by the loading factors that represent the underlying synergy pattern. The standard deviation of the loading factors informs the inter-cycle variation of the movement. For all ANOVAs, when a significant effect was found, Tukey *post hoc* tests were performed to further identify the origin of statistical differences between conditions. All statistical analyses were conducted using JASP (v.0.10.2) and Matlab (Mathworks Inc., Novi, USA), including the Matlab Toolbox for Dimensionality Reduction [67]. For all statistical tests, significance was set to  $p < 0.05$ .

Before each statistical analysis, the cycles were visually inspected and obvious outliers (manifestly linked to a measurement artefact) dismissed. Considering the high number of observations (greater than 30), the normality distribution was not assessed [68,69] based on the high robustness of the ANOVA against the non-normality of residuals [70,71]. In addition, a Levene test was used to test the homogeneity of the variances. When not met, a permutation ANOVA (lmPerm package for R, the R Core Team, 2020) was performed [72].

## 3. Results

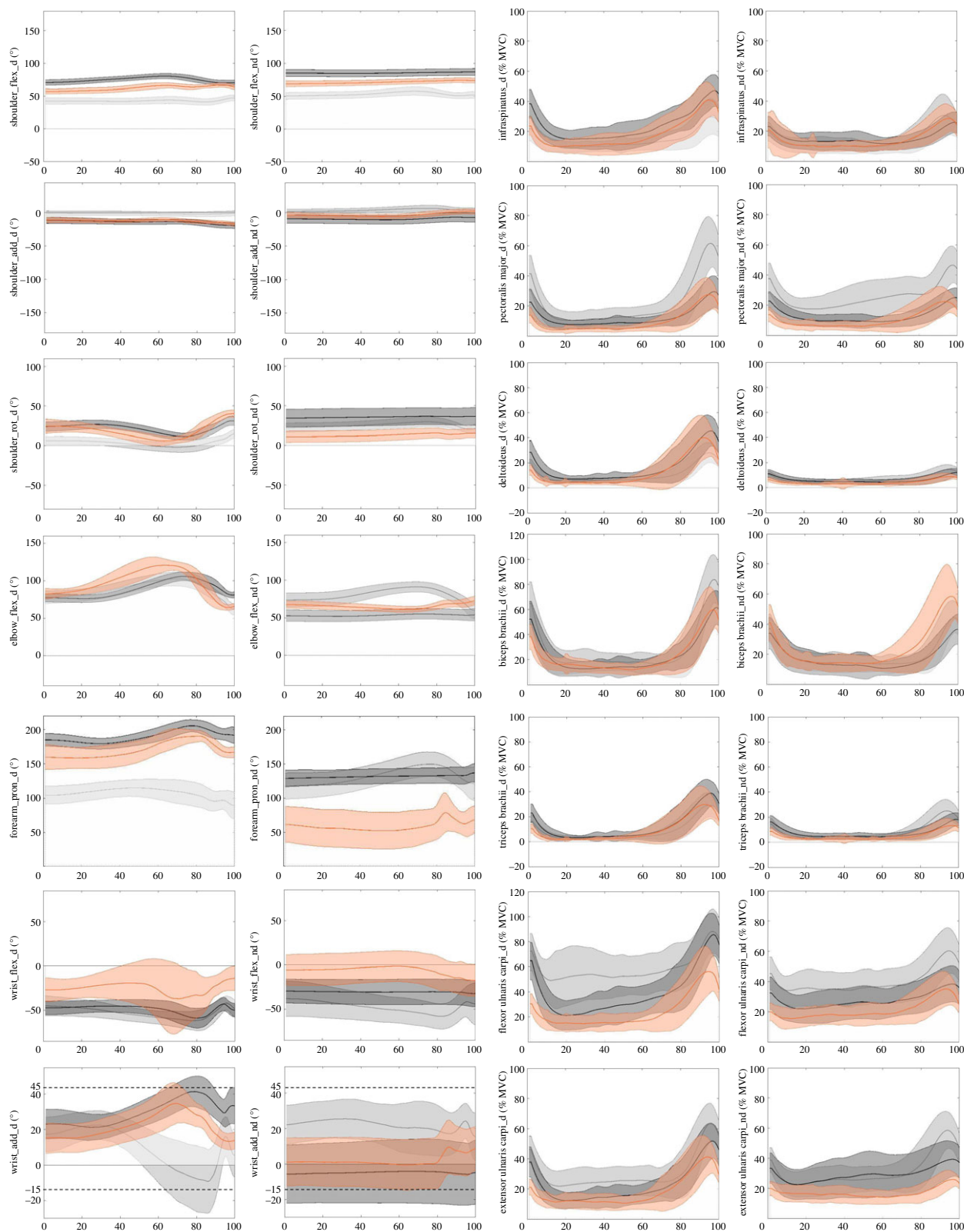
### 3.1. Technique output

No significant difference was found between the output of each technique: the percentage was 25.60% for PH (43 flakes out of 168 strikes), 22.30% for BP (66 flakes out of 296 strikes) and 25.8% for FH (43 flakes out of 171 strikes). More precisely between PH and BP:  $|Z| = 0.8053 < 1.9600$ ,  $p > 0.42$ ; between PH and FH:  $|Z| = 0.0950 < 1.9600$ ,  $p > 0.92$ ; and between BP and FH:  $|Z| = 0.7012 < 1.9600$ ,  $p > 0.48$ .

### 3.2. Physical demands

#### 3.2.1. Joint excursion

There was a significant effect of the technique on the time course of all joint angles and during most of the time (see SPM statistical test results in electronic supplementary material, figure S2). From a general view, the PH technique especially solicited wrist abduction (dominant limb) close to



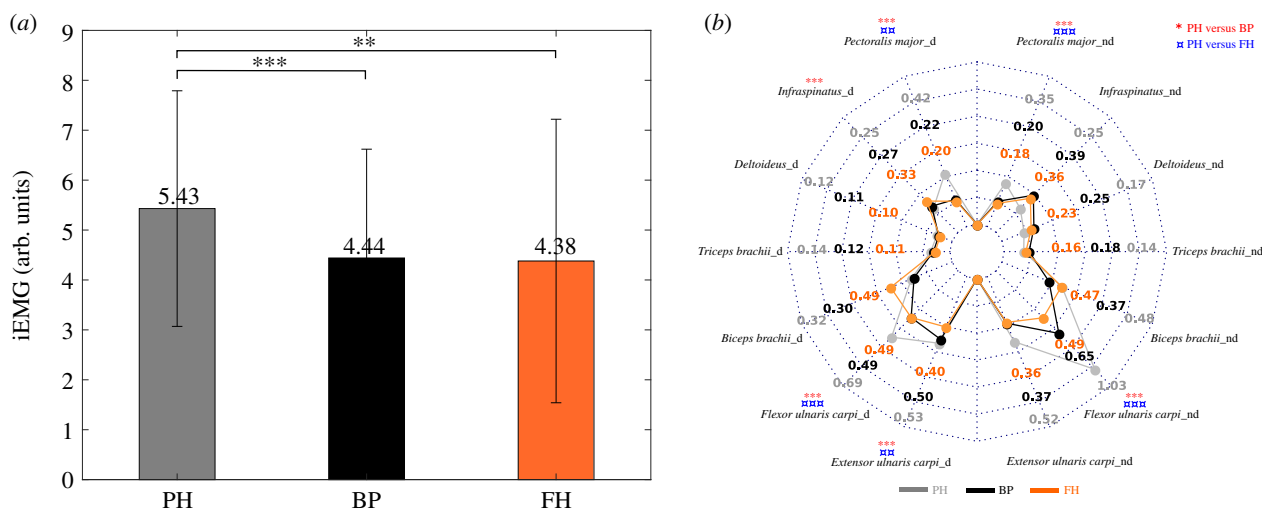
**Figure 2.** Time courses of joint angles (left) and EMG (right) averaged (with standard deviation) over swing phases and sessions for the three techniques, PH (grey), BP (black) and FH (orange). Joint angle limits according to Kapandji [62].

its theoretical maximal joint range of motion [62]. BP and FH techniques highly solicited wrist adduction (dominant limb) and abduction (non-dominant limb), as well as forearm pronation (dominant limb) (figure 2, left).

### 3.2.2. Maximal muscle solicitation

There was a significant effect of the technique on muscle activity (see SPM statistical test results in electronic

supplementary material, figure S3). For example, the *Pectoralis major* of the dominant limb exhibited a larger activation peak during the PH technique than during the other techniques (figure 2, right). Generally, PH especially solicited *Flexor carpi ulnaris* and *Extensor carpi ulnaris* of the non-dominant limb, unlike FH and BP. Regardless of the technique, muscles of the dominant limb were generally more solicited than their non-dominant limb homologues especially for *Flexor carpi ulnaris* and *Deltoidus. Biceps brachii*



**Figure 3.** iEMG (expressed in arbitrary units), averaged over cycles and sessions for PH, BP and FH techniques. (a) Sum of all muscles of both limbs. (b) Individual muscle ( $n = 14$ ) solicitation, dominant limb (right-hand side) and non-dominant (left-hand side).

and *Flexor carpi ulnaris* were the most solicited (up to 80% of MVC at the time of impact for a few cycles) while *Infraspinatus*, *Deltoideus* and *Triceps brachii* were the least solicited, especially for the non-dominant limb. For all muscles and all techniques, peak activation was observed towards the end of the down-swing phase, around the time of impact.

### 3.2.3. Overall muscle solicitation (iEMG)

In terms of muscle solicitation (figure 3a), PH ( $5.43 \pm 2.36$ ) was significantly more demanding than BP ( $4.44 \pm 2.18$ ) with a difference of 18.3% ( $t = 4.10$ ;  $p < 0.05$ ;  $d = 0.435$ , i.e. small effect), and than FH ( $4.38 \pm 2.84$ ) with a difference of 19.4% ( $t = 2.98$ ;  $p < 0.001$ ;  $d = 0.393$ , i.e. small effect). The permutation ANOVA revealed a significant interaction effect ( $F_{26,6188} = 20.27$ ;  $p < 0.001$ ) of technique on individual muscle demand (figure 3b). *Post hoc* analyses revealed a higher demand of PH over BP and FH for the *Flexor carpi ulnaris* of both limbs (*Flexor carpi ulnaris\_d*: +28.4%;  $t = -13.90$ ;  $p < 0.001$  and +29.7%;  $t = 14.96$ ;  $p < 0.001$ , respectively), and *Flexor carpi ulnaris\_nd*: +29.6%;  $t = 6.51$ ;  $p < 0.001$  and +29.6%;  $t = 5.75$ ;  $p < 0.001$ , respectively), for the *Pectoralis major* of both limbs (*Pectoralis major\_nd*: +48.4%;  $t = 7.26$ ;  $p < 0.001$  and +52.1%;  $t = 6.31$ ;  $p < 0.001$ , respectively), and *Pectoralis major\_d*: +42%;  $t = 5.13$ ;  $p < 0.001$  and +47%;  $t = 4.70$ ;  $p < 0.01$ , respectively), and for the *Extensor carpi ulnaris* of the dominant limb (*Extensor carpi ulnaris\_d*: +28.4%;  $t = 5.41$ ;  $p < 0.001$  and +29.7%;  $t = 4.58$ ;  $p < 0.01$ ). PH was significantly less demanding than BP for the *Infraspinatus* of the dominant limb ( $-35\%$ ;  $t = 5.78$ ;  $p < 0.001$ ), but not than FH ( $t = 3.78$ ;  $p = 0.079$ ). Also, FH was significantly more demanding than PH and BP for the *Biceps brachii* of the non-dominant limb (+33.8%;  $t = 5.86$ ;  $p < 0.001$  and +38.3%;  $t = 6.02$ ;  $p < 0.01$ , respectively).

There was no major difference between the dominant and non-dominant limb as revealed by the vertical axis of symmetry displayed in figure 3b excepted for the *Flexor carpi ulnaris* for PH which was notably more solicited for the dominant limb. The *Triceps brachii* was the least solicited muscle for all three techniques while the *Flexor carpi ulnaris* was the most solicited. In addition, figure 3b illustrates a similar overall pattern between BP and FH. The main differences between these two techniques are observed for *Biceps brachii* and the wrist

flexor–extensor apparatus. By contrast, PH differed from the two other techniques by extensive *Flexor carpi ulnaris* and *Pectoralis major* demands.

### 3.3. Motor control demands

Joint and muscle coordination was evaluated through PCA as an evaluation of motor control demands.

#### 3.3.1. Percentage of variance of joint angles and muscle activity accounted for in the first principal component

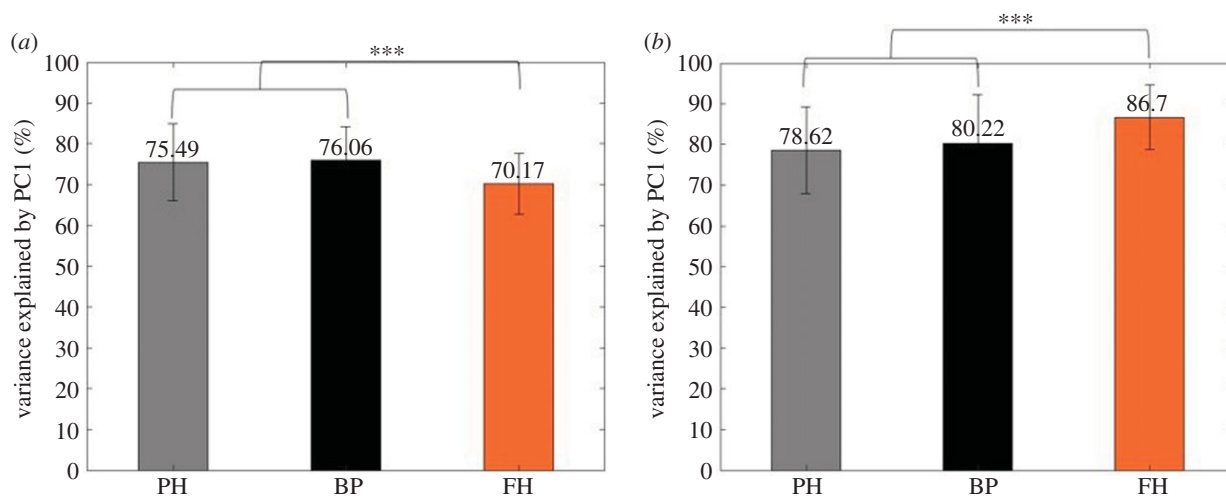
As a whole, FH can be distinguished from BP and PH for both kinematics and muscle synergy. In terms of kinematics, there was a significant effect of the technique on the percentage of variance accounted for by PC1 ( $F_{2,299} = 7.962$ ;  $p < 0.001$ ) (figure 4). *Post hoc* revealed that FH was smaller than BP ( $-7.75\%$ ;  $t = -3.860$ ;  $p < 0.001$ ;  $d = 0.743$ , i.e. moderate effect) and PH ( $-7.05\%$ ;  $t = -3.550$ ;  $p = 0.001$ ;  $d = -0.591$ , i.e. moderate effect). In terms of muscle synergy, there was also a significant effect of the technique on the percentage of variance accounted for by PC1 ( $F_{2,442} = 16.884$ ;  $p < 0.001$ ) (figure 4). *Post hoc* revealed that FH was greater than BP (+7.47%;  $t = 4.661$ ;  $p < 0.001$ ;  $d = 0.593$ , i.e. moderate effect) and PH (+9.31%;  $t = 5.693$ ;  $p < 0.001$ ;  $d = 0.827$ , i.e. large effect).

#### 3.3.2. Joint and muscle patterns

The contribution of joint degrees of freedom and muscles to the intra-cycle variance of movement was evaluated through the loading factors of each variable in PC1. In terms of kinematics, no matter the technique, the elbow joint (elbow\_flex\_d, forearm\_pron\_d) provided the highest contribution to PC1 for all the techniques. However, these seemed slightly higher for BP and FH techniques. In addition, the wrist contribution (especially in adduction for the dominant limb) was not negligible. Conversely, the shoulder joint was very little solicited, save one exception (Shoulder\_rot\_d).

In terms of muscle pattern, loading factors were more evenly distributed. Regardless of the technique, *Biceps brachii\_d* and *Flexor carpi ulnaris\_d* were the highest contributing muscles while *Deltoideus\_nd* and *Triceps brachii\_nd/d* were the smallest. Inter-technique dissimilarities are mainly illustrated by high contributions of *Biceps brachii\_nd* for FH,





**Figure 4.** Percentage of variance accounted for by PC1 for each technique (PH, BP and FH) in terms of kinematics (a) and muscle activity (b). The PCAs were performed separately for each technique on all joint angles or muscles, respectively, during the swing phases.

and *Pectoralis major\_d* and *Extensor carpi ulnaris\_nd* for PH figure 5.

## 4. Discussion

This study examined biomechanical and motor control demands associated with flake production processes to shed light into the earliest known stages of hominin technological evolution. We collected kinematics and EMG data from an expert knapper who replicated the earliest known flake production strategies using the three main percussive techniques as currently identified in the Lomekwian and the Oldowan: unipolar flaking on the PH, BP flaking on anvil and multidirectional flaking with FH. This study highlights similarities but also major differences between the three flake production techniques which are discussed below.

### 4.1. Technique output

Whereas Acheulean and other Pleistocene technologies result from a step-by-step implementation to obtain the desired end-product, Lomekwian flake production (and Oldowan to some extent) seem to result from *ex tempore* operation to obtain sharp edges from a block [44]. Therefore, it was possible to evaluate technique output as the percentage between the number of flakes produced and the number of strikes. As expected by our first hypothesis (H1), our results did not show significant differences between the three analysed percussive techniques. Given the above-mentioned definition of Oldowan and Lomekwian techniques (each strike aims at producing one flake) and the similar output (the same amount of strikes was necessary to produce one flake), each strike can be considered as representative of a technique and then directly comparable. For instance, this would not be the case if a technique would necessitate an average of three strikes to produce one flake while another one would only necessitate one strike.

### 4.2. Muscle demands

In order to assess the energetic cost associated with each strike, we evaluated muscle activity in terms of iEMG. Fourteen main contributor muscles (seven on both limbs) that are recordable

using surface electrodes were analysed and results showed that, overall, PH was approximately 20% more demanding than BP and FH. This indicates that the PH technique requires more energy to produce a flake than the other techniques. This result is in line with our second hypothesis (H2), given that the PH technique involves the manipulation of a heavier stone. Interestingly, FH is not more demanding than BP, whereas the former technique does not require an anvil but rather the non-dominant hand to stabilize the core. This result underlines the primary stabilizing role of the non-dominant hand whatever the technique [73] and emphasizes the need to investigate the non-dominant limb during stone tool production.

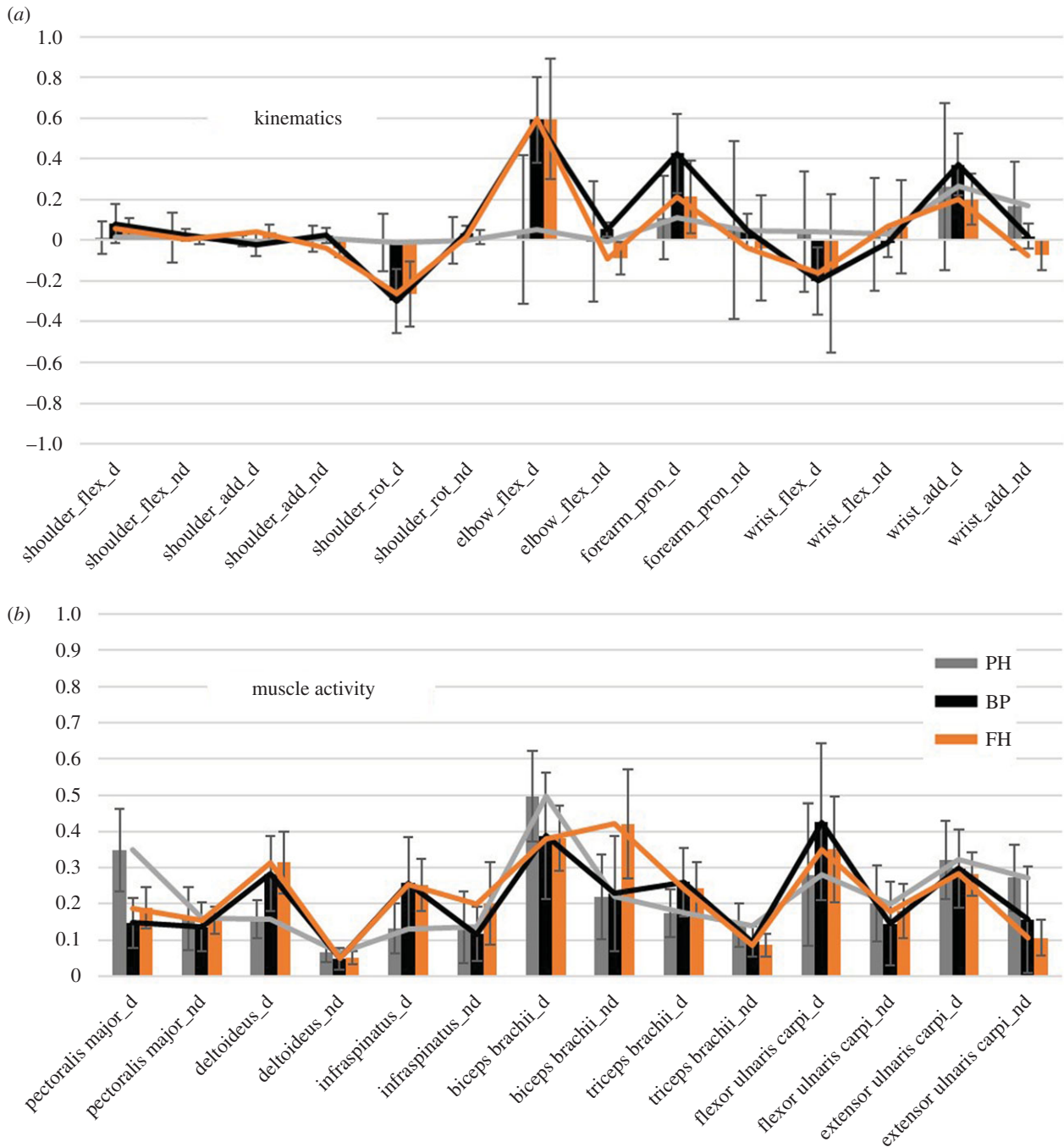
Taken together, results of technique output and economy highlight that a similar number of strikes is needed to detach a flake (one out of four), but PH still requires more muscle activity than the other two techniques. This has to be put into perspective with the energetic cost associated with locomotion though: even if significant, this discrepancy likely may not have played a critical evolutionary role [74].

A closer look at single muscles' EMG activities (figure 2) revealed that, regardless of the techniques, the most solicited muscles (relative to their maximum potential) were: the wrist flexors–extensors, as previously stressed [11,27,75], and *Biceps brachii* and *Infraspinatus*. On the contrary, *Deltoideus* and *Triceps brachii* muscle activities were smaller. In terms of inter-technique differences, PH differs from the other two techniques by higher solicitation of the *Pectoralis* and wrist flexors/extensors.

The three techniques are associated with similar overall muscle solicitation between the two upper limbs. Such a result is in line with the analysis of Key & Dunmore [73] that showed that the non-dominant limb is susceptible to experience higher solicitation (in terms of pressure) than the dominant one during Oldowan stone tool reduction. Interestingly, we registered a high solicitation of the non-dominant *Flexor carpi ulnaris* (almost double the value of the dominant side) during the PH technique. This highlights that besides the apparent symmetry of the bimanual technique, a differential role of the two limbs remains notable.

In evolutionary terms, the particular solicitation of the wrist flexors/extensors, *Biceps brachii*, and *Pectoralis major* echoes the archaic (*sensu* more 'ape-like') morphology of their entheses in the earliest hominins (i.e. *Ardipithecus*, *Australopithecus*, *Paranthropus* and Early *Homo* as *Homo habilis sensu lato* and *Homo*





**Figure 5.** Loading factors of PC1 (contribution to the intra-cycle covariance of movement) averaged over all swing phases derived from joint angle (a) and muscle activity (b) patterns for each technique.

*erectus sensu lato*) as compared to extant humans [76–78]. Interestingly, this archaic morphology, which may have been primarily promoted by arboreal behaviours, includes a rod-like pisiform, a relatively deep intertubercular groove and a distally located radial entheses [79–84]. Hence, the hypothesis that non-*Homo* hominins may have been able to co-opt their archaic morphology to make stone tools (Lomekwian and Oldowan) is reasonable. Otherwise, the differences in muscle solicitation between techniques can be explained by postural differences of the hand. The higher solicitation of the *Pectoralis* and wrist flexors/extensors typical of PH is likely due to the manipulation of large-sized stones (mean weight = 3 kg) with both hands. Both *Deltoideus* and *Triceps brachii* showed very minimal activity in the present study despite their probable functions in human-like manipulation [3,85,86]. Nevertheless, the low contribution of those muscles could be explained by the fact that the expert

mostly solicited the heads of those muscles that were not monitored by the electrodes.

### 4.3. Joint excursion

Overall, based on the joint limits reported by Kapandji [62], the visualization of kinematic curves (figure 2) showed neither substantial excursion nor extreme positions at the shoulder joint during our stone tool production experiments. In other words, for all the techniques, achieving the speed of the endpoint effector (i.e. the hand) necessary to detach a flake did not require a great range of motion of the shoulder. From an evolutionary perspective, this tends to indicate that mobility of the shoulder joint complex would have played little role in the evolution of percussive techniques.

The greater joint excursion was observed for the elbow/forearm and wrist joints that reached or even exceeded their theoretical joint boundaries provided by Kapandji [62]. This result concerned wrist abduction/adduction and forearm pronation. Exceeding theoretical joint boundaries has to be put into perspective, as those limits are indicative and not specific to the participant. Still, BP and FH necessitated a greater amount of forearm pronation than PH. Therefore, it could be hypothesized that limited pronation capabilities would prevent using BP and FH techniques while 'individuals' with such a limitation would easier use the PH technique. Thus, regarding the overall small joint excursions of PH our third hypothesis was validated.

Great changes in wrist flexion/extension and adduction/abduction were observed during the down-swing, indicating a large joint angular velocity that serves in accelerating the core as previously observed [27]. As expected, the non-dominant limb exhibited larger joint excursions for PH than for BP and FH, the latter two in which the limb mainly remains immobile to maintain the core. Nonetheless, joint excursions were not symmetrical, even if, *a priori*, the movement may resemble a simple bimanual task. For example, wrist adduction was more solicited for the dominant limb than for the non-dominant limb and conversely for forearm pronation. The relatively high standard deviation observed for the forearm and wrist joint would underline their importance in the modulation of the movement. This question was addressed thoroughly through the analysis of the motor control demands associated with each technique.

#### 4.4. Motor control demands

Stone tool production has been linked to cognitive and motor skill evolution, in particular the idea that the transition from anvil and hammer percussive techniques to freehand knapping techniques in early hominins would have necessitated improved motor control superior to that of non-human primates [87]. We compared techniques' complexity in terms of control strategies involved in the processes, at the level of both kinematic and muscle activity patterns. More specifically, we used PCA to report variance accounted for by PC1 as it significantly depends on the conditions of the motor task and therefore can be interpreted as a measure of the complexity of movement control for the CNS [37].

Overall, our PCA revealed that a high percentage of variance (70–85%) was explained by PC1, for both kinematics and muscle activity. This indicates that intra-cycle fluctuations can predominantly be represented by a single synergy and argues in favour of stone knapping being a highly coordinated movement. Faisal *et al.* [43] used PCA to investigate the complexity of grip patterns in the supporting hand during Oldowan and Acheulean stone knapping in one modern expert knapper. Analysis of the fingers' joint angles showed that PC1 accounted for only 25–40% of the variance in the data and five strategies (PC1–PC5) were needed to explain 85% of the variance. They also indicated no significant differences between Oldowan and Acheulean toolmaking in grip pattern complexity. Biryukova & Bril [31], who investigated arm segment kinematics of the striking arm in stone bead knapping among Indian workers, used a similar approach. They reported that PC1 accounted for 79–98% of the variation in joint angle data. They also found a negative relationship between

level of expertise and percentage of variance accounted for by PC1. Based on these two studies we hypothesized (H4) that the percentage of covariance accounted for by PC1 would be greater in the PH technique than in the other techniques, thus revealing a less complex technique. Our study partially invalidates this hypothesis as there was no significant difference between PH and BP, in terms of both kinematics and muscle activity. Nonetheless, FH was distinguished from the other two: for kinematics, PC1 was lower (70%) than BP and PH (both approx. 75%). This result tends to indicate that BP and PH share the same level of complexity while, given the smaller part of variance accounted by the first synergy in FH, the later technique would be more complex. This difference in kinematic strategies is not corroborated by the intra-cycle variation of EMG as PC1 was higher for FH than for BP and PH, this time indicating a less complex task from a muscle activation strategy point of view.

If a definitive and comprehensive answer to this apparent discrepancy between kinematic and muscle activation strategies remains to be explained, a few elements are presented. First, we found that regardless of the technique, the percentage of variance explained by PC1 was higher for muscle activity than for kinematics. The percentage of variance explained depends on the numbers of degrees of freedom accounted for by the regression model (i.e. the loading factors). We analysed 14 kinematic degrees of freedom and 14 muscles; therefore, this cannot be an explanation in our study. An identical result was previously reported by Tagliabue *et al.* [88] who argued that this may reflect the higher degree of motor redundancy compared to kinematic redundancy, even if all muscles acting during the movement were not recorded [89]. Tagliabue *et al.* [88] hypothesized that muscle synergies are thus only partially at the source of kinematic synergies. One evident illustration is that muscle activity and kinematics are totally dissociated under strict isometric conditions. The higher contribution of *Biceps brachii* in the FH technique over PH and BP is especially remarkable for the non-striking limb. This result highlights the essential role of the non-dominant/supportive limb in the evolution of stone tool knapping, as previously stressed [73,90]. Lastly, a closer look at loading factors shows that, compared to the wrist and elbow–forearm, the shoulder accounted for little variance in the kinematics strategy revealed by PC1, in line with the limited mobility reported in the analysis of joint excursion. The elbow joint played a greater role in the strategy than the wrist joint, as previously reported [90].

In an evolutionary perspective, analyses of motor control demands emphasize that FH is more complex than PH and BP in terms of joint angle synergies but less complex in terms of muscle synergies, partially invalidating our fourth hypothesis (H4). Interestingly, FH greater distinguished from the two other techniques. This may indicate that the transition from anvil and hammer percussive techniques (PH and BP) to freehand knapping techniques (FH) would have been associated with better motor control. This better motor control may have originated from the acquisition of a behavioural repertoire that gradually formed an evolutionary advantage for dissociated bimanual limb movements in general and stone tool production in particular [90]. Task complexity and motor control demands are multifactorial, and their analysis remains an ongoing concern [31,37]. Variance accounted for by PC1 is an indicator among

others, and further studies using complementary approaches are needed to get a more comprehensive view on this point.

#### 4.5. Limitations

Some limitations are acknowledged. Limitations typically associated with marker-based motion analysis and surface electromyography apply. More specifically, joint angles results depend on the kinematic model used and may be affected by simplification, especially at the shoulder level. Muscle demand results are inevitably sensitive to the EMG normalization process based on MVC that relies on individual will and the posture retained by experimenters. This study investigated muscle and kinematic demands of a single knapper. Even if we report high degree of intraindividual repeatability, the results of this study would need to be reinforced by including a panel of experts to ensure that our main conclusions withstand the interindividual variation, especially from an anatomical point of view [26]. The recruitment of experts would necessitate a long-time training period for them to master the replication of the three techniques of interest here [48–50]. Our findings are based on a modern human morphology that significantly differs from fossil hominins. Modern humans remain the best extant analogue [91] for experimental studies, but biomechanical simulation could help to further address the influence of musculoskeletal variation such as bone morphology and muscle attachment sites [10,12,47]. This study aimed at considering the overall musculature and mobility of the upper limb at three joints (wrist, elbow and shoulder) in an evolutionary perspective. Similarly, additional biomechanical analyses focused on the hand should be of prime interest since this anatomical complex was intensively studied in the frame of stone tool use and making. In line with this limit, the synergies being dependent on the number of variables included in the matrix, additional muscles or joint angles may marginally alter our findings. Each cycle was considered independent and unrelated to another [43,44]; considering that physical

demands and synergies may still be influenced by the varying size and shape all along the replication session, this assumption should be addressed through an additional dedicated study.

**Ethics.** The participant in this study gave his written informed consent under guidelines of the local research ethics committee and the protocol was carried out in compliance with the Helsinki Declaration.

**Data accessibility.** Data are available from Dryad: <https://doi.org/10.5061/dryad.cfxpvnv51> [92]. Code can be downloaded from: [https://github.com/mdomalai/BiomechStoneToolmaking\\_RSI](https://github.com/mdomalai/BiomechStoneToolmaking_RSI). The data are provided in the electronic supplementary material.

**Authors' contributions.** G.D. and M.D. designed the study/experiments. R.M. wrote the original manuscript. S.H., J.L. M.B. and S.P. collected the raw material from the field. M.B. made the stone tool replications. L.H. and M.D. collected the data. R.M. and M.D. made the analyses. All authors contributed in the interpretation and edited the manuscript. All authors gave final approval for publication and agree to be held accountable for the work performed therein.

**Competing interests.** We declare we have no competing interests.

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