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Independently tuning elastomer softness and firmness by incorporating side chain mixtures into bottlebrush network strands

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ABSTRACT

Softness and firmness are opposing traits that synergistically define the elastic response of biological systems. Currently, no single class of synthetic materials including elastomers and gels provides independent control of these mechanical characteristics, particularly without altering chemical composition. To address this challenge, we explore a hierarchical bottom-up approach via architectural modulation of bottlebrush mesoblocks followed by their self-assembly into linear-brush-linear triblock copolymer networks. By judiciously incorporating side chains of different lengths, we seamlessly demonstrate full control over elastomer firmness at a fixed Young's modulus thus bypassing the infinitely laborious synthesis of targeted side chain lengths. This industrially scalable iteration upon the design-by-architecture approach to network construction delivers thermoplastic elastomers with unprecedented softness-firmness combinations desired in soft robotics, flexible electronics, and biomedical devices.

INTRODUCTION

Stress-strain responses of elastic materials can be expressed by two distinct mechanical characteristics: (i) Young's modulus (E_0), which defines material stiffness (or softness) at small strains, and (ii) firmness (β) which characterizes stiffening during deformation (**Figure 1A**).^{1,2}

Although firmness is colloquially used in the English language as a synonym of stiffness, various sectors in industry use this mechanical label to characterize the resistance to deformation of *soft* systems such as mattresses,³ food,⁴ and biological tissues.⁵ In other words, *firmness is not stiffness*. This distinction is observable in stress-strain curves of representative classes of soft materials (**Figure 1A**). Specifically, tissues and gels may show similar softness with $E_0 \sim 10$ kPa, but their stress-strain curves rapidly diverge during deformation.⁶ This intense strain-stiffening represents one of Nature's defense mechanisms preventing accidental rupture and uncontrolled sagging of living tissues.

While the molecular mechanism of biological firmness is complex and viscoelastic in nature,^{7,8} the structural interpretation of polymer network's elastic response is straight forward.^{1,9} The non-linear modulus increase results from finite extensibility of network strands defined by the initial mean-square end-to-end distance between crosslinks $\langle R_{in}^2 \rangle$ to the square of the strand contour length R_{max}^2 as $\beta = \langle R_{in}^2 \rangle / R_{max}^2$ within interval $0 < \beta < 1$ (**Figure 1A**). Networks with flexible strands ($R_{in} \ll R_{max}$) display weak strain-stiffening with $\beta \cong 0.01 - 0.1$, while semiflexible networks ($R_{in} \sim R_{max}$) are characterized by $\beta \approx 0.1 - 1$.

For various elastic systems, the softness (E_0) and firmness (β) are readily quantified by fitting experimental stress-strain curves (**Figure 1A**) with the following equation of state:⁹

$$\sigma_{true}(\lambda) = \frac{E}{9}(\lambda^2 - \lambda^{-1}) \left[1 + 2 \left(1 - \frac{\beta(\lambda^2 + 2\lambda^{-1})}{3} \right)^{-2} \right] \quad (1)$$

where E is the structural modulus related to crosslink density. Jointly, E and β define the Young's modulus $E_0 = E(1 + 2(1 - \beta)^{-2})/3$, which corresponds to the stress-strain slope at $\lambda \rightarrow 0$. By plotting the extracted parameters of various elastic systems on an $[E_0, \beta]$ map, we expose a remarkable absence of independent control over E_0 and β to cover the entire map (**Figure 1B**).

For instance, conventional elastomers with flexible strands exhibit low firmness $\beta < 0.01$ and relatively high modulus $E_0 > 10^5$ Pa as they are architecturally limited by chain entanglements.^{10,11} In polymer gels, swelling with solvent enables decoupling the elastic features that leads to both dilution of network crosslinks and strand extension towards lower E_0 and higher β , respectively. However, gels are also limited by strand entanglements bounding firmness to $\beta < 0.2$ (**Figure 1B**).^{6,11} Although significant progress has been achieved with more complex architectures such as dual network gels¹² and sacrificial crosslinks,¹³ these systems face similar limitations ($\beta < 0.4$) and typically possess high E_0 due to dense crosslinking.⁶ On the opposite end of the $[E_0, \beta]$ map, we realize biology's unrivaled mechanics demonstrating broad softness $10^2 < E_0 < 10^6$ and firmness $\beta > 0.7$ (**Figure 1B**).^{6,14-16} Yet, from the $[E_0, \beta]$ map, it is apparent that neither Nature nor current synthetic strategies contain the tools to successfully decouple E_0, β over the entire elastic landscape. Therefore, the goal of this study is to develop a materials design platform that broadly and independently varies firmness and softness. Specifically, we aim to demonstrate continuous firmness enhancement from $\beta \sim 0 \rightarrow 1$ at constant Young's modulus E_0 .

Figure 1. The elastic landscape. (A) Representative stress-elongation curves of various elastic materials with similar softness ($E_0 = 20$ kPa), but vastly distinct firmness: PAM gel (blue),⁶ a

covalently crosslinked brush elastomer (magenta, $n_x=600$, $n_{sc}=14$, $n_g=2$),¹⁷ and fetal membrane tissue (red).⁶ Linear elastomers (green) cannot reach tissue relevant softness due to linear entanglements.¹⁰ (B) $[E_0, \beta]$ map depicting distinct classes of materials including linear elastomers ($\square$),^{1,10,11} gels ($\diamond$),⁶ brush-like elastomers ($\triangle$),^{17,18} and tissue ($\circ$).⁶

In this regard, brush-like polymers^{6,17-27} offer a promising path forward by exploiting the oxymoronic duality of side chains as mechanical softeners and stiffeners. At a given network strand length, introducing side chains has two concurrent effects: (i) increased strand volume resulting in decreased E_0 and (ii) strand extension resulting in enhanced β . Two classes of brush elastomers mimic the mechanical properties of gels and tissues: (i) covalently crosslinked elastomers^{17,18} and (ii) physically crosslinked elastomers obtained by self-assembly of linear-brush-linear (LBL) triblock copolymers.^{6,27} The elastic footprint of covalently crosslinked brush-like elastomers is strikingly similar to those of gels with limited firmness of $\beta < 0.3$ (**Figure 1B**).^{17,18} Therefore, we focus on elastomers, which afford higher firmness due to the strong segregation of both the compositionally and architecturally distinct blocks.^{6,27,28} In previous studies, varying brush block length and linear block length led to an undesirable simultaneous increase of E_0 and β .²⁷ To enable independent control over E_0 and β , we employed longer side chains, which excel at respectively augmenting strand volume and stiffness.⁶ Although these materials successfully decouple E_0 and β as the first elastomers to replicate the unprecedented softness-firmness combination of tissue, they encompassed a narrow elastic range. Therefore, broadly augmenting both side chain length and linear block volume fraction paves a pathway to covering the entire landscape within a single copolymer platform as investigated by this report.

RESULTS AND DISCUSSION

One of the most efficient ways to vary the average degree of polymerization (DP) of side chains, $\langle n_{sc} \rangle$, is through copolymerization of small and large (macro)monomers at controlled molar fractions (**Figure 2**). This side chain mixing approach bypasses the commercial limitations found in previous brush systems with monodisperse side chains^{6,27} by enabling broad and continuous tuning of $\langle n_{sc} \rangle$ with minimum synthetic efforts while delivering elastomers with well-defined mechanical properties.

Figure 2. Linear-Bottlebrush-Linear (LBL) plastomer synthetic route. Copolymerization of two PDMS-MA macromonomers with $n_{sc}=14$ and 71 , and MMA monomer enables accurately tuning the average $\langle n_{sc} \rangle$ of the brush block within LBL macromolecules that subsequently self-assemble into physical networks.

To validate this approach, we have synthesized nine series of LBL triblock copolymers with increasing $\langle n_{sc} \rangle$ (**Table 1**) via atom transfer radical polymerization (ATRP). In the comb group (Series 1-3), $\langle n_{sc} \rangle$ was controlled by the copolymerization of poly(dimethylsiloxane)-methacrylate (PDMS-MA) macromonomer ($n_{sc} = 14$) and methyl methacrylate (MMA) monomer (**Figure 2**). In the bottlebrush group (Series 4-9), $\langle n_{sc} \rangle$ was varied by randomly copolymerizing (PDMS-MA) macromonomers with $n_{sc} = 14$ and 71 (**Figure 2**). Each series contains triblocks with different volume fractions (ϕ_L) of PMMA chosen as the linear block (for complete data sets see **Table S1**, **Table S2** and **Figure S1-S18**), although additional L-block chemistry should be investigated in future work. Side chain inclusion during polymerization was monitored by time resolved ^1H -NMR showing an anticipated enrichment of shorter macromonomers at initial degrees of conversion

(~10%) but yield brush blocks within stoichiometric expectations (<15%) (**Figure S1-S10, Table S3 and Table S4**). The resulting bottlebrush dimensions and side-chain homogeneity along the backbone were verified by atomic force microscopy (AFM) and ultra-small angle X-ray (USAXS) (**Figure 3**). Molecular imaging of dense monolayers by AFM reveals evenly spaced worm-like macromolecules with no signs of bimodality (**Figure 3A**). The spacing increases linearly with side chain weight average $\langle n_{sc,w} \rangle$ (**Figure 3B**), which is consistent with the thermodynamically preferred adsorption of longer side chains to substrates.²⁹ Likewise, USAXS measurements of bulk LBL plastomers **and B block melts** show a consistent monomodal shift of a characteristic scattering peak around $q \approx 1 \text{ nm}^{-1}$ (**Figure 3C**), which is typically oversimplified as a backbone-backbone correlation or brush diameter.^{28,30-32} The resulting spacing $\xi = 2\pi/q$ scales with $\langle n_{sc} \rangle$ as $\xi \sim \langle n_{sc} \rangle^{0.41 \pm 0.01}$ (**Figure 3D**) and is consistent with recent small-angle neutron scattering ($\xi \sim n_{sc}^{0.40 \pm 0.04}$),³² computer simulations ($\xi \sim n_{sc}^{0.39 \pm 0.01}$), and theoretical studies ($\xi \sim n_{sc}^{3/8}$).³³ The last highlights the complex physical origin of ξ due to coupled density fluctuations from both backbone monomers and side chains constrained by melt incompressibility.³³ The theory considers dependence of n_{sc} on the effective bottlebrush block Kuhn length as $b_K \sim n_{sc}^{1/2}$ resulting in $\xi \sim n_{sc}^{1/4} b_K^{1/4} \sim n_{sc}^{3/8}$, which is weaker than the distance between brush backbones $\xi \sim n_{sc}^{1/2}$. A weaker power law may be also explained by an increased distance between neighboring side chains along the backbone with longer n_{sc} as $l \sim n_{sc}^\alpha$, which would lead to $\xi \sim n_{sc}^{1/2} / l = n_{sc}^{1/2-\alpha}$.

Table 1: Molecular parameters of LBL block-copolymers

Sample	m_1/m_2^c	n_{sc}^d	n_{bb}^e	n_L^f	ϕ_L^g	Schematics
Series 1 ^a MMA/M11 50/50	52/48	7.5	336	78	0.069	Combs
		7.5	336	102	0.089	
		7.5	336	119	0.102	
Series 2 ^a MMA/M11 25/75	27/73	10.8	196	34	0.038	
		10.8	196	58	0.062	
		10.8	196	64	0.068	
Series 3 ^a MMA/M11 10/90	11/89	12.9	197	29	0.027	
		12.9	197	52	0.047	
		12.9	197	76	0.067	
Series 4 ^b M11/M17 100/0	100/0	14.4	363	57	0.026	Bottlebrushes
		14.4	363	116	0.053	
		14.4	363	168	0.077	
Series 5 ^b M11/M17 75/25	84/16	23.6	285	88	0.026	
		23.6	285	123	0.036	
		23.6	285	201	0.059	
Series 6 ^b M11/M17 50/50	66/34	33.8	249	62	0.014	
		33.8	249	106	0.024	
		33.8	249	133	0.029	
Series 7 ^b M11/M17 25/75	42/58	47.1	308	187	0.025	
		47.1	308	261	0.035	
		47.1	308	430	0.058	
Series 8 ^b M11/M17 0/100	0/100	71.2	447	288	0.020	
		71.2	447	604	0.041	
		71.2	447	772	0.052	
		71.2	447	894	0.060	
Series 9 ^b M11/M17 0/100	0/100	71.2	292	144	0.021	
		71.2	292	263	0.038	
		71.2	292	468	0.067	
		71.2	292	696	0.099	

^aBrush blocks copolymerized with molar fractions MMA and PDMS-MA $n_{sc} = 14$ (M11) macromonomers. ^bBrush blocks copolymerized with molar fractions of PDMS-MA $n_{sc} = 14$ (M11) and $n_{sc} = 71$ (M17) macromonomers. ^cFinal copolymer molar fractions measured by ¹H-NMR (**Figure S1-S10**) where m_1 and m_2 are molar fractions of the respective (macro)monomers. ^dNumber average degree polymerization of side chains calculated as $n_{sc} = m_1 n_{sc,1} + m_2 n_{sc,2}$. ^eNumber average degree polymerization of brush backbones. ^{f,g}Degree polymerization and volume fraction of linear MMA blocks as determined from ¹H-NMR (**Figure S11-S18**) where $\rho_{PMA} = 1.15 \text{ g/mL}$, $\rho_{PDMS} = 0.96 \text{ g/mL}$.

Figure 3. LBL Characterization. (A) Atomic force microscopy micrographs of Langmuir-Blodgett monolayers of brush blocks show increased interbrush distance with increasing fractions of long side chains ($n_{sc} = 71$). (B) Interbrush distance as determined by AFM (**Figure S19** and **Table S5**) increases linearly with weight average $\langle n_{sc,w} \rangle$. (C) The brush scattering peak, as determined in recent literature,^{6,28} consistently shifts to lower magnitudes of the scattering wavevector q with increasing number average side chain length $\langle n_{sc} \rangle$. (D) The brush scattering distance peak position ($\xi = 2\pi/q$) increases with $\langle n_{sc} \rangle$ as $\xi \sim \langle n_{sc} \rangle^{0.41}$ (inset), which is consistent with theoretically predicted scaling behavior $\xi \sim n_{sc}^{3/8}$.²⁵ The dashed line corresponds to a linear fit with $\xi = 0.5 + 1.2n_{sc}^{0.41}$. The solid and open symbols correspond to LBL elastomers and melts of brush blocks, respectively, including a melt of PDMS bottlebrushes with long side chains ($n_{sc} = 156$). Importantly, upon background subtraction the brush scattering peak reveals its second order which indicates that packing of the bottlebrush segments is characterized by long-range order (cf. **Figures S24-25**).

For each sample in all nine series, we measured their stress-elongation response (**Figure S20**) and characterized their E_0 and β (**Figure S20**, **Table S1** and **Table S2**). Two sets of representative curves with either similar E_0 and varied β (**Figure 4A**) or vice versa (**Figure 4B**) demonstrate the unprecedented ability of the LBL plastomer platform to cover the $[E_0, \beta]$ landscape. In **Figure 4A**, the curves show significant variation of strain-stiffening (β) at nearly constant slope at $\lambda \rightarrow 1$ (E_0) with larger $\langle n_{sc} \rangle$. In **Figure 4B**, increasing E_0 at nearly constant β was achieved by concomitantly varying $\langle n_{sc} \rangle$ and volume fraction of the linear block (ϕ_L) as indicated. The corresponding E_0 and β values were extracted by fitting the stress-strain curves with Equation 1 with an $[E_0, \beta]$ map of all synthesized materials confirming near complete β coverage within a given E_0 range (**Figure 4C**). The map yields several notable correlations highlighted by dashed cross-sectional lines: (i) Horizontal cross section I represent collections of plastomers with constant E_0 and increasing β similar to those found in **Figure 4A** as achieved by larger $\langle n_{sc} \rangle$. (ii) Two vertical cross sections II and III correspond to plastomers with constant β and variable E_0 realized by concomitantly varying ϕ_L and $\langle n_{sc} \rangle$ (**Figure 4B**). (iii) Diagonal dashed lines correspond to plastomers with a given $\langle n_{sc} \rangle$ (Series 1-9 in **Table 1**), where increasing ϕ_L simultaneously increases E_0 and β up the coalesced line, which can be exploited to fill the elastic landscape beyond the reported samples. These correlations enable general design rules towards architecturally traversing the $[E_0, \beta]$ landscape. Further theoretical analysis discussed in literature^{6,34} allows collapsing the individual series trends into distinct correlations for bottlebrushes and combs (**Figure 4D**), which demonstrates overarching universality by normalizing the attained mechanical properties (E_0, β) by their corresponding architectural parameters (n_{bb} , n_{sc} , n_L , ϕ_L). However, trendline boundaries are currently ill-defined as there could be a change in microdomain symmetry upon reaching high ϕ_L ,³⁵ which will be a topic of future study.

Further demonstrating the adaptability of the side chain mixing approach, we deliberately introduce heterogeneous distribution of side chains with different n_{sc} along the brush backbone. To this end, we have synthesized two pentablock copolymers $LB_{14}B_{71}B_{14}L$ and $LB_{71}B_{14}B_{71}L$, where B_{14} and B_{71} correspond of monodisperse blocks with $n_{sc}=14$ or $n_{sc}=71$ side chains, respectively (**Figure S21** and **Figure S22**). The two brush triblocks ($B_{14}B_{71}B_{14}$ and $B_{71}B_{14}B_{71}$) with inverted side chains distributions were grown to have similar $\langle n_{sc} \rangle \cong 47$ (**Table S6**), which is analogous to Series 7 in **Table 1**. The stress-elongation curves (**Figure 4E**) of these blocky plastomers show slightly lower β from Series 7 obtained with random copolymerization (**Figure 4F**), and although they differ in ϕ_L and n_{bb} (**Table S6**), their similar $\langle n_{sc} \rangle$ enables their self-consistent trend line that is reminiscent of random copolymerization. This observation suggests that LBL plastomer footprint on the $[E_0, \beta]$ landscape is largely $\langle n_{sc} \rangle$ controlled, however, the precise effect of side chain distribution within a given brush strand will be investigated in future studies.

Figure 4. Mechanical Characterization. (A) Stress-elongation curves of selected LBL plastomers with similar $E_0 = 25$ kPa and different β . (B) Stress-elongation curves of LBL plastomers of two groups (dashed vs solid line) respectively with similar $\beta = 0.77$ and $\beta = 0.46$ but different E_0 . (C) Elastic parameters of reported LBL plastomers extracted from a collection of stress-elongation curves (**Figure S20**) on an $[E_0, \beta]$ map. Each colored symbol set represents a series according to **Table 1**. Dashed lines are provided to guide the reader and delineate the coalescence of each series.

Collections of stress-elongation with either constant E_0 and different β (**Figure 4A**) or constant β and different E_0 (**Figure 4B**) may be identified by respectively dropping lateral lines (I) or vertical lines (II,III). General design rules (arrows) can be inferred for tuning mechanical properties (E_0 , β) with architectural parameters (n_{bb} , n_{sc} , n_L , ϕ_L). (D) Universal **collapse of mechanical properties in relation to their architectural parameters informed** by theoretical considerations **from literature**^{6,34} provides a direct route for programmable design, where $\varphi = n_g/(n_g + n_{sc}) = (1 + n_{sc})^{-1}$ or the volume fraction of the backbone in the brush ($n_g = 1$) block. Both bottlebrushes and combs exhibit distinct coalescence due to their fundamental difference in their effective Kuhn length.³⁶ (E) Stress-elongation curve profiles of LB₁₄B₇₁B₁₄L and LB₇₁B₁₄B₇₁L pentablock elastomers. (F) LB₁₄B₇₁B₁₄L and LB₇₁B₁₄B₇₁L pentablock elastomers on the elastic map programmed with $\langle n_{sc} \rangle$ similar to series 7. The observed shift is likely due to small errors in determining $\langle n_{sc} \rangle$ of randomly mixed brushes (**Figure S6** and **Figure S7**).

CONCLUSION

In conclusion, self-assembly of linear-bottlebrush-linear macromolecules yields physical networks that are able to span the entire elastic landscape via their architectural multiplet $[n_{bb}, n_{sc1}, n_{sc2}, n_L, \phi_L, m_1]$, where m_1 is the molar fraction of side chain with DP = n_{sc1} . Specifically, the side chain mixing approach allows covering the entire firmness range at a given Young's modulus to replicate the elastic properties of both synthetic gels and biological tissue. Thus, the average side chain length $\langle n_{sc} \rangle$ is the defining architectural feature that enables **encoding** unique pairings of both softness and firmness **into elastomers**. We believe this industrially friendly platform **that has eluded the polymer field will revolutionize** future applications in the emerging biomedical and soft-robotics fields, **which to date have been hampered by the lack of access to these materials**.

ASSOCIATED CONTENT

The Supporting Information is available free of charge on the ACS Publications website at DOI:

Synthetic procedures with ^1H -NMR and sample summaries, atomic force microscopy and mechanical characterization with stress-elongation curves of triblock and pentablock elastomers with mixed side chains.

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Author Contributions

A.N.K. designed, synthesized, and characterized the monomers, block-copolymers, and polymer networks; A.N.K. performed mechanical tests and AFM experiments. Y.T. and A.V.D. provided theoretical analysis of mechanical properties, developed theoretical foundation for materials design and LBL networks; C.C., A.L., E.B. and D.A.I. conducted X-ray studies and data analysis; S.S.S. is the principal investigator and corresponding author; A.N.K. and S.S.S were primary writers of the manuscript. All authors discussed the results and provided feedback on the manuscript.

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