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Similar Cardioventilatory but Greater Neuromuscular Stimuli With Interval Drop Jump Than With Interval Running

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Ducrocq GP, Hureau TJ, Meste O, Blain GM *Similar Cardioventilatory but Greater Neuromuscular Stimuli With Interval Drop Jump Than With Interval Running*

Purpose: Drop-jumps and high-intensity interval-running are relevant training methods to improve explosiveness and endurance performance, respectively. Combined training effects might however be achieved by performing interval-drop-jumping. Our goal was thus to determine the acute effects of interval-drop-jumping on oxygen uptake ($\dot{V}O_2$) – index of cardioventilatory / oxidative stimulation level, and peripheral fatigue – a limiting factor of explosiveness.

Methods: Thirteen participants performed three 11-min 'interval-training' sessions, during which participants ran 15-s at 120% of the velocity that elicited maximal $\dot{V}O_2$ ($\dot{V}O_{2-MAX}$) (IT_{RUN}) or drop-jumped at 7 (IT_{DJ7}) or 9 (IT_{DJ9}) jumps per 15-s, interspersed with 15-s of passive recovery. $\dot{V}O_2$ and the time spent above 90% of $\dot{V}O_{2-MAX}$ ($T \dot{V}O_{2-MAX}$) were collected. Peripheral fatigue was quantified via pre- to post-exercise changes in evoked potentiated quadriceps twitch (ΔQT). Power output was estimated during IT_{DJs} using optical sensors.

Results: All participants reached 90% of $\dot{V}O_{2-MAX}$ or higher during IT_{RUN} and IT_{DJ9}, but only eleven did during IT_{DJ7}. $T \dot{V}O_{2-MAX}$ was not different between IT_{RUN} and IT_{DJ9} (145 ± 76 -s vs 141 ± 151 -s; $p=0.92$) but was reduced during IT_{DJ7} (28 ± 26 -s; $p=0.002$). Mean ΔQT in IT_{DJ9} and IT_{DJ7} were not different ($-17 \pm 9\%$ vs $-14 \pm 8\%$; $p=0.73$) and greater than in IT_{RUN} ($-8 \pm 7\%$; $p=0.001$). No alteration in power output was found during IT_{DJs} (37 ± 10 W.kg⁻¹).

Conclusion: Interval-drop-jumping at high work rate stimulated the cardioventilatory and oxidative systems to the same extent than interval-running, while the exercise-induced increase in fatigue did not compromise drop-jump performance. Interval drop-jumping might be a relevant strategy to get concomitant improvements in endurance and explosive performance.

Key words: *high intensity interval training, drop-jump, plyometric exercise, endurance and strength training, neuromuscular fatigue.*

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INTRODUCTION

Exercise performance of many sport disciplines (e.g. team sports, racquet sports, short and mid-distance running, etc.) requires both high endurance and muscle power output capabilities^{1,2}. Usually, these specific physical capabilities are developed separately but the increasing number of competitions in professional athletes significantly reduces the time allocated to physical training. Therefore, improving the time-efficiency of physical training is of critical importance and this goal might be achieved by combining the development of endurance and muscle power / explosiveness within the same physical exercise.

Plyometric jump-training is a well-known and effective training method to enhance the stretch-shortening cycle of muscle function and improve muscle power³⁻⁵, jump performance⁶, agility⁷, sprint ability⁵ as well as running economy⁸. Previous findings⁹ also suggest that, if effectively designed, this training method might be used to develop maximal oxygen uptake ($\dot{V}O_{2-MAX}$), a key determinant of endurance performance¹⁰. Indeed, eight series of ten drop-jumps separated by three minutes of passive recovery can elevate oxygen uptake ($\dot{V}O_2$) up to 83% of $\dot{V}O_{2-MAX}$ ⁹. Given the tight relationship between work rate and O_2 uptake¹¹, the pre-requisites of an effective plyometric jump-training approach combining improvements in $\dot{V}O_{2-MAX}$ and muscle power would be: 1) to perform a high volume of drop jumps at a high work rate to increase the metabolic demand, reach $\dot{V}O_{2-MAX}$ and maximize the time spent above 90% of $\dot{V}O_{2-MAX}$ ($T \dot{V}O_{2-MAX}$) – a threshold beyond which major cardiorespiratory and oxidative adaptations are thought to occur^{12,13}, and 2) to perform 120 drop-jumps per session or above¹⁴ with a ground contact time below 260-ms¹⁵ and at a high muscle power¹⁶ to optimize training effects on muscle power and explosiveness.

High intensity interval running is a training method commonly used by physical trainers and generally accepted as the gold standard approach for $\dot{V}O_{2-MAX}$ development¹⁷⁻²¹. Replacing the sequences of running by repeated drop jumps (i.e. interval drop-jumping) might be an effective training method to combine improvements in $\dot{V}O_{2-MAX}$ and muscle power. However, performing drop jumps at a high work rate could impair muscle activation and force / power production - that is fatigue could develop^{22,23}. The mechanisms associated with exercise-induced neuromuscular fatigue involve the alterations of processes within the muscle (i.e. peripheral fatigue)²⁴ and/or the central nervous system (i.e. central fatigue)²⁵. Little is known on the time-course of neuromuscular fatigue recovery following a high-volume of drop jumps and on the contribution of peripheral and central fatigue to force recovery. Moreover, fatigue during repeated drop jumps might be associated with a loss of tolerance of stretch loads, a progressive lengthening of the ground contact time and a reduction in muscle power¹⁶, which may not be optimal to improve the stretch shortening cycle^{15,16}.

To date, the effects of interval drop-jumping on the time spent above 90% of $\dot{V}O_{2-MAX}$, on neuromuscular fatigue and on jumping performance characteristics are unknown. This is crucial because the risk of such a combined training method is, while trying to develop both capabilities at the same time, to finally not stimulate the underlying physiological processes enough to get significant training adaptations in any of these capabilities^{12,15}. The purpose of the present study was thus to test the $\dot{V}O_2$, neuromuscular fatigue and jump performance responses to interval drop-jumping, during which sequences of repeated drop-jumps at two different jumping frequencies (i.e. two different work rate) were alternated with sequences of passive recovery. We hypothesized that 1) $\dot{V}O_{2-MAX}$ can be reached during interval drop-jumping at a high work rate and 2) the time spent at $\dot{V}O_{2-MAX}$ is dependent upon the level of work

rate and the total amount of work. We also aimed to determine whether the increase in work rate, necessary to elevate $\dot{V}O_2$ to $\dot{V}O_{2-MAX}$ level, would increase neuromuscular fatigue to a degree that would compromise drop jump performance. The responses from interval drop-jumping were then compared to the responses obtained during high-intensity interval running of similar duration.

METHOD

Participants.

Nine males and four females participated in this study (age = 21.2 ± 1.9 years [mean $\pm$ SD], height = 173.1 ± 9.0 cm, body mass = 67.4 ± 9.4 kg, body fat = 17.1 ± 6.6 %). All participants were students at the faculty of Sport Sciences and trained at least three times per week in team or racket sports. The study was approved by the local ethics committee and conducted according to the Helsinki Declaration for human experimentation.

Experimental Design.

During two preliminary visits, participants were thoroughly familiarized with testing procedures. The drop height that produced the greatest power output was determined. Participants also performed a maximal incremental exercise test ($9\text{-km}\cdot\text{h}^{-1} + 0.5\text{-km}\cdot\text{h}^{-1}$ every minute) until voluntary exhaustion on a motorized treadmill (RUN900, Technogym, Rome, Italy) to determine $\dot{V}O_{2-MAX}$ and the minimal velocity that elicits $\dot{V}O_{2-MAX}$ ($v\dot{V}O_{2-MAX}$). After 5-min of passive recovery, a constant-workload running test at 105% of $v\dot{V}O_{2-MAX}$ ($CW_{105\%}$) was performed until exhaustion to ensure that the peak $\dot{V}O_2$ ($\dot{V}O_{2-PEAK}$) measured during the previous incremental test corresponded to $\dot{V}O_{2-MAX}$ ²⁶.

During three separated experimental visits, participants performed an 11 min 'interval-training sessions' (IT), during which participants ran (IT_{RUN}) or repeated drop-jumps (IT_{DJ}) for 15-s, alternated with 15-s of passive recovery. No warm up preceded the ITs in order to accurately determine the time to reach $\dot{V}O_{2-MAX}$ from the start of exercise. During IT_{RUN} , participants ran at a velocity corresponding to 120% of $v\dot{V}O_{2-MAX}$. This running speed has been shown to elicit the greatest $\dot{V}O_{2-MAX}$ during a similar interval running protocol²⁷. During IT_{DJ} , participants dropped and jumped back and forth with their own sport footwear from two stackable plyometric boxes separated by one meter and from the drop height that maximized power output (Fig. 1). To modulate work rate, jumping frequency was set at either 7 (IT_{DJ7}) or 9 (IT_{DJ9}) drop-jumps per 15-s. Participants performed a total of 154 and 198 drop jumps in IT_{DJ7} and IT_{DJ9} , respectively. Participants were instructed to reach the hard linoleum surface with both feet and to jump as fast and as high as possible toward the box located in front of them. Drop-jump frequency was set by a custom-made soundtrack, with a beep occurring every time the participants had to drop and jump from one box to the other. Neuromuscular testing was performed prior and immediately after the end of every IT. Experimental sessions were performed at the same time of day. To account for potential order effects, a randomized block design was used for the three experimental visits.

Figure 1. Schematic of the interval drop-jumping procedure. Participants dropped and jumped back and forth with their own sport footwear from two stackable plyometric boxes separated by one meter and from the drop height that maximized power output. The frequency at which the participants had to jump was set by a custom sound-track. Note that during the last jump, the participants landed on the floor to quantify power output, jump height and reactive strength index.

Data collection and analysis

Drop-jump height and mechanical performance. Prior to every maximal incremental exercise test, participants performed a series of drop-jumps with both feet at 20, 30, 40, 50 and 60-cm (random order). Drop-jumps were repeated three times at every height and separated by 1-min of passive recovery. To ensure that performance was maximized during each drop-jump, participants were instructed to jump "as fast and as high as possible"²⁸. Power output, jump height and the reactive strength index were estimated from the ground contact and the flight times, measured by an optical acquisition system (accuracy: 0.001-s; OPTOJUMP, Microgate, Bolzano, Italy)²⁹. The drop height (45 ± 12 cm) that elicited the greatest power output (43 ± 14 W.kg⁻¹) was subsequently used during IT_{DJ7} and IT_{DJ9} ²⁸. At this drop height, the jump height (31.4 ± 10.6 cm) and the reactive strength index (1.59 ± 0.6 m.s⁻¹) corresponded to 97.8 ± 3.7 % and 99.1 ± 2.1 % of their maximum value (estimated during the series of drop-jumps from different heights), respectively. During IT_{DJ} s, ground contact time was recorded during each jump. Participants were also instructed to land between the optical sensors (*i.e.* on the floor) following the last jump of every work bout to estimate power output, the jump height, and the reactive strength index.

Exercise responses. Minute ventilation ($\dot{V}_E$), breathing frequency (f_R), tidal volume (V_T), oxygen uptake ($\dot{V}O_2$) and carbon dioxide output ($\dot{V}CO_2$) were measured breath-by-breath at rest and during exercise using a calibrated stationary automatic ergospirometer (MS-CPX, Viasys, San Diego, California, USA). Heart rate (HR) was recorded by a heart rate monitor (RS800CX, Polar Electro, Kempele, Finland) and averaged every 5-s. Blood lactate concentration ($[La]_b$) was determined at rest and 3-min post-exercise by an ampero-metric method (LactatePro, Arkray, Kyoto, Japan) using blood samples collected from a fingertip (5 μ l). Rate of perceived exertion was obtained at rest and at every minute during exercise using the Borg's modified CR10 scale³⁰.

Processing of the gas exchange data. During exercise, breath-by-breath data were disrupted by occasional errant breaths (*e.g.* swallows, coughs, sighs), which were not considered as part of the underlying physiological response to exercise. To remove these artifacts, raw data were linearly interpolated to obtain one

datapoint per second and fitted using an exponential function. The resulting fitted curve was subtracted from the raw signal and the data exceeding three times the standard deviation of the residual signal were removed³¹. $\dot{V}O_{2-MAX}$ was calculated for every IT_s as the time during which $\dot{V}O_2$ was equal to or exceeded 90% of $\dot{V}O_{2-MAX}$. To test the effect of work rate on $\dot{V}O_{2-MAX}$ during IT_{DJs}, $\dot{V}O_{2-MAX}$ was also determined during IT_{DJ9} when the same amount of work than IT_{DJ7} was completed (i.e. 154 drop-jumps; IT_{DJ9 ISO-WORK}).

Contractile properties and voluntary activation. For the assessment of the contractile function, participants were seated on a custom-made bench with a trunk/thigh angle of 135° and the right knee joint angle at 90°. A non-compliant strap attached to a calibrated load cell (model SM-2000N, Interface, Scottsdale, AZ, USA) was fixed to the participant's right ankle. The cathode electrode (3 x 3 cm, Ag-AgCl, Mini-KR, Contrôle-Graphique, Brie-Comte-Robert, France), was placed on the femoral triangle, at the stimulation site which resulted in both the maximal force output and the maximal amplitude of the compound muscle action potential (M_{MAX}) for the *vastus lateralis* (VL), *vastus medialis* (VM) and *rectus femoris* (RF). The anode electrode (70 x 50-mm) was placed on the gluteal fold. A constant current stimulator (DS7A, Digitimer, Hertfordshire, United-Kingdom) delivered a square wave stimulus (1-ms) at a maximum of 400 V. To assure maximal spatial recruitment of motor units during the neuromuscular tests, the stimulation intensity (201 ± 30 mA) corresponded to 120% of the intensity eliciting maximal quadriceps twitch and M_{MAX} . For the evaluation of the quadriceps function, potentiated quadriceps twitches were measured 3-s after a maximal voluntary contraction (MVC). Six MVCs, separated by 1-min, were performed prior to every IT. Following exercise, measurements of the neuromuscular function were obtained exactly at 30-s, 1, 2, 4 and 6-min post-exercise. Potentiated quadriceps twitch force evoked by paired 100Hz (QT₁₀₀), 10Hz (QT₁₀) and single (QT_{single}) electrical stimulations of the femoral nerve were elicited 3, 6, and 9-s after each MVC, respectively. For all QT₁₀, QT₁₀₀, and MVCs, we determined peak force. For all QT_{single}, peak force, contraction time to peak force (CT), maximal rate of force development (MRFD, maximal value of the first derivative of the force signal) and half relaxation time (HRT, time to obtain half of the decline in maximal force) were assessed. Superimposed paired stimuli at 100Hz (QT_{100,superimposed}) were delivered during the peak force of each MVC to determine voluntary activation of the quadriceps (VA)³². Voluntary activation was calculated as follows: $VA (\%) = (1 - QT_{100,superimposed} / QT_{100}) \times 100$. Quadriceps fatigue was calculated as the difference in evoked twitch force from pre- to post-exercise and expressed as a percent change from pre-exercise (ΔQT_{single} , ΔQT_{10} , and ΔQT_{100}). A decrease in the ratio QT_{10} / QT_{100} ($QT_{10:100}$) was used as an index of low-frequency fatigue³³.

Surface electromyography (EMG). Electrical activity of the right VL, VM and RF was recorded by pairs of Ag/AgCl surface electrodes (diameter = 10 mm; inter-electrode distance = 20 mm; impedance = 1.7 ± 0.8 kΩ) placed on the muscle belly and connected to an EMG system (Octal Bio-Amp, ML138, ADInstrument, Bella-Vista, Australia). The reference electrode was placed on the right lateral tibial condyle. EMG signals were amplified (gain = 20 mV), filtered (bandwidth frequency, 0.03 Hz – 1 kHz), and recorded (sampling frequency, 4 kHz) using a

commercially available software (Labchart 7, ADInstruments, Bella-Vista, Australia). Each burst onset and offset of the rectified EMG signal recorded during each work bout of every IT was determined. The root mean square (RMS) of each burst from the EMG signal was calculated, normalized to the RMS recorded during pre-exercise MVC ($RMS_{\%MVC}$) and averaged. RMS during each MVC was calculated as the average value over a 0.5-s interval during the plateau phase of the MVC³⁴.

Statistical analysis.

Data presented in the results section are expressed as mean $\pm$ SD. Normality of every dependent variable and homogeneity of the variance of the distributions were confirmed using the Kolmogorov-Smirnov test and the Levene test, respectively. Reliability of $\dot{V}O_{2-MAX}$ and $v\dot{V}O_{2-MAX}$ determined from the two maximal incremental exercise tests was tested by verifying that both samples did not differ using Student's paired t-test and by evaluating how strongly these samples resembled to each other using intraclass correlation coefficients (ICC) and coefficients of variation³⁵. Reliability was considered excellent, good, fair and poor when ICC was > 0.75 , $0.75 - 0.60$, $0.60 - 0.40$, and < 0.40 , respectively³⁶. A multivariate analysis (MANOVA) was conducted on our dependent variables to protect against the risk of type I error arising from multiple comparisons³⁷. A significant ($p < 0.01$) condition $\times$ time effect was found for both the exercise and post-exercise recovery dataset. Then, two-way ANOVAs with repeated measures were used to test for condition effect across time. In addition, a one-way ANOVA with repeated measures was used to determine differences across conditions on absolute values of $\dot{V}O_{2-MAX}$, time to reach 90% of $\dot{V}O_{2-MAX}$, $\Delta \dot{V}O_2$ and $[La]_b$. When a significant difference was found, multiple comparisons analysis was performed using the Tukey's HSD test. Effect size was assessed using partial eta-squared (η^2). Statistical analyses were conducted using Statistica 8.0 (StatSoft, Inc., Tulsa, OK, US). Statistical significance was set at $p < 0.05$.

RESULTS

Determination of $\dot{V}O_{2-MAX}$ and $v\dot{V}O_{2-MAX}$. $\dot{V}O_{2-PEAK}$, peak HR and $[La]_b$ recorded during every exercise trial are presented in Table 1. No significant difference was observed in $\dot{V}O_{2-PEAK}$ during maximal incremental exercise tests and subsequent CW_{105%} ($p=0.19$), showing that $\dot{V}O_{2-PEAK}$ corresponded to $\dot{V}O_{2-MAX}$. No significant difference ($p=0.90$) and "excellent" reliability ($ICC > 0.974$, $CV < 1.9\%$) were found for $\dot{V}O_{2-MAX}$ and $v\dot{V}O_{2-MAX}$ between the two maximal incremental exercise tests. Thus, $\dot{V}O_{2-MAX}$ and $v\dot{V}O_{2-MAX}$ were calculated as the average of the $\dot{V}O_{2-MAX}$ and the $v\dot{V}O_{2-MAX}$ reached during the two tests, and equaled 55 ± 7 ml.min⁻¹.kg⁻¹ and 14.4 ± 1.8 km.h⁻¹, respectively.

Gas exchange and cardioventilatory variables. As shown in Figures 2-3, $\dot{V}O_2$ ($p=0.94$), $\dot{V}CO_2$ ($p=0.97$), $\dot{V}CO_2 \cdot \dot{V}O_2^{-1}$ ($p=0.94$), $\dot{V}_E$ ($p=0.95$), $\dot{V}_E \cdot \dot{V}CO_2^{-1}$ ($p=0.99$), f_R ($p=0.14$), V_T ($p=0.14$) and HR ($p=0.37$) responses to exercise were not different between IT_{DJ9} and IT_{RUN} but lower during IT_{DJ7} ($p=0.001$, $\eta^2 > 0.41$). Moreover, no significant difference in $\dot{V}O_{2-PEAK}$ was found between IT_{DJ9} compared to IT_{RUN} ($p=0.64$). All participants reached 90% of $\dot{V}O_{2-MAX}$ during IT_{RUN} and IT_{DJ9}, while only 11 did during IT_{DJ7}. During IT_{RUN} and IT_{DJ9}, the time to reach 90% of $\dot{V}O_{2-MAX}$ (180 ± 116 s vs 122 ± 117 s; $p=0.30$), $\dot{V}O_{2-MAX}$ (145 ± 76 s vs 141 ± 151 s; $p=0.91$) were not different between conditions. During IT_{DJ7}, the time to reach 90% of

Figure 2. Oxygen uptake and time spent above 90% of maximal oxygen uptake during interval running and drop-jumping. Individual $\dot{V}O_2$ data were averaged every 5 s and are shown as a group mean in the left panel. Time spent above 90% of $\dot{V}O_{2\text{-MAX}}$ ($T\dot{V}O_{2\text{-MAX}}$) is presented in the right panel as mean $\pm$ SE. ITRUN, high intensity interval running at 120% of the velocity that elicited the maximal oxygen uptake; ITDJ9, interval drop-jumping at 9 drop-jumps per 15 s; ITDJ7, interval drop-jumping at 7 drop-jumps per 15 s. Error bars were omitted from the $\dot{V}O_2$ time-course in the left panel graph to aid clarity. † Indicates significant difference in ITDJ7 compared to ITRUN and ITDJ9 on the mean data ($p < 0.05$). No significant difference was found between ITDJ9 and ITRUN.

Figure 3 (previous page). Gas exchange and cardioventilatory responses to interval running and drop-jumping.

Individual gas exchange and cardioventilatory data were averaged every 5 s and represented as a group mean. $\dot{V}O_2$, CO₂ output; $\dot{V}_E$, minute ventilation; f_R , respiratory frequency; HR, heart rate; IT_{RUN}, high intensity interval running at 120% of the velocity that elicited the maximal oxygen uptake; IT_{DJ9}, interval drop-jumping at 9 drop-jumps per 15-s; IT_{DJ7}, interval drop-jumping at 7 drop-jumps per 15-s. Error bars were omitted from the time-course data to aid clarity. † Indicates significant difference in IT_{DJ7} compared to IT_{RUN} and IT_{DJ9} during exercise and on the mean data ($p < 0.05$). No significant difference was found between IT_{DJ9} and IT_{RUN}.

$\dot{V}O_{2-MAX}$ (120 ± 88 s) was not different than IT_{RUN} and IT_{DJ9}, whereas $\tau \dot{V}O_{2-MAX}$ (23 ± 26 s) was significantly reduced ($p=0.001$, $\eta^2=0.47$). $\tau \dot{V}O_{2-MAX}$ during IT_{DJ7} was also significantly reduced ($p = 0.05$) compared to IT_{DJ9} ISO-WORK (103 ± 113 s), when a similar amount of work was completed in both conditions (i.e. 154 drop-jumps). Increasing the amount of work from 154 to 198 drop jumps in IT_{DJ9} increased $\tau \dot{V}O_{2-MAX}$ (i.e. from 103 ± 113 s to 141 ± 151 s), but this difference did not reach statistical significance ($p = 0.58$). $[La]_b$ was significantly lower after IT_{DJ9} and IT_{DJ7} compared to IT_{RUN} ($p=0.001$, $\eta^2=0.81$; Table 1).

Table 1. Work duration and peak physiological responses to incremental, constant workload and interval training exercises

Visits	Work duration (s)	$\dot{V}O_{2-PEAK}$ (ml.min ⁻¹ .kg ⁻¹)	HR-PEAK (beats.min ⁻¹)	$[La]_b$ (mmol.l ⁻¹)
1 st max test	822 ± 274	55.4 ± 6.7	182 ± 11	11.2 ± 2.1
1 st CW _{105%}	150 ± 14	55.7 ± 6.7	186 ± 7	-
2 nd max test	810 ± 274	55.3 ± 7.2	182 ± 11	10.7 ± 1.8
2 nd CW _{105%}	161 ± 14	56.0 ± 6.6	184 ± 18	-
IT _{RUN}	330	54.3 ± 6.7	182 ± 11	7.4 ± 2.2*
IT _{DJ9}	330	55.7 ± 7.3	184 ± 18	5.4 ± 1.8*†
IT _{DJ7}	330	45.2 ± 6.4*†#	175 ± 14*†#	3.1 ± 1.5*†#

Work duration calculated for interval training exercise (i.e. 330s) corresponded to the sum of 22 sets of 15s work. $\dot{V}O_{2-PEAK}$, peak oxygen uptake; HR-PEAK, peak heart rate; $[La]_b$, blood lactate concentration; max test, maximal incremental exercise test; CW_{105%}, constant work load trial at 105% of the velocity that elicited $\dot{V}O_{2-PEAK}$ during the previous maximal incremental exercise test; IT_{RUN}, high intensity interval running at 120% of $\dot{V}O_{2-MAX}$; IT_{DJ9}, interval drop-jumping at 9 drop-jumps per 15-s; IT_{DJ7}, interval drop-jumping at 7 drop-jumps per 15-s. No significant physiological difference was found between the first and second maximal incremental exercise test as well as between a given maximal incremental exercise test and the subsequent CW_{105%}. *, significantly different from the maximal incremental exercise test ($p < 0.05$); †, significantly different from IT_{RUN} ($p < 0.05$); #, significantly different from IT_{DJ9} ($p < 0.05$).

Surface electromyography. Exercise had no effect on VL M_{MAX} ($p=0.26$, $\eta^2=0.10$) and VM M_{MAX} ($p=0.08$, $\eta^2=0.13$), while a significant exercise-induced reduction in RF M_{MAX} ($p=0.002$, $\eta^2=0.29$) was found in IT_{DJ9}. During exercise, VL RMS_{%MVC} ($p=0.001$, $\eta^2=0.61$), VM RMS_{%MVC} ($p=0.03$, $\eta^2=0.26$) and RF RMS_{%MVC} ($p=0.001$, $\eta^2=0.57$) were significantly greater during IT_{DJ9} and IT_{DJ7} compared to IT_{RUN} (Fig. 4). No significant difference was found between IT_{DJ9} and IT_{DJ7} (VL RMS_{%MVC}: $p=0.75$; VM RMS_{%MVC}: $p=0.95$; RF RMS_{%MVC}: $p=0.99$).

Fatigue variables. As presented in Table 2 and Figure 5, MVC, VA, QT_{single}, QT₁₀, QT_{10:100}, CT and HRT were significantly impaired following interval running and drop-jumping ($p<0.001$, $\eta^2>0.25$), whereas QT₁₀₀ ($p=0.03$, $\eta^2=0.13$) was reduced following IT_{DJ9} only. Significant reductions in MRFD were also found following IT_{DJ9} and IT_{DJ7} ($p<0.001$, $\eta^2=0.30$). ΔQT_{single} ($p=0.73$), ΔQT_{10} ($p=0.99$), $\Delta QT_{10:100}$ ($p>0.88$) and $\Delta MRFD$ ($p=0.90$) were not different after IT_{DJ9} and IT_{DJ7} but significantly greater compared to IT_{RUN} ($p<0.001$). No significant between-condition difference was found for ΔMVC ($p=0.93$, $\eta^2<0.01$), ΔVA ($p=0.30$, $\eta^2<0.10$), ΔQT_{100} ($p=0.09$, $\eta^2=0.18$), ΔCT ($p=0.43$, $\eta^2=0.06$) and ΔHRT ($p=0.54$, $\eta^2=0.05$).

Figure 4. Quadriceps electromyographic amplitude during interval running and drop-jumping.

Data are presented as mean ± SE. Muscle activation was calculated as the root mean square (RMS) of each burst recorded during exercise. These data were averaged for each work bout and normalized by the RMS calculated during pre-exercise maximal voluntary isometric contractions (RMS%MVC). VL, vastus lateralis; VM, vastus medialis; RF, rectus femoris; IT_{RUN}, high intensity interval running at 120% of the velocity that elicited the maximal oxygen uptake; IT_{DJ9}, interval drop-jumping at 9 drop-jumps per 15-s; IT_{DJ7}, interval drop-jumping at 7 drop-jumps per 15-s. † indicates significant difference in IT_{RUN} compared to IT_{DJ7} and IT_{DJ9} during exercise and on the mean data ($p < 0.001$). No significant difference was found between IT_{DJ7} and IT_{DJ9}.

Table 2. Effects of interval running and drop-jumping on the neuromuscular function.

	IT _{RUN}		IT _{DJ7}		IT _{DJ9}	
	Baseline	Post-exercise	Baseline	Post-exercise	Baseline	Post-exercise
MVC, N	598 ± 137	559 ± 127 *	581 ± 138	547 ± 125*	594 ± 147	558 ± 141*
Δ%		-6 ± 7		-5 ± 7		-6 ± 5
VA, %	87 ± 10	77 ± 12 *	87 ± 7	74 ± 10 *	87 ± 9	74 ± 11 *
Δ%		-12 ± 7		-15 ± 9		-15 ± 5
QT _{single} , N	204 ± 37	187 ± 34 *	198 ± 34	170 ± 37 *†	204 ± 38	170 ± 33 *†
Δ%		-8 ± 7		-14 ± 8 †		-17 ± 9 †
QT ₁₀ , N	291 ± 60	242 ± 51 *	282 ± 62	216 ± 62 *†	293 ± 62	217 ± 53 *†
Δ%		-17 ± 6		-24 ± 11 †		-26 ± 9 †
QT ₁₀₀ , N	262 ± 45	259 ± 48	260 ± 50	252 ± 57	263 ± 54	243 ± 45 *†
Δ%		-2 ± 6		-4 ± 9		-7 ± 9
QT _{10:100} , N	1.11 ± 0.11	0.94 ± 0.12 *	1.09 ± 0.11	0.86 ± 0.13 *†	1.12 ± 0.09	0.89 ± 0.12 *†
Δ%		-15 ± 6		-21 ± 7 †		-20 ± 6†
CT, ms	114 ± 4	109 ± 3 *	114 ± 4	110 ± 4 *	114 ± 3	109 ± 4 *
Δ%		-4 ± 2		-4 ± 2		-4 ± 2
MRFD, N.ms ⁻¹	1.8 ± 0.3	1.7 ± 0.3	1.7 ± 0.1	1.6 ± 0.3 *†	1.8 ± 0.3	1.6 ± 0.3 *†
Δ%		-4 ± 7		-11 ± 8 †		-13 ± 9 †
HRT, ms	80 ± 27	46 ± 9 *	74 ± 28	43 ± 7 *	77 ± 29	44 ± 7 *
Δ%		-40 ± 12		-37 ± 16		-38 ± 16
VL M _{MAX} , mV	13.8 ± 4.2	14.2 ± 4.7	13.3 ± 4.5	13.6 ± 4.2	13.6 ± 4.3	13.8 ± 4.7
Δ%		2 ± 6		4 ± 8		1 ± 8
VM M _{MAX} , mV	17.4 ± 4.3	17.0 ± 3.7	16.8 ± 4.0	15.7 ± 3.5	17.0 ± 3.9	16.0 ± 4.3
Δ%		-2 ± 6		-7 ± 5		-7 ± 7
RF M _{MAX} , mV	5.4 ± 1.6	5.2 ± 1.7 *	5.7 ± 1.4	5.6 ± 1.3	5.5 ± 1.3	5.2 ± 1.3*
Δ%		-3 ± 5		-1 ± 6		-6 ± 8 ‡

IT_{RUN}, high intensity interval running at 120% of the velocity that elicited the maximal oxygen uptake; IT_{DJ9}, interval drop-jumping at 9 drop-jumps per 15 s; IT_{DJ7}, interval drop-jumping at 7 drop-jumps per 15 s; MVC, maximal voluntary isometric contraction; VA, voluntary activation of the quadriceps; QT_{single}, QT₁₀ and QT₁₀₀ represent the potentiated quadriceps twitch evoked by single, 10 Hz-paired and 100 Hz-paired electrical stimulation of the femoral nerve, respectively; QT_{10:100}, low-frequency fatigue ratio (QT₁₀ / QT₁₀₀); MRFD, maximal rate of force development; CT, contraction time; HRT, half relaxation time; M_{MAX}, maximal amplitude of the compound muscle action potential; VL, *vastus lateralis*; VM, *vastus medialis*; RF, *rectus femoris*; Δ%, Δ percentage change from baseline. Post-exercise values corresponded to the average of the data measured from 30 s through 6 min after the end of exercise. * Indicates significant difference from baseline measurements ($p < 0.01$); † Indicates significant difference from IT_{RUN} ($p < 0.05$); ‡ Indicates significant difference from IT_{DJ7} ($p < 0.05$);

Figure 5 (left). Percent change in peripheral fatigue indices following interval running and drop-jumping.

Data are presented as mean ± SE. Post-exercise values were measured from 30-s through 6-min after the end of exercise. QT_{single}, QT₁₀ and QT₁₀₀ represent the potentiated quadriceps twitch evoked by single, 10 Hz-paired and 100 Hz-paired electrical stimulation of the femoral nerve, respectively. QT_{10:100}, low-frequency fatigue ratio (QT₁₀ / QT₁₀₀); IT_{RUN}, high intensity interval running at 120% of the velocity that elicited the maximal oxygen uptake; IT_{DJ9}, interval drop-jumping at 9 drop-jumps per 15-s; IT_{DJ7}, interval drop-jumping at 7 drop-jumps per 15-s. * indicates significant difference compared to the post-exercise value measured at 30-s; † indicates significant difference compared to IT_{RUN} ($p < 0.05$). Note that exercise-induced reductions in QT₁₀₀ were not significantly different from baseline following IT_{RUN} and IT_{DJ7}.

Following IT_{RUN} and IT_{DJs}, ΔQT₁₀ and ΔQT_{10:100} significantly decreased during the post-exercise recovery period ($p=0.002$). Similar reduction during recovery were found in ΔQT_{single} for IT_{DJ7} and IT_{DJ9} only ($p<0.001$).

Mechanical performance during interval drop-jumping. No difference between IT_{DJ7} and IT_{DJ9} ($p=0.08$, $\eta^2=0.11$) were found for the ground contact time, power output, jump height and the reactive strength index (Figure 6). No time effect was also found for ground contact time and power output ($p=0.09$, $\eta^2<0.10$). A significant time effect was found for reactive strength index ($p=0.01$, $\eta^2=0.14$) and jump height ($p=0.04$, $\eta^2=0.12$) but post-hoc analysis did not reveal a significant difference between the first and the following datapoints, suggesting that drop-jumping performance was unaltered over time.

Rate of perceived exertion. During IT_{RUN} and IT_{DJ9}, RPE increased linearly throughout exercise, from 1.3 ± 0.9 and 1.4 ± 1.0 to 6.4 ± 2.2 and 6.8 ± 2.0 , respectively. No difference was

found between conditions ($p=0.80$). During, IT_{DJ7} , RPE also increased linearly (from 1.4 ± 1.1 to 4.2 ± 1.4) but remained lower ($p=0.03$) than IT_{DJ9} and IT_{RUN} from the 3rd to the last work bout.

DISCUSSION

Our findings showed that an 11-min bout of interval drop-jumping at 9 drop-jumps per 15-s, elicited $\tau\dot{V}O_{2-MAX}$ that was not different than high-intensity interval running. Reducing the work rate from 9 to 7 drop-jumps per 15-s, significantly decreased the $\dot{V}O_2$ response to exercise. Quadriceps EMG and exercise-induced neuromuscular fatigue were higher during interval drop-jumping compared to interval running, indicating that the neuromuscular system was activated and stimulated to a higher extent during interval drop-jumping. This greater stimulation of the neuromuscular system did not however compromise drop-jump performance during interval drop-jumping. Our results therefore confirmed our hypotheses and suggest that interval drop-jumping at a high work rate (i.e. 9 drop-jumps per 15-s) might be an effective method to produce concomitant cardioventilatory and neuromuscular adaptations, which is particularly relevant to many sports requiring both endurance and muscle power capabilities.

Effect of interval running and drop-jumping on the time spent at $\dot{V}O_{2-MAX}$.

Our results showed that gas exchange and cardioventilatory responses to exercise during IT_{DJ9} was not different than IT_{RUN} (Fig. 2 and 3). Moreover, no significant difference in $\tau\dot{V}O_{2-MAX}$, a key determinant of $\dot{V}O_{2-MAX}$ improvement with training^{12,13,38,39}, was found between IT_{DJ9} and IT_{RUN} . Our findings therefore indicate that, the repetition of 192 drop jumps – a training method commonly used during physical training to improve explosive performance³⁻⁵ –, was effective when performed at a work rate of 9 jumps per 15-s to stimulate the cardiorespiratory and oxydative systems to levels that are known to produce long term positive adaptations with training^{12,13,38,39}. Our results extend previous findings from Brown *et al.*⁹, which showed that participants reached 83% of $\dot{V}O_{2-MAX}$ during eight series of ten drop-jumps (height: 80 cm), with three minutes of passive recovery between series. Our findings showing that $\tau\dot{V}O_{2-MAX}$ was greatly improved in IT_{DJ9} and $IT_{DJ9-ISO WORK}$ compared to IT_{DJ7} indicate that the metabolic and cardioventilatory response to repeated drop-jumps is critically dependent on the work rate. Therefore, the improved $\dot{V}O_2$ response in our study compared to the abovementioned study is likely due to 1) the shorter recovery duration between work bouts (i.e. 15-s vs. 3-min) and 2) a higher number of jumps per minute, which contributed to increase the work rate and prevent a fall in $\dot{V}O_2$ during recovery (Fig. 2).

Our results showed that, despite similar work / recovery intensity and duration, $\tau\dot{V}O_{2-MAX}$ in IT_{RUN} was less than previously reported by Dupont *et al.* (145 ± 76 s vs 323 ± 172 s)²⁷. Differences in the warm-up protocol (with vs without), the exercise termination modality (exhaustion vs eleven minutes) and in the running surface (track vs treadmill) likely explain the discrepancies between Dupont *et al.*²⁷ and our study, respectively.

Figure 6. Ground contact time, power output, jump height and reactive strength index measured during interval drop-jumping at different jump frequencies.

Data are presented as mean $\pm$ SE. Ground contact time was measured during each drop-jump and averaged for each work bout. Power output, jump height and reactive strength index were measured during the last drop-jump of each work bout. IT_{DJ9} , interval drop-jumping at 9 drop-jumps per 15-s ; IT_{DJ7} , interval drop-jumping at 7 drop-jumps per 15-s . Note that no significant alteration in performance over time and no significant difference between conditions were found.

Effect of interval running and drop-jumping on exercise-induced neuromuscular fatigue

Our results showed that quadriceps force was significantly impaired after IT_{RUN} and IT_{DJs} (Fig. 5). The exercise-induced reductions in potentiated twitch force as well as in voluntary activation suggest that the reduction in MVC peak force was caused by the alteration of processes within the working muscles (*i.e.* peripheral fatigue) and within the central nervous system (*i.e.* central fatigue)^{24,25}.

Absence of exercise-induced reductions in VL and VM M_{MAX} indicates that the reduced potentiated twitch force following exercise was unlikely related to a reduced membrane excitability⁴⁰. In contrast, the decrease in $\Delta QT_{10:100}$ indicates that the main cause of peripheral fatigue was likely a failure of the excitation-contraction coupling within the working muscles⁴¹. Moreover, the absence of potentiated twitch force recovery following ITs suggest that the observed peripheral fatigue was not mainly attributable to metabolic disturbances in energy-rich phosphates and pH – which are readily reversible⁴². Rather, the relatively preserved ΔQT_{100} associated with the progressive reduction in ΔQT_{10} and $\Delta QT_{10:100}$ during the recovery period (Fig. 5) suggest that mechanisms related to prolonged low-frequency force depression (*e.g.* free radicals accumulation and/or muscle damage) have mainly contributed to the observed failure of the excitation-contraction coupling^{33,43}. The absence of any increase in the ground contact time or any reduction in power output, jump height and reactive strength index during IT_{DJs} , suggest however that the exercise-induced fatigue was not sufficient to compromise drop-jumping performance. In contrast, a ~80% and ~30 % reduction in the potentiated quadriceps twitch force evoked with low and high frequency doublets were found following a series of 100 drop jumps at a 50-cm drop height (vs. 22% and 7% in the present study)⁴⁴. This was associated with a ~12 % reduction in jump height that persisted for at least 3 days. The much larger reduction in the evoked force by low frequency doublets and in the low frequency fatigue ratio in the above-mentioned study (corresponding to QT_{10} and $QT_{10:100}$ in the present study, respectively) suggests that the higher drop height significantly increased prolonged low frequency fatigue and muscle damages^{44,45}, therefore compromising performance.

The greater reduction in potentiated twitch force after IT_{DJs} compared to IT_{RUN} coincided with a 25 to 45% higher EMG amplitude (Fig. 4) – indicative of a higher muscle activation⁴⁶, as well as a larger decrease in $\Delta QT_{10:100}$. We thus interpret these findings to indicate that the increased ‘neural’ drive to the working muscles during drop-jumping compared to running likely elicited the recruitment and the subsequent fatigue of a larger number of the highly fatigable fast-twitch motor units⁴⁷. Moreover, given the greater reduction in $\Delta QT_{10:100}$ after IT_{DJs} compared to IT_{RUN} , the recruited motor units were more sensitive to prolonged low-frequency force depression following IT_{DJs} .

Both running and drop-jumping involve the activation and the contraction of different muscles groups (*e.g.* the plantar flexors)⁴⁸ which might be activated and fatigue differently than the quadriceps during interval running and drop-jumping. The absence of reduction in drop jump performance indices during IT_{DJs} suggest however that the net fatigue effect of the involved locomotor muscles was not sufficient to compromise the participant’s drop-jumping capabilities. Alternatively, the coordination of these locomotor muscles might have been

adapted by the central nervous system in response to fatigue development in the quadriceps in order to preserve drop jumping performance⁴⁹.

Practical Applications

Our results showed that interval drop-jumping at a work rate corresponding to 9 drop-jumps per 15-s is a suitable exercise to elicit and spend time above 90% of $\dot{V}O_{2-MAX}$, a threshold beyond which major cardiorespiratory and oxidative adaptations are thought to occur^{e.g., 12,13,38,39}. In addition, we found that a high volume of drop-jumps ($n = 198$ in IT_{DJs}) can be performed within a short period of time (11 min) without compromising power output, ground contact time (which remained well below 260-ms^{15,16}), jump height and the reactive strength index throughout exercise (Fig. 6). Because a high volume of drop jumps (*i.e.* 120 or above) and a high level of power output are prerequisites for optimized plyometric training effects¹⁴⁻¹⁶, these findings suggest that explosive and reactive strength might also be enhanced following 11 minutes of interval drop-jumping. Finally, the higher degree of peripheral fatigue and quadriceps EMG found after IT_{DJs} showed that the neuromuscular system was activated and stimulated to a greater extent compared to interval running. Thus, interval drop-jumping may have complementary training effects – *e.g.* increase in $\dot{V}O_{2-MAX}$, $v\dot{V}O_{2-MAX}$, explosive and reactive strength, jump height – that would benefit performance in sports requiring both endurance and muscle power (*e.g.* team sports, racket sports, mid-distance runners, etc.). Further research on the chronic effects of interval drop-jumping is however warranted to confirm this hypothesis.

CONCLUSION

Our results showed that interval drop-jumping allowed participants to spend a significant amount of time at $\dot{V}O_{2-MAX}$ and elicited peripheral fatigue without compromising drop-jumping performance, which are key determinants of oxidative, cardioventilatory and neuromuscular adaptations to training. A high work rate (*i.e.* at least 9 jumps per 15-s) and a large amount of work (*i.e.* ~200 drop-jumps) is however required to achieve a similar metabolic demand during interval drop-jumping compared to high intensity interval running. Together our findings suggest that interval drop-jumping might be a relevant training method to combine endurance and muscle power enhancements in a minimum amount of time, therefore improving time-efficiency during physical training.

Additional information

Competing interest

The authors have no conflicting interests.

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