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# Detection of the conformational changes of *Discosoma* red fluorescent proteins adhered on silver nanoparticles-based nanocomposites via surface-enhanced Raman scattering

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## Abstract

Description of the relationship between protein structure and function remains a primary focus in molecular biology, biochemistry, protein engineering and bioelectronics. Moreover, the investigation of the protein conformational changes after adhesion and dehydration is of importance to tackle problems related to the interaction of proteins with solid surfaces. In this paper the conformational changes of wild-type *Discosoma* recombinant red fluorescent proteins (DsRed) adhered on silver nanoparticles (AgNPs)-based nanocomposites are explored via surface-enhanced Raman scattering (SERS). Originality in the present approach is to work on dehydrated DsRed thin protein layers in link with natural conditions during drying. To enable the SERS effect, plasmonic substrates consisting of a single layer of AgNPs encapsulated by an ultra-thin silica cover layer were elaborated by plasma process. The achieved enhancement of the electromagnetic field in the vicinity of the AgNPs is as high as  $10^5$ . This very strong enhancement factor allowed detecting Raman signals from discontinuous layers of DsRed issued from solution with protein concentration of only 80 nM. Three different conformations of the DsRed proteins after adhesion and dehydration on the plasmonic substrates were identified. It was found that the DsRed chromophore structure of the adsorbed proteins undergoes optically assisted chemical transformations when interacting with the optical beam, which leads to reversible transitions between the three different conformations. The proposed time-evolution scenario endorses the dynamical character of the relationship between protein structure and function. It also confirms that the conformational changes of proteins with strong internal coherence, like DsRed proteins, are reversible.

Keywords: silver nanoparticles, plasma deposition process, plasmonic substrate, surface-enhanced Raman scattering, *Discosoma* red-fluorescent protein DsRed, protein conformation

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## 1. Introduction

Proteins represent an important class of biomolecules underpinning every reaction occurring in living organisms [1]. Recent advances in biotechnology enlarged the possibilities to explore their structural and functional properties. The potential use of proteins in newly created niche applications like biosensors, bioelectronics, photosensitizers, drug screening systems, and artificial implants among others [2–7], determines the intensive research on the relationship between protein structure and function promoting the release of more than 3000 scientific articles on protein biosensors and no less than 300 articles on protein bioelectronics in the last three years only [8].

Regardless the targeted application, the current strategies on revealing the relationship between protein structure and function lead to exposure and interaction of proteins with non-biological organic and inorganic solid surfaces [9, 10]. Proper description of the underlying mechanisms will certainly unveil the fundamental protein-adsorption problem and add value to the effort of record and quantification of the conformational changes of the protein native state when interacting with solid surfaces. To that end the application of physics-based diagnostic methods is suitable and highly demanded.

Raman spectroscopy appears the most frequently used method for the study of biological systems. However, to tackle the sensitivity limitations of Raman spectroscopy imposed by the small Raman cross sections, the biological systems should be coupled with metallic nanostructures. The scattering efficiency can be thus increased by several orders of magnitude [11] due to the activation of localized surface plasmon resonance (LSPR) that induces strong enhancement of the electromagnetic (EM) field in the vicinity of the metallic surface. This enables to largely extend the application of Raman spectroscopy in molecular spectroscopy, biomolecule recognition, and ultra-sensitive analysis, down to a single molecule [12–15]. Besides the sensing properties, the strong EM enhancement can be exploited to probe protein conformational changes under photoexcitation, including real-time monitoring [16–18]. Therefore, since its discovery in the late 70 s [19, 20], the Surface-Enhanced Raman Scattering (SERS) has proven to be a very powerful and reliable analytical tool for chemo- and bio-sensing [21–23], due to the strong enhancement of the vibrational signatures of analytes in different chemical environments [12–14].

In this context, a lot of resources and time have been employed in the effort to develop plasmonic substrates based on metallic nanostructures aiming at a further increase of the EM enhancement for the realization of noninvasive, highly-sensitive, and large-scale optical sensors [17, 24, 25]. A large variety of metallic nanostructure morphologies and arrangements (nanosphere, nanotriangles, nanodisks, nanorods,

nanocubes, etc) and different coupling geometries (dimers, trimers, arrays, etc) have been developed up to date for SERS platforms [16, 26–29]. However, their conversion to macroscopic plasmonic substrates relies generally on the NPs volunteer arrangement on dielectric surfaces (mainly through applying chemical methods), thus often resulting in non-uniform distribution on large areas, without a well-defined control of the spacing between the metallic nanostructures and the probed molecules, high point-to-point variability, scarce reproducibility and stability under irradiation conditions (due to photothermal and photodegradation processes) [30]. To overcome the limitations in producing solid SERS substrates various physical approaches, like thermal evaporation [31], combined nanoimprint lithography-shadow evaporation [32], gas aggregation source (GAS) [33], pulsed laser deposition [34], low-energy ion beam synthesis [35–37], and plasma-based deposition processes [38, 39], have been proposed in the literature.

It is generally acknowledged that the silver nanoparticles (AgNPs) realize the best nanoscale antenna in the visible range for amplifying local electronic and vibrational signals, thus providing unique molecular information in the optical far-field regime. Indeed, compared to gold nanoparticles, the AgNPs offer the advantage of stronger plasmonic enhancement because of lower interference between intraband and interband electronic transitions [40]. Accordingly, the SERS substrates based on AgNPs provide excellent way to study complex biological systems and in particular appear very well adapted for quantification of the conformational changes of proteins brought in contact with solid surfaces [17, 18, 21]. Moreover, the use of AgNPs covers another aspect of the relationship between protein structure and function which concerns the biological activity of the AgNPs. Because of their antimicrobial properties, the AgNPs have the potential to impact human health and environment [41–45]. The biological activity of AgNPs goes both ways, through the activity of ionic silver ( $\text{Ag}^+$ ) and through direct contact with the AgNPs resulting in protein denaturation at different cell locations; specifically sensible are those enzymes of the respiratory chain and transport channels [46]. Therefore, there exists a recognized need to address the relationship between protein structure and function from two distinctly different vantage points: (i) quantification of the conformational changes of proteins by using the antenna effect of AgNPs and (ii) analysis of the conformational changes of proteins induced by the AgNPs extreme chemical and biological activities.

The intent of this work is to bring additional insight into the mechanisms of adsorption of proteins on solid surfaces through quantification of the conformational changes of proteins adhered on AgNPs-based nanocomposites via SERS. We focus on the wild-type *Discosoma* recombinant red fluorescent protein (DsRed) [47], belonging to the family of

naturally fluorescent proteins (FPs). The strong interest toward the FP family originates from their application in molecular biology as reporters of gene expression, as non-invasive markers in molecular biology and other singular events of cell activity [2]. Potential use of the FPs extends toward bioelectronics and protein engineering for tissue regeneration, therapeutics, and nanotechnology [48–51]. The most widely characterized member of this family is the green fluorescent protein (GFP). The lately cloned from reef coral *Discosoma* sp. DsRed protein possesses the longest yet reported, for a wild-type spontaneously FP, excitation and emission maxima at 558 nm and 583 nm, respectively [47]. Owing to its high fluorescence yield the red fluorescent DsRed protein has become important both as a model for understanding FPs and as a tool for biomedical research. The DsRed protein and its engineered derivatives have found broad use in cell and molecular biology including fluorescence microscopy as a marker, fluorescence correlation spectroscopy and fluorescence activated cell sorting. Recently, the DsRed was found suitable for rational design of ultra-stable and reversible photoswitches for super-resolution imaging [52]. Moreover, it has been hypothesized that FPs from reef-building corals operate as part of an adaptive mechanism to optically interact and to regulate the symbiotic relationship between corals and photosynthetic algae [53]. Structural rearrangements near the chromophore influence the maturation speed and brightness of the DsRed variants. It is therefore essential to examine the conformational transitions that affect the protein's ability to transfer optical excitation energy [54].

Studies of the conformational changes of DsRed protein have been reported in the literature [55–57] but the DsRed Raman fingerprints were investigated only by recurring to chemically synthesized model chromophores [55, 56]. However, the later differ from the wild-type DsRed protein for the absence of the  $\alpha$ -helix and  $\beta$ -sheets that naturally surround the chromophore and for the different extensions of the conjugated  $\pi$ -system. The choice of chemically synthesized model chromophores is explained by the complications brought by the presence of immature green species in the solution created as a photoproduct of the red ones [55–57], thus often resulting in an unclear or incomplete band assignment. The novelty of this work lays down the point that we work with the wild-type DsRed protein in its native state and not with DsRed model chromophore. All reported experimental studies in the literature were performed in solution. No information on the DsRed protein structural and conformational changes can be found when the DsRed protein is adhered on a solid substrate and irradiated by light.

The lack of information on the above discussed issues motivated this study focusing on the investigation of the interaction of wild-type DsRed proteins with AgNPs-based plasmonic substrates. Our approach involves analysis of dehydrated DsRed protein layers in link with natural conditions during drying. To perform the SERS study on the conformational changes of DsRed proteins adhered on AgNPs-based nanocomposites we have elaborated, by plasma process, highly uniform and reproducible plasmonic

substrates composed of a single layer of AgNPs coated by a silica layer [38]. Focus was made on the possibility to well control, on a large scale, the AgNPs size distribution and interparticle distances. The resulting uniformity of hot-spot distribution guarantees the reproducibility and stability of this plasmonic sensor. Subsequently, we show how the enhanced EM field in the vicinity of the AgNPs could be employed to detect the presence and identify the conformational changes of proteins, adsorbed and adhered to the plasmonic substrate, during optical irradiation.

## 2. Materials and methods

### 2.1. Proteins

The DsRed fluorescent protein was purchased from Biovision. According to the SDS-PAGE, the recombinant DsRed was at least 97% pure and in a freeze-dried form. A DsRed stock solution of  $0.1 \text{ g l}^{-1}$  was prepared in water for injectable preparations (PPI water). Aliquots of DsRed stock solution were diluted 1–10 times into PPI water. The pH-value of the DsRed stock solution was measured to 6.6 and its stability was continuously monitored during the measurements. The assays were performed at room temperature ( $23 \text{ }^\circ\text{C}$ ).

### 2.2. Gas precursors and substrates

The hexamethyldisiloxane (HMDSO,  $\text{Si}_2\text{O}(\text{CH}_3)_6$ ) used as precursor in the plasma polymerization process was purchased from Sigma Aldrich with purity greater than 99.5% while the argon and oxygen gases were purchased from AirLiquid AlphaGaz 2 with a purity of 99.9995%. The silver target used for sputtering was more than 99.99% pure, and was purchased from Inland Europe. The quartz substrates ( $25 \times 25 \times 1 \text{ mm}$ ) were purchased from Oxford Instruments. The silicon substrates (intrinsic, resistivity  $R > 200 \text{ } \Omega\text{cm}$ ) were purchased from Sil'tronix.

### 2.3. Plasma deposition process for synthesis of SERS active delta-layer of AgNPs embedded in silica host matrix

The targeted AgNPs-based nanocomposites were elaborated in a plasma process that successfully combines in the same reactor silver sputtering for the deposition of AgNPs and plasma enhanced chemical vapor deposition for the deposition of the plasma silica cover layer. This approach, offers several advantages compared to other deposition techniques: (i) possibility to obtain metallic concentrations from a few percent up to 100%, (ii) homogeneous dispersion of the metal nanoparticles, and (iii) fine control over the size of the metal nanoparticles. The plasma was sustained in an axially-asymmetric capacitively-coupled radio-frequency (RF,  $f = 13.56 \text{ MHz}$ ) discharge at low gas pressure (a few Pa) [58]. The RF-driven top electrode was smaller, made of silver to bear the sputtering. The bottom electrode, which is also the substrate holder, and the walls were grounded. This RF-discharge produces axially-asymmetric plasma inducing a self-bias voltage ( $V_{dc}$ ) on the powered electrode. The self-bias voltage (negative in this case) results from

the DC voltage drop between the bulk plasma and the electrodes across the plasma sheaths connecting the driven electrode to the ground. It is at the origin of the acceleration of argon ions towards the Ag-target to achieve sputtering. The plasma behavior during the deposition was controlled by optical emission spectroscopy through the line ratio of a silver and an argon lines:  $I_{\text{Ag}(546.6\text{ nm})}/I_{\text{Ar}(549.6\text{ nm})}$ . This ratio indeed gives an image of the Ag-amount in the plasma, which can be related to the deposited Ag-volume fraction [58]. Moreover, the self-bias voltage, reflecting the plasma stability, was continuously measured. The used plasma process is suitable for large scale technology transfer and fully compatible with standard microelectronic technologies.

Prior to deposition, the quartz and/or silicon substrates covered by a 80 nm thick layer of thermal SiO<sub>2</sub> were cleaned in Piranha solution for 2 min and then rinsed with deionized water until attaining zero conductivity. The delta-layer of AgNPs was deposited by Ag-sputtering in an Ar-discharge maintained at low gas pressure ( $p_{\text{Ar}} = 5.2\text{ Pa}$ ) and power of  $P = 80\text{ W}$ . The induced self-bias voltage was of  $V_{\text{dc}} = -950\text{ V}$ . The sputtering time was set to  $t_s = 5\text{ s}$ . The plasma silica (SiO<sub>2</sub>) cover layer embedding the AgNPs was deposited in the same reactor in the plasma sustained in a gas mixture of argon (Ar flow: 2.8 sccm, where sccm stands for standard cubic centimeters per minute at standard temperature and pressure), HMDSO and oxygen (O<sub>2</sub> flow: 1.25 sccm) at total gas pressure of  $p_{\text{tot}} = 7.68\text{ Pa}$ . A strong particularity of the used plasma process which makes it original and highly efficient is the pulsed injection of the precursor. The HMDSO was introduced in the discharge by pulses with period  $T = 5\text{ s}$  ( $T = t_{\text{on}} + t_{\text{off}}$ ) and injection time  $t_{\text{on}} = 3.1\text{ s}$ , giving an average flow of 0.25 sccm. The injected RF power for the SiO<sub>2</sub> plasma deposition was fixed at 120 W giving a self-bias voltage of  $V_{\text{dc}} = -880\text{ V}$ . The thickness of the SiO<sub>2</sub> plasma cover layer was controlled by the deposition time, fixed at 30 s for this study. More details about the plasma process, plasma properties and the resulting AgNPs delta layers covered by plasma silica layers, in relation with their structural characterization and optical response, are provided elsewhere [38, 39, 58, 59].

#### 2.4. Optical and morphological characterization of the plasmonic substrates

Optical transmittance spectra were recorded using a Hewlett Packard HP8452A Diode Array Spectrophotometer in the UV-vis-NIR range (190–820 nm) to obtain the position of the AgNPs LSPR resonance.

High resolution transmission electron microscopy (HRTEM) imaging of the plasmonic substrates was performed using a cold field emission gun Hitachi HF 3300 C microscope operating at 300 kV equipped with a spherical aberration corrector. To achieve observation, specimens transparent to electrons have been prepared in accordance with the standard procedure, i.e. mechanical polishing and Ar<sup>+</sup> ion milling in both cross-section and plan view configurations. The former configuration is used for the accurate measurement of the position of AgNPs with respect to the

surface while the later allows measurement of the total Ag-amount contained within the NPs (deduced from their size-distribution and surface density).

#### 2.5. Synthesis of dehydrated DsRed thin layers on the plasmonic substrates

DsRed thin protein layers deposited on the AgNPs-based nanocomposites surfaces were realized by a dip coating process. The substrates, with a fixed superficial area of  $1 \times 1\text{ cm}^2$ , were immersed for 1 h in 1.0 ml protein solutions. After immersion, the samples were rinsed with PPI water to remove the non-adhered proteins and left dehydrating at room temperature and atmospheric pressure. Thin DsRed dehydrated layers resulting from different DsRed solution concentrations, starting from  $0.01\text{ g l}^{-1}$  (80 nM) up to the highest possible in this study one of  $0.1\text{ g l}^{-1}$  (800 nM) were investigated.

#### 2.6. Optical characterization of the dehydrated DsRed protein layers

The thickness and the optical parameters (refractive index and extinction coefficient) of the dehydrated DsRed protein layers deposited on quartz substrates were determined by spectroscopic ellipsometry. A Semilab ellipsometer SE-2000 with a rotating polarizer and a fixed analyzer was used in the spectral range 250–850 nm. The simulations of the recorded spectra were performed with spectroscopic ellipsometry analyzer software provided by Semilab [60]. Lorentz method was used in the procedure as the DsRed is a weakly absorbing protein [61].

#### 2.7. Photoluminescence (PL) and Raman measurements

The confocal imaging and spectroscopy of the elastically scattered light and of the Raman scattering were carried out using a Jobin-Yvon XploRa setup. In all PL and Raman measurements, the laser beam was focused through a 50× objective to spot of size of  $2\text{ }\mu\text{m}^2$  on the freshly deposited protein layers. The PL was excited at 532 nm close to resonance with the DsRed absorption band. The Raman scattering was excited at 532, 638, and 785 nm. In order to avoid possible degradation of the proteins due to laser heating, the incident intensity was limited to 1% of its maximum value (of around 0.15 mW for the 532 and 638 nm excitations and 0.8 mW for the 785 nm excitation). The Raman spectra were recorded with an accumulation time of 30 s.

#### 2.8. Electrodynamic modeling of the AgNPs-based nanocomposites

FDTD method [62] was used to calculate the plasmonic properties (far- and near-field) of the SERS substrates. The calculations were performed by using geometrical parameters based on data extracted from the TEM images. The SERS substrates were simulated as composed of a bimodal NP distribution: (i) large ellipsoidal AgNPs with major axis of 19.6 nm, minor axis of 16.7 nm, density of  $0.8 \times 10^{11}\text{ NPs cm}^{-2}$  and an

average interparticle distance of 5.5 nm, and (ii) small spherical AgNPs with size distribution of  $3.0 \pm 2.0$  nm and density of  $2.0 \times 10^{11}$  NPs  $\text{cm}^{-2}$ . The AgNPs were taken embedded at 5.0 nm underneath the  $\text{SiO}_2$  cover layer. The dielectric permittivities tabulated by Palik have been used for Ag [63] and  $\text{SiO}_2$  [64]. We modeled a  $2 \times 2 \mu\text{m}^2$  AgNPs distribution and used periodic boundary conditions in the  $x$ - and  $y$ -directions to model an infinite substrate (perfectly-matched layers were taken along the  $z$ -direction). To accurately discretize the entire nanoparticle distribution the FDTD mesh size was fixed at 1 nm in all calculations. In order to investigate the optical properties of the NP distributions, we first calculate the absorption cross-section and near-field response at 532 nm. Calculations were performed with linearly-polarized light at normal and oblique ( $30^\circ$ ) incidence where the oblique incidence uses the broadband fixed angle source technique [65]. Convergence was obtained for a propagation time of  $\sim 90$  fs. In order to estimate the experimental SERS EM enhancement, we calculated the fourth power of the electric near-field ( $|E/E_0|^4$ ) [28–30].

### 2.9. Electronic structure calculations of the DsRed chromophore

The density functional theory (DFT/B3LYP) implemented into Gaussian 03 software package [66], was used to optimize the molecular geometry and to calculate the vibration mode frequencies of the DsRed chromophore. In these calculations, the used basis set (6–31 G\*\*) represents an extended base of the split-valence type. All calculations of the molecular geometries converged to a true energy minimum attested by the lack of vibrational frequencies. The assignment of the vibration modes was based on the visual inspection of the atomic displacements animated by graphical MOLDEN software [67]. The Raman spectra were plotted using a Lorentzian line shape with a full width at half maximum (FWHM) of  $10 \text{ cm}^{-1}$ . The visualization of the atom displacements in a given vibrational mode was made by using the MOLDEN software.

## 3. Results and discussion

### 3.1. AgNPs-based plasmonic substrates: structure and morphology

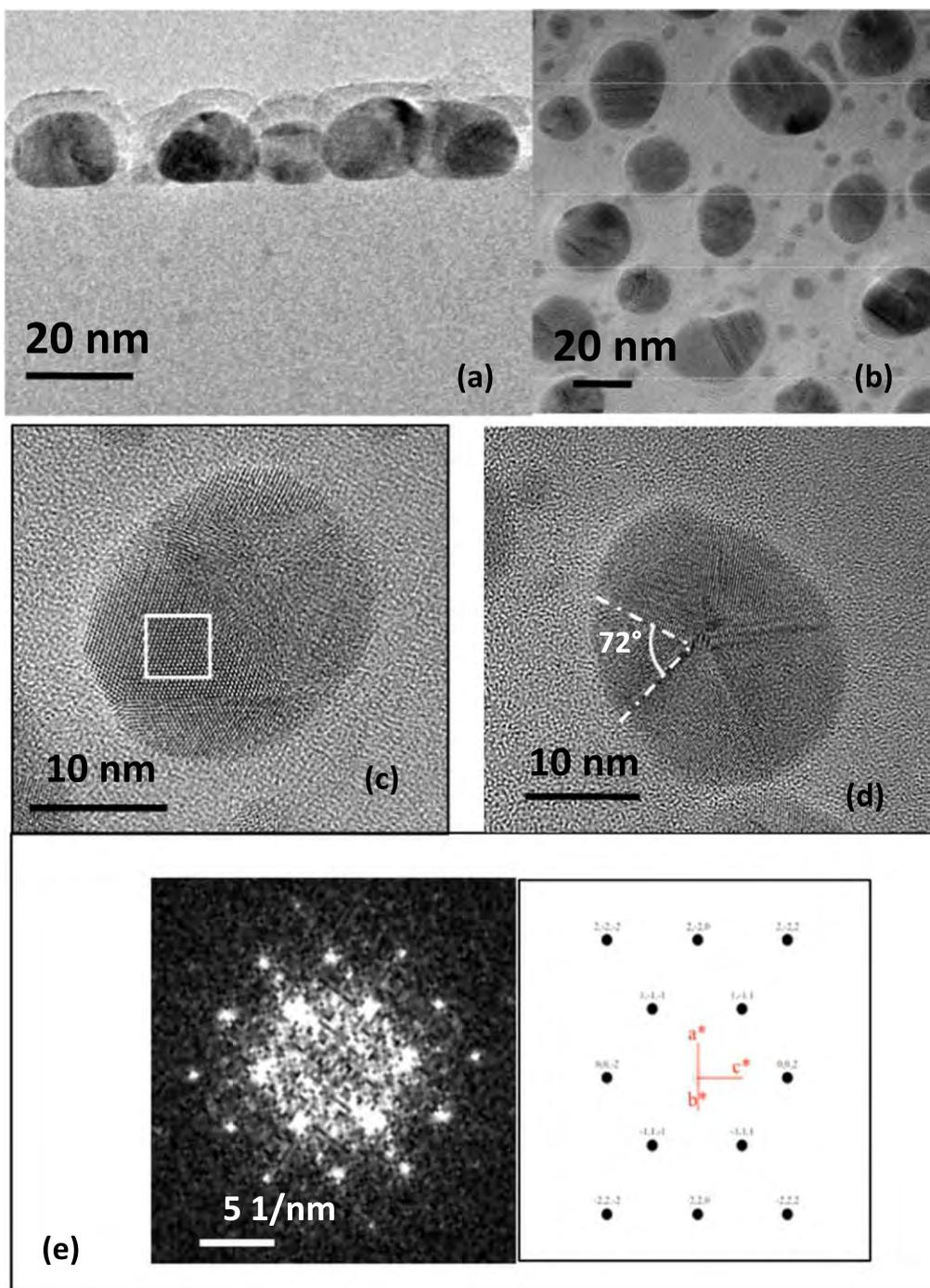
The specific architecture of plasmonic substrates used in the current study is based on a single layer of AgNPs deposited onto quartz substrates and coated by a plasma silica layer at a controlled nanometric distance from the free surface. Having the AgNPs not directly exposed to the surrounding environment presents several advantages. First, the silica cover layer acts as a barrier layer protecting the metallic silver against quick disappearance and/or premature aging, mainly through fast oxidation [68]. Second, it properly avoids the direct contact (i.e. chemisorption) of proteins with the AgNPs-active surface. This precaution limits the biological activity of AgNPs and prevents the DsRed proteins from denaturation and/or unfolding processes potentially related to the toxicity

of AgNPs [69, 70]. In addition, due to the presence of thin silica as dielectric spacer between the metal surface and the molecules (i.e. proteins) under study, the SERS is supplied mainly by the EM mechanism (based on ‘plasmon resonance’), strongly limiting the chemical one (based on ‘charge transfer’) [71].

The morphological analysis of the AgNPs-based plasmonic substrates has been performed by transmission electron microscopy (TEM). From the TEM cross-section views in figure 1(a), one can clearly notice that the AgNPs form a planar single layer. It is also possible to appreciate the thin silica cover layer that conformably envelops the AgNPs. Its thickness of 5.5 nm is compatible with the plasmonic near-field range [72], thus allowing to keep the SERS effect efficient. Moreover, from both the cross-section (figure 1(a)) and plan view (figure 1(b)) images one can see that most of the nanoparticles have prolate spheroidal shape. Their major axes are randomly-oriented on the substrate in the plane of the AgNPs delta-layer. Smaller nanoparticles are also detectable. They correspond to NPs issued from lately formed in the plasma Ag-clusters as the nucleation phase of AgNPs starts immediately after the Ag-atoms sputtering in the plasma gas-phase. The subsequent phases of aggregation and growth of AgNPs in the plasma lead to formation of larger in size AgNPs. Once the Ag-atoms/AgNPs reach the substrate surface their size increases through surface growth mechanisms powered by the increased kinetic energy of the sputtered Ag-atoms, the high surface diffusion of Ag, and most likely involving Ostwald ripening. The apparent shell surrounding the AgNPs, visible in figure 1(b), corresponds to the silica cover layer projection.

HRTEM observations (figures 1(c) and (d)) show that all the AgNPs (including the smallest ones) are polycrystalline and/or twinned. This is well explained by the AgNPs growth mechanisms in the plasma process that involve aggregation and sticking phases. The measured angles and interplanar distances (2.36, 2.04, and 1.44 Å) in the associated FFT (figure 1(e)), taken in the monocrystalline domain of the NP (figure 1(c)), perfectly fit ones of pure silver in the [110] zone axis. The NP shown in figure 1(d) is fivefold twinned one with the typical  $2\pi/5$  angle between each domain. Multiple twinned NP formation is, in general, favored in diamond and face-centered cubic crystals. Transition metal NPs like the AgNPs are thus ideal materials for fivefold twinning [73].

Statistical analysis performed on more than 500 AgNPs in the plan view image is reported in figure 2. The nanoparticles follow a bimodal distribution in size. The smaller NPs have major axis of  $5.1 \pm 1.7$  nm and minor axis of  $3.9 \pm 1.5$  nm, while the major and minor axes of the larger NPs are  $19.9 \pm 10.0$  nm and  $17.0 \pm 7.6$  nm, respectively (figure 2(a)). Information on the density of nanoparticles has also been extracted from the plan view image. The surface density of AgNPs is estimated to  $1.7 \times 10^{11}$  NPs  $\text{cm}^{-2}$ , corresponding to a covered area of 42.6%. The average edge-to-edge interparticle distance is 5.2 nm, with dispersion as large as 3.1 nm, as reported in figure 2(b). The evolution in shape of the AgNPs from spherical to prolate spheroid is well pronounced for the large AgNPs with the highest eccentricity



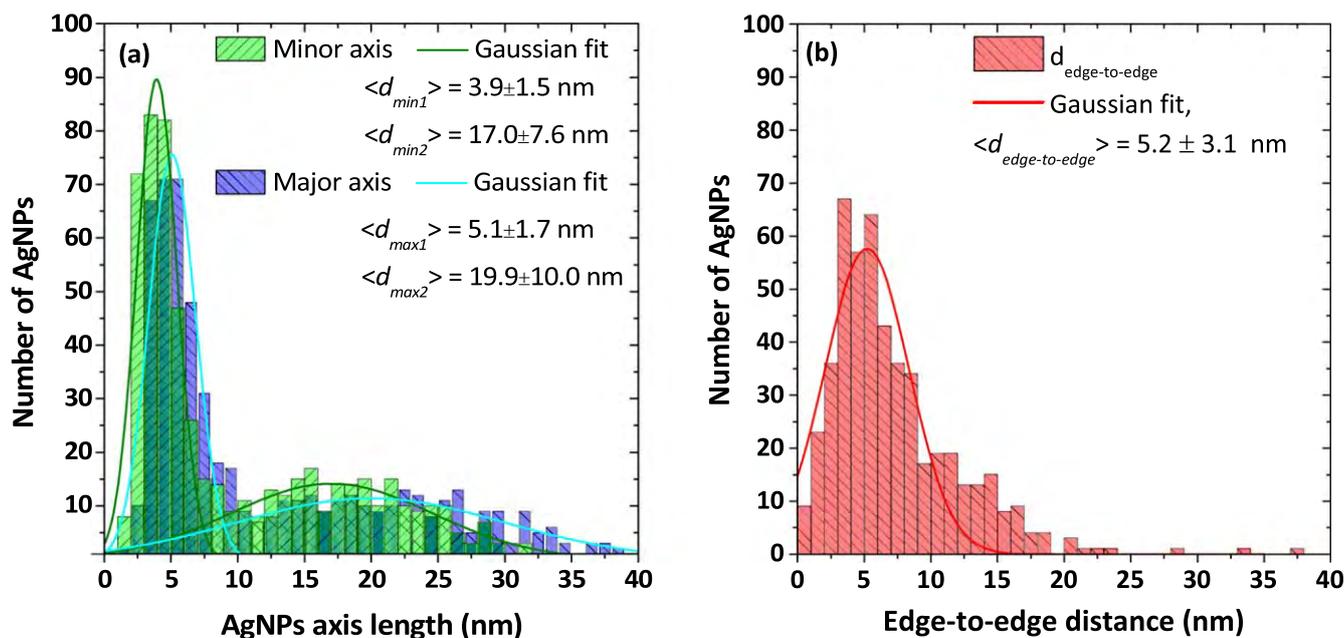
**Figure 1.** (a) Bright-field cross-sectional TEM image showing the single layer of AgNPs with their conformal 5.5 nm thick silica cover layer; (b) bright-field plan-view TEM image of the AgNPs; (c) HRTEM image of individual polycrystalline and (d) fivefold twinned NP; (e) FFT associated to the square region drawn in the HRTEM image. The measured distances and angles perfectly match the reciprocal space of Ag oriented in [110] zone axis.

found of  $\varepsilon = 0.52$ . The irregular shape of some of the AgNPs, where sharp edges can be observed, alongside with the formed assemblies of AgNPs allows for creation of hot spots, thereby promoting the EM field enhancement.

### 3.2. DsRed protein layers: optical properties

Here, we focus on the optical properties of thin layers of DsRed proteins, whose chromophoric structure is reported in

figure 3(a) together with a scheme of the main electronic energy levels. Because of the strong interest in multicolor tagging and in fluorescence resonance energy transfer the optical properties of DsRed are widely investigated for *in vivo* and *in vitro* samples as a spectrally distinct companion of GFP [74]. However, very few reports on the PL properties of nanometric layer of dehydrated DsRed proteins are available [61, 75]. Thus, before going deeper into the study of the DsRed conformational changes through SERS effect we have



**Figure 2.** Statistical analysis performed on more than 500 AgNPs on the plan view image: (a) minor and major axes of the AgNPs. The continuous lines show the corresponding Gaussian fits; (b) edge-to-edge distance between the AgNPs and the corresponding Gaussian fit.

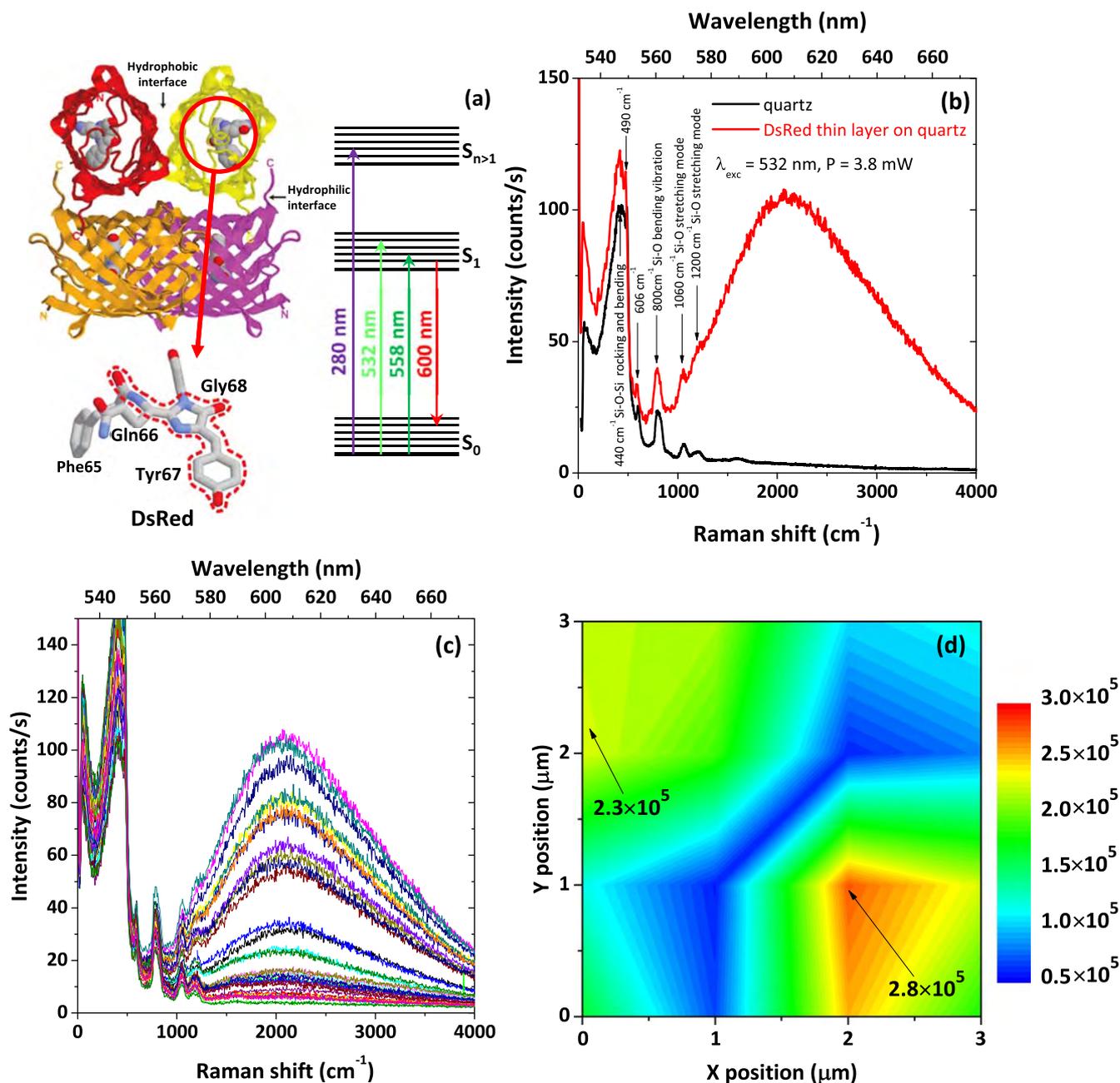
investigated the optical properties of a thin DsRed layer adhered and dehydrated on top of a pristine quartz substrate. The DsRed protein layer was deposited by dip coating process. For the PL study the DsRed layer was obtained from protein concentration in solution of  $0.1 \text{ g l}^{-1}$  (i.e. 800 nM). The resulting protein layer is thin, discontinuous, and composed mainly of DsRed monomers with some residues of dimers and tetramers. It has effective thickness of 3.7 nm and covers 35% of the substrate surface, as measured by spectroscopic ellipsometry [61].

The DsRed layer was irradiated with a 532 nm laser in resonance with the  $S_0$  to  $S_1$  transition (see energy diagram in figure 3(a)). Under this excitation, we observe a broad PL signal at about 600 nm, overlapped with sharp peaks at lower wavelengths (figure 3(b)). The PL band is ascribed to the recombination from the  $S_1$  level to the ground state. The red-shift from the PL emission of DsRed in solutions (583 nm) [47] is most likely due to modification/re-organization of the protein structure after adsorption onto the solid surface and subsequent dehydration. The presence of strong PL emission from the DsRed protein layer after dehydration indicates the absence of denaturation and unfolding processes of the proteins secondary structure or damages in the chromophore after interaction with the substrate solid surface. PL mapping over a  $3 \times 3 \mu\text{m}^2$  region with step size of  $0.5 \mu\text{m}$  has also been recorded to investigate the protein distribution on the surface. Some of the acquired PL spectra, as well as a map of the integrated PL intensity are reported in figures 3(c) and (d). Since the PL intensity is generally proportional to the number of emitting centers [76], and assuming that the non-radiative de-excitation mechanisms are the same for each protein in the layer, the variation in the PL intensity (figures 3(c) and (d)) can be considered to reflect the morphology of the DsRed thin layer. Indeed, the non-uniform PL emission is in agreement

with ellipsometry measurements showing formation of a discontinuous protein layer [61], for the studied case (protein concentration in solution  $0.1 \text{ g l}^{-1}$ ). Another essential aspect is that despite the clear observation of PL emission from the discontinuous DsRed layer, no Raman signal related to the proteins was detected. The only sharp peaks visible in figures 3(b) and (c) are due to the Raman scattering by the optical vibrational modes of the quartz substrate [77].

### 3.3. Interaction of DsRed proteins with AgNPs-based plasmonic substrates: optical response and SERS effect

The optical response of the AgNPs-based plasmonic substrates was measured by UV-visible transmission spectroscopy (figure 4(a), blue line). The LSPR peak of the AgNPs is observed at 454 nm with a FWHM of 110 nm. It is red-shifted compared to the LSPR of a single spherical AgNP in silica (410 nm, see supplementary information, available online at [stacks.iop.org/NANO/30/165101/mmedia](http://stacks.iop.org/NANO/30/165101/mmedia)), because of the elongated shape of the AgNPs and their mutual EM interaction [40, 78]. The absorption spectrum calculated by finite-difference time-domain (FDTD) [62] method for an infinite 2D-distribution of ellipsoidal NPs with size, shape, and spatial distributions in accordance with the experimentally obtained AgNPs is shown on figure 4(a), black line. The absorption peak of the calculated spectrum occurs at slightly shorter wavelengths (420 nm) as compared to the experimental LSPR (figure 4(a), blue line). Given the large number of parameters taken into account in the calculations this difference is most likely due to non-uniformity in size, irregularity in shape and AgNP density variations. The localized surface plasmon band of the ellipsoidal-NP distribution results from the spectral overlap of the multiple LSPRs coming from randomly-oriented ellipsoids and their size distribution. It can also be noticed that the substrates exhibit

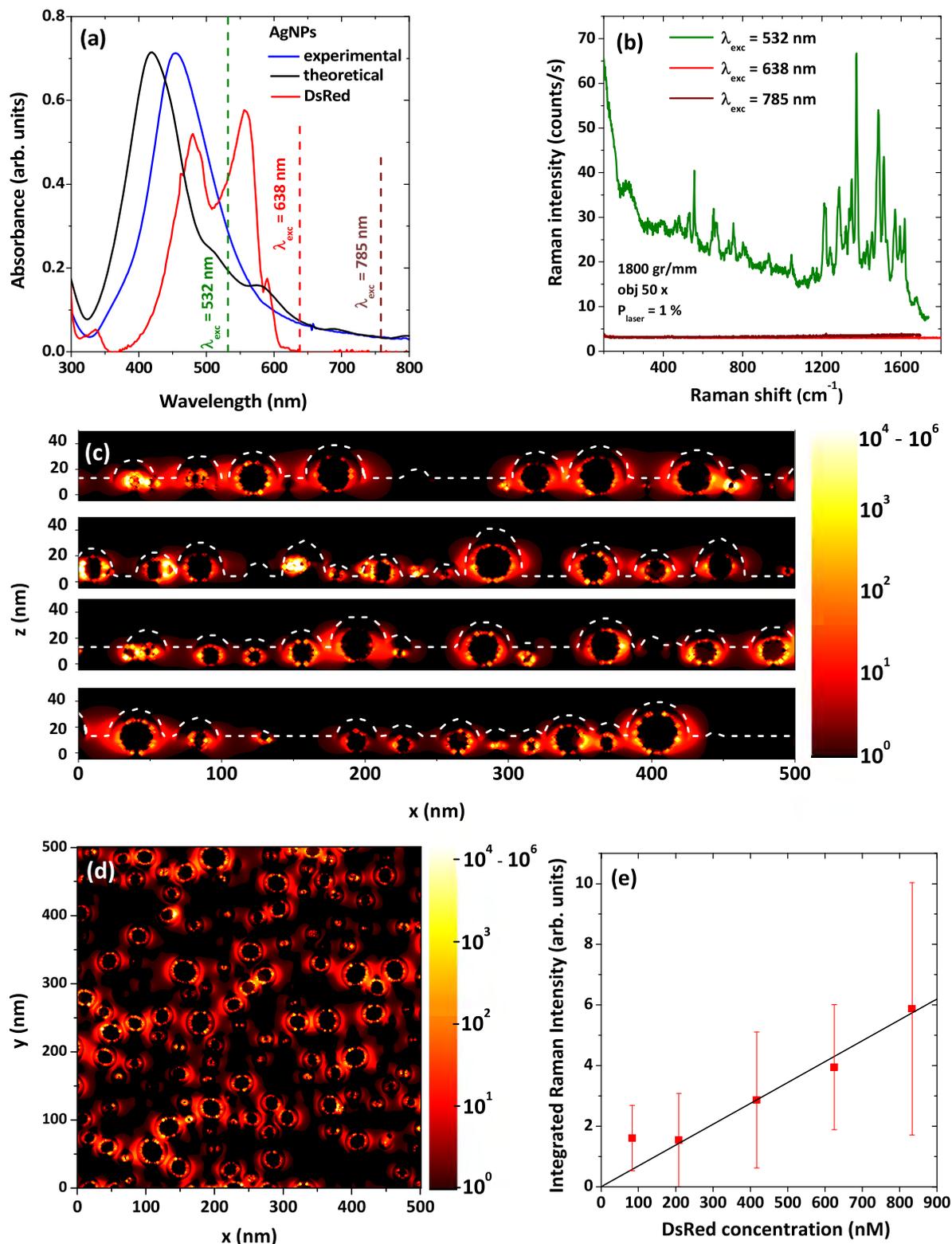


**Figure 3.** (a) Schematic representation of the tetrameric DsRed fluorescent protein, its chromophoric structure and a scheme of the main electronic energy levels, (b) Raman spectra recorded on a pristine quartz substrate (black line) and on a thin layer of DsRed proteins adsorbed on quartz substrate (red line), (c) PL spectra of the DsRed thin layer acquired at different points on the DsRed thin layer, and (d) PL mapping over a  $3 \times 3 \mu\text{m}^2$  square of the DsRed layer recorded with a step size of  $0.5 \mu\text{m}$ .

lower intensity LSPRs above 700 nm resulting from strongly interacting dimers, trimers, and other NP clusters.

To the best of our knowledge, the Raman scattering properties of DsRed in its native state have not been investigated. Density Functional Theory (DFT) calculations of the electronic and Raman scattering properties have been performed for DsRed model chromophores [55] and the calculated Raman spectra were compared with those measured under non-resonant excitation (752 nm), from chemically synthesized DsRed chromophores in solution [56]. Moreover, the structure of the model chromophore is slightly different from that of the recently cloned naturally fluorescent wild-

type DsRed protein, resulting in shifted excitation and emission bands, as well as in much lower optical quantum yields [56]. Besides, no information is reported on the protein conformational changes when adhered on solid substrates or under illumination. The SERS-active substrates used in this study are suitable for investigation of adhesion of molecules (proteins) as they allow for significant enhancement of the Raman signatures of very small quantities. Indeed, the plasmonic resonance of the AgNPs-based substrates and the absorption band of the DsRed protein (figure 4(a), red line) match rather well, which provides additional enhancement through a resonant SERS effect. To confirm the presence of



**Figure 4.** (a) Absorption spectra of the AgNPs-based plasmonic substrate, experimental (blue line) and theoretical (black line), and of the DsRed protein (red line), (b) Raman spectra recorded on a thin layer of DsRed proteins adsorbed on the AgNPs-based plasmonic substrate for different excitation wavelength, (c)  $|E/E_0|^4$  calculated at 532 nm for four different cross-sections taken along the polarization direction (i.e.  $x$ -direction). The white dashed line highlights the free surface of the silica layer, (d)  $|E/E_0|^4$  spatial distribution calculated at 532 nm in the  $(x, y)$  plane. The Raman spectra were normalized to the same accumulation time and laser power, in order to compare their relative intensities, and (e) integrated Raman intensity for DsRed-thin layers deposited from solution with DsRed concentrations in the range 80–800 nM. The vertical bars show the deviations in the integrated Raman intensity for the protein layers issued from each DsRed concentration in solution.

efficient SERS, the samples were excited at three wavelengths: 532, 638, and 785 nm (figure 4(b)). Raman peaks are clearly observed only for the lowest excitation wavelength i.e. close to resonance with both the AgNPs LSPR and the DsRed absorption band. This resonant Raman scattering behavior was consistently noted for all the investigated samples, hence confirming the role of the AgNPs at the origin of the SERS signal of the adhered protein layer. Experimental evaluation of the SERS enhancement factor of our plasmonic substrates was not possible as without AgNPs no Raman signal from DsRed protein layers could be detected (figure 3(b)), even for the layer resulting from the highest concentration of proteins in solution (800 nM).

In order to investigate the EM near-field enhancement of the Raman scattering in our samples, we performed FDTD numerical simulations. The simulations give an idea on the plasmonic enhancement factor of the Raman scattering but more importantly they allow determining the spatial distribution of the plasmonic field and its dependence on the nanoparticles morphology, interaction and location with respect to the sample surface. Figures 4(c) and (d) display cross-section and plan view maps of the fourth power  $|E/E_0|^4$  of the calculated near-field at 532 nm wavelength, which gives the magnitude of the SERS EM enhancement factor [28–30]. It can be noticed that the hot spots form in the gap regions between the AgNPs (figure 4(c)) and are uniformly distributed across the substrate (figure 4(d)). With the exception of a few very intense hot spots reaching enhancement factors of  $10^6$ , the enhancement factor at 532 nm typically lays at  $10^5$  with an averaged value of  $2.0 \times 10^4$  per nanoparticle. Although most of the EM field is enhanced at the AgNP-SiO<sub>2</sub> interface, the near-field does penetrate the thin silica layer, spilling out at the free surface. This phenomenon, which has been observed in the case of Ag-Cu<sub>2</sub>O core-shell NPs [79], occurs when the thickness of the dielectric cover (i.e. SiO<sub>2</sub>) is comparable to the near-field characteristic decay length. This near-field spill-out explains the observed SERS effect. For larger silica thicknesses, the near-field would then be exclusively re-localized at the metallic surface, canceling any SERS effect.

In order to probe the performance of our AgNPs substrates in terms of SERS efficiency, we have acquired Raman data for several DsRed protein layers deposited with concentrations in solution spanning from 80 to 800 nM. The spectrally integrated Raman intensities measured for different DsRed concentrations are reported in figure 4(e). The integrated Raman intensity increases linearly with increasing DsRed concentration in solution, as expected. However, due to the formation of non-uniform and inhomogeneous proteins layers, the Raman scattering intensity strongly fluctuates from point-to-point thus leading to a quite important scattering of the measured Raman intensity for a given protein layer. Nevertheless, the observed in figure 4(e) linear behavior confirms that the measured Raman signal is due to the DsRed proteins and not to some contaminants that could have adhered to the surface during manipulation of the samples.

The departure of the SERS measurements from linear trend for the protein layer resulting from 80 nM concentration in solution is due to local fluctuations of the DsRed protein. It is worth underlining that, for the lowest concentration (0.01 g l<sup>-1</sup>, 80 nM) the protein layer is organized in rod-like structures of isolated DsRed monomers with small residues of tetramers spread over the substrate at a distance from each other of more than 15  $\mu$ m [61]. Presence of DsRed tetramers is actually at the origin of the departure of the Raman intensity from linear trend for the protein layer deposited with 80 nM concentration in solution.

Although 80 nM is the lowest protein concentration used to obtain a protein layer for the current study, it cannot be defined as the lowest detection limit for the plasmonic substrates. The possibility to detect very intense Raman signal from proteins deposited at 80 nM suggests that this value could be decreased. However, the nature of the protein (the DsRed is initially under tetrameric form in the solution and transforms into monomers when interacting with the solid surface of the plasmonic substrate [61]) and the morphology of the obtained dehydrated layer should be considered if searching for the lowest detection limit.

During the experiments, we have systematically observed strong fluctuations of the Raman scattering intensities: spectral features which are very weak or absent may suddenly become very intense (several thousand of counts/s), whereas other features may strongly fluctuate before they fade away. This phenomenon is well-known as SERS blinking [80] and is typical of Raman scattering by a small number of molecules located at plasmonic hot spots. It is usually observed in single molecule SERS experiments [81, 82]. Because of blinking the SERS intensity is very difficult to estimate with precision. Indeed, time averaging may lead to random SERS intensity values depending on the occurrence time and the duration of this phenomenon.

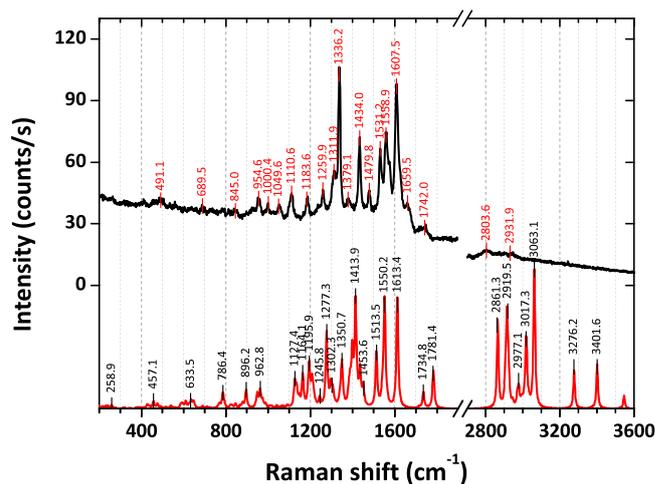
#### 3.4. DsRed proteins adhered on AgNPs-based nanocomposites: assignment of the SERS features

Aiming at an assignment of the measured Raman features to the vibration modes of the proteins, we have performed calculations based on the DFT which allows for predicting the vibration eigenmodes of the proteins (see materials and methods section). To generate the corresponding Raman activity DFT calculations make use of the molecular polarizability modulation which is appropriate only for non-resonant Raman scattering experiments. It does not account for the plasmonic resonance effect, and therefore cannot predict the SERS intensities. In addition, because of the SERS blinking, the intensity of the Raman features strongly fluctuates, which is another reason for the discrepancy between the measured SERS intensities and the DFT-calculated Raman activities. Nevertheless, DFT calculations are very useful for assignment of the observed Raman features based on their measured vibrational frequencies [15, 80].

Since the SERS blinking is often associated with molecular configuration fluctuations and/or photo-induced chemical processes which may alter the molecular structure, for

the DFT calculations we have considered three different molecular configurations of the DsRed chromophore (labeled hereafter A, B, and C; see supplementary information) with very close energy minima. In configuration A, with a minimum energy of  $-1332.6434$  Ha, the phenol ring carried by 67Tyr (tyrosine 67) lies nearly in the same plane as the imidazolinone ring formed by 68Gly (glycine 68) and the same 67Tyr. Configuration B has a minimum energy of  $-1332.6511$  Ha i.e. 0.2 eV below configuration A. It differs from configuration A for the perpendicular positioning of the phenol ring with respect to the imidazolinone one. In configuration C, the C=N bond of the imidazolinone ring is broken, completely altering in this way the chromophore structure. Its minimum energy is  $-1332.6689$  Ha i.e. 0.68 eV below configuration A. By comparing the Raman spectra calculated for configurations A, B and C one can understand of how the molecular configuration fluctuations, or in our case the protein conformational changes, may impact the Raman peak intensities and give rise to Raman blinking in experimental situations. However, it is important to underline that the interpretation of the SERS blinking phenomenon is still under debate in the SERS community and vibrational frequency fluctuations were reported and exploited in very few works [80]. The main issue lies in the modeling of realistic situations (interaction of large molecules physically or chemically adsorbed on a surface) at the atomic scale using quantum chemistry techniques. Moreover, since SERS blinking is a photo-thermo-induced phenomenon, there is a need of time-dependent simulation techniques capable of modeling excited states of large molecule ensemble. It is worth to underline that in most of the situations where SERS blinking was observed, the molecules under study were either tightly bounded to or coated on the metal nanoparticle. In our case, the very thin SiO<sub>2</sub> cover layer (thickness of 5.5 nm) acts as a barrier against direct interaction between the adsorbed proteins at the sample surface and the AgNPs underneath the sample surface. Hence, the SERS blinking is solely due to photo-induced configuration fluctuations and not to the molecular adsorption/desorption process at the metal nanoparticle surface.

The assignment of the Raman features observed in SERS spectra is not straightforward because of the strong blinking of the Raman signal mentioned above. Therefore, to extract general trends from the Raman signature of the protein, we have analyzed a large set of experimental data (over 300 Raman spectra) acquired from DsRed proteins located at different points on the samples. The spectra presented and discussed in this section are representative of each one of the simulated configurations. We can affirm that 70% of the data are totally assignable to one of the three simulated configurations. The remaining 30% of the recorded spectra could not be fully ascribed to any of the three configurations for the following reasons: (i) the Raman signal is not observed in all scanned points. This is due to the fact that the studied DsRed protein layers are discontinuous, even for the layer resulting from the highest protein concentration in solution:  $0.1 \text{ g l}^{-1}$  (800 nM). As given in section 3.2 it covers only one third of the sample surface. There are no proteins at all in some



**Figure 5.** SERS spectrum of DsRed dehydrated protein layer deposited from solution with DsRed concentration of  $0.05 \text{ g l}^{-1}$  (400 nM) (black line) and DFT-simulated Raman spectrum of the DsRed chromophore in configuration A (red line). The identified Raman features are also shown.

regions on the sample. So, most of the remaining 30% of the spectra displayed no signal i.e. only background signal due to AgNPs, taken as reference, was detected and (ii) in very few regions, we have observed the co-presence of different configurations. These spectra were not considered as no clear identification of the protein's conformation can be achieved.

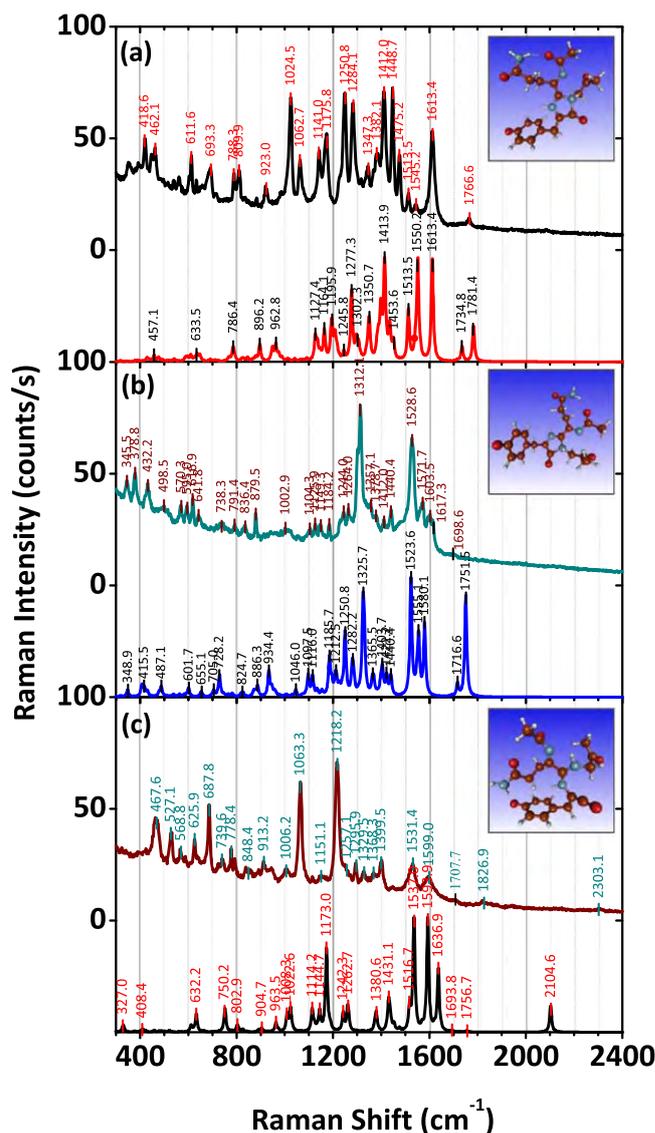
Comparison between the SERS spectrum of the DsRed measured for a dehydrated protein layer deposited from protein concentration in solution of  $0.05 \text{ g l}^{-1}$  (400 nM) and DFT-simulated Raman spectrum of the DsRed chromophore in configuration A is reported in figure 5. Three distinct spectral regions,  $200\text{--}1000 \text{ cm}^{-1}$ ,  $1000\text{--}1800 \text{ cm}^{-1}$ , and  $2700\text{--}3500 \text{ cm}^{-1}$ , can be identified (figure 5). All the observed Raman features below  $1000 \text{ cm}^{-1}$  belong to angular (in- and out-of-plane) deformations of the imidazolinone and the phenol rings carrying the three amino-acids (Gln-Tyr-Gly) that compose the DsRed chromophore and to vibrations of the entire protein [83, 84]. This assignment is also supported by previous reports on the Raman scattering properties of the GFP protein [85]. The presence of glycine in the polypeptide chain has important consequences for the overall structure of DsRed proteins. Due to the lack of any significant functional group the glycine possesses little intrinsic chemical reactivity. Thus the absence of a large side chain results in conformational flexibility about the N-C and C-C bonds in the polypeptide chain [1]. Consequently, this spectral region of the Raman spectra holds information on the secondary structure of the DsRed. The spectral range  $1000\text{--}1800 \text{ cm}^{-1}$ , where the most intense Raman features are observed, is correlated to the vibration modes of the phenol and imidazolinone rings as well as to the C=C double bond stretching vibrations ( $1500\text{--}1800 \text{ cm}^{-1}$ ). The Raman features barely visible in the  $2800\text{--}3500 \text{ cm}^{-1}$  range are related to C-H, N-H, and O-H stretching modes. They are particularly sensitive to the molecule chemical environment because of the reactivity of the hydrogen atom [85]. Detailed assignment of

the observed Raman features based on the DFT calculations and on published works [83–87] is given in the supplementary information.

It is interesting to compare the measured SERS peaks of the adhered wild-type DsRed proteins with the Raman data reported for three DsRed model chromophores: 4-Hydroxybenzylidene-1, 2-dimethylimidazolinone (HBDI), 4-hydroxybenzylidene-1-methyl-2-propenyl-imidazolinone (HBMPI) and 4-hydroxybenzylidene-1-methyl-2-penta-1, 3-dien-1-yl-imidazolinone (HBMPDI) [56]. These model chromophores have been synthesized and investigated aiming at an identification of the chromophore formation mechanisms responsible for the strong red-shift of the PL emission. They differ from the wild-type DsRed proteins for the absence of the  $\alpha$ -helix and  $\beta$ -sheets that naturally surround the chromophore and for the different extensions of the conjugated  $\pi$ -system, that is partially responsible for the red-shifted spectroscopic properties of DsRed when compared to GFP [56, 88–91]. Therefore, the differences between the Raman feature frequencies observed in wild-type DsRed proteins and the model chromophores HBDI, HBMPI and HBMPDI can be due either to the different extensions of the conjugated  $\pi$ -system or to the chromophore environment that influences the molecular structure [87]. Although most of the observed Raman features in the SERS spectra belong to the DsRed model chromophores, there are additional Raman peaks that cannot be ascribed to the later, no matter the configuration considered by the DFT simulations. These additional Raman peaks can be instead attributed to the reminder of the protein i.e. the protein secondary structure, which is not in resonance with the used excitation wavelength. Specifically, the peak at around  $1660\text{ cm}^{-1}$ , well visible in the protein spectrum of figure 5, can be assigned to the amide I vibration mode of the protein (mostly coming from the protein  $\alpha$ -helices), as already reported for wild-type GFP [87]. This agrees with the Fourier transform infrared data analysis performed on the same dehydrated DsRed protein layers [61, 75]. The peak at  $1050\text{ cm}^{-1}$  can be assigned to the aromatic side-chain mode of the protein, while the additional weaker peaks in the range  $1200\text{--}1400\text{ cm}^{-1}$  range can be related to the amide III vibration modes of the protein (giving complementary structural information on the protein structure) [87]. Finally, the peak observed at  $1530\text{ cm}^{-1}$  has contributions coming from the proteins amide II band [61, 75] (linked mainly to the protein  $\beta$ -sheets) although it appears broader and shifted towards higher wavenumbers when compared to the related C=N stretching of the imidazolinone ring ( $1513\text{ cm}^{-1}$ ) on the DFT-simulated spectrum.

### 3.5. DsRed proteins adhered on AgNPs-based nanocomposites: conformational changes and temporal evolution

Most of the Raman spectra acquired from different points of the sample surface and for the different investigated DsRed layers are well accounted for by the DFT simulations performed for the DsRed chromophore in configuration A. There exists however Raman signatures which are not in line with



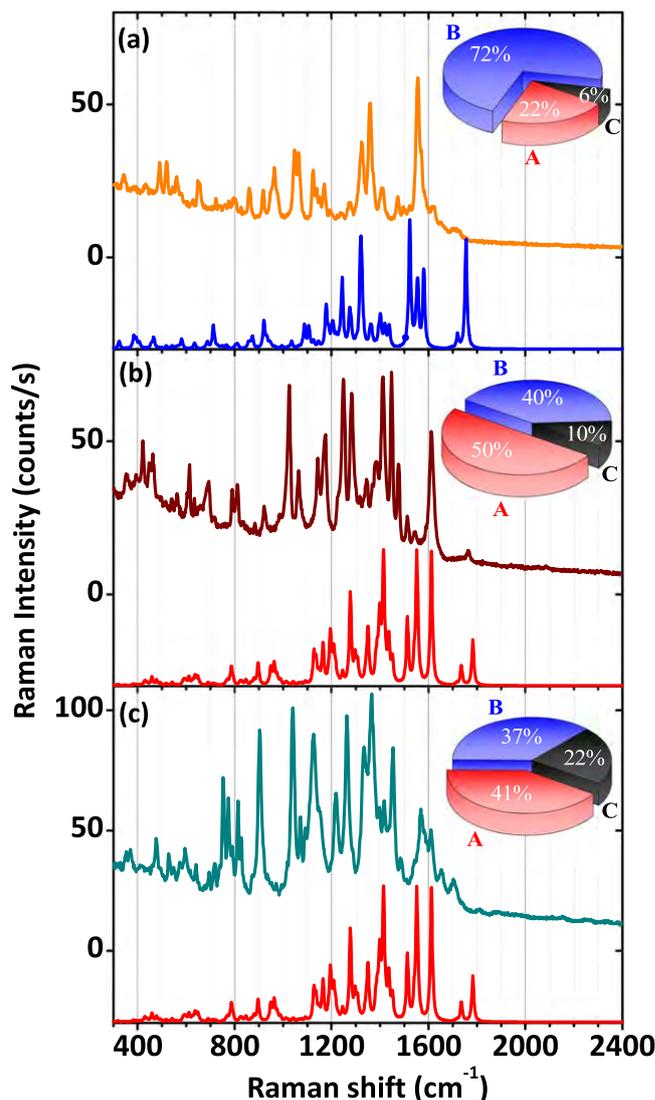
**Figure 6.** Experimentally recorded SERS spectra (upper spectra) of DsRed dehydrated protein layer deposited from solution with DsRed concentration of  $0.05\text{ g l}^{-1}$  ( $400\text{ nM}$ ) and DFT-simulated Raman spectra (lower spectra) of the DsRed chromophore in three different configurations: (a) configuration A, (b) configuration B and (c) configuration C. The Raman spectra were recorded with an accumulation time of 30 s. Images of the three identified conformations are shown in insets for the corresponding configuration A, B and C.

configuration A. The DFT simulations performed in two other configurations, namely B and C, appear very useful to investigate whether the adsorbed and dehydrated DsRed proteins can be stabilized in other conformational (configuration B) and/or chemical forms (configuration C).

The SERS spectra extracted from systematic mapping of the DsRed dehydrated layer (concentration in solution of  $0.05\text{ g l}^{-1}$ , i.e.  $400\text{ nM}$ ) are presented in figure 6. These spectra match rather well the DFT-simulated Raman spectra of the three considered configurations, reported in the same graph. Detailed description of the observed molecular vibrations, including those related to the three amino-acids (Gln–Tyr–Gly) [84] present in the peptide sequence of DsRed

and the related band assignment are reported in the supplementary information. Configurations A and B differ from each other only for the relative positioning of the imidazolone and phenol rings (the latter is perpendicular to the former in configuration B), resulting in a shift of the frequency of the main C=C double bond stretching vibrations ( $1500\text{--}1800\text{ cm}^{-1}$ ). On the contrary, the configuration C presents a broken C=N bond of the imidazolone ring, which strongly impact its vibration modes and influences those of the phenol ring. The presence of this broken configuration C is evidenced in the Raman spectrum in figure 6 through the decrease of the Raman intensities of most of the spectral features observed in the  $1200\text{--}1600\text{ cm}^{-1}$  range and through the appearance of features between  $2000$  and  $2500\text{ cm}^{-1}$  (even though with small intensity). All these differences make the broken molecule (configuration C) distinguishable from the two other stable configurations only due to its SERS fingerprint.

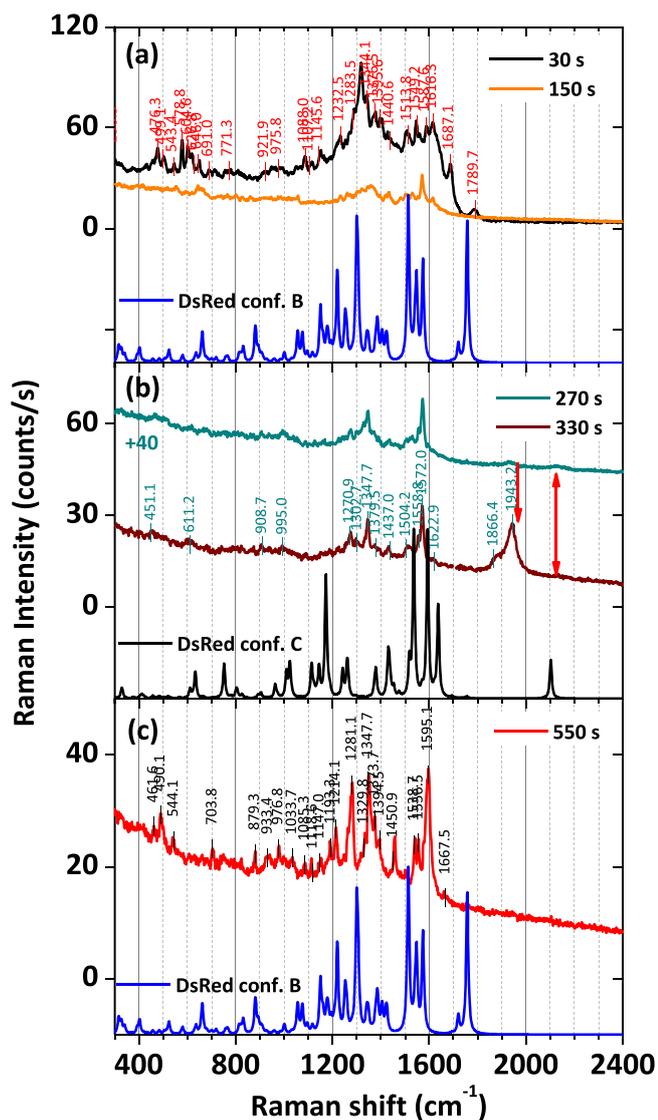
Furthermore, the population distribution of DsRed proteins stabilized on the substrate was analyzed as a function of the DsRed concentration in solution. Figure 7 reports experimental and simulated spectra of the most frequently observed configuration for three protein concentrations:  $0.01\text{ g l}^{-1}$  ( $80\text{ nM}$ , figure 7(a)),  $0.05\text{ g l}^{-1}$  ( $400\text{ nM}$ , figure 7(b)) and  $0.1\text{ g l}^{-1}$  ( $800\text{ nM}$ , figure 7(c)), alongside with the protein population distributions in the insets. DsRed proteins adhered on the surface and stabilized in configuration B predominate significantly ( $72\%$ ) for the layer resulting from the lowest DsRed concentration in solution ( $80\text{ nM}$ ) (inset in figure 7(a)). The contributions of the different configurations evolve with increasing the DsRed concentration. In the layers issued from protein concentration in solution higher than  $400\text{ nM}$ , the DsRed proteins stabilize mainly in configurations A and B, with majority of configuration A. For example, the estimation gives that configuration A is present at  $50\%$ , configuration B at  $40\%$  and configuration C at  $10\%$  of the analyzed spectra for concentration of  $0.05\text{ g l}^{-1}$  ( $400\text{ nM}$ ) displayed in figure 7(b). Globally, the quantity of the proteins displaying configuration C increases as a function of the DsRed concentration in solution (from  $6\%$  up to  $22\%$  starting from the lowest DsRed concentration). This latter aspect could be due to the presence of different photo-induced interaction mechanisms between the DsRed proteins and the AgNPs-based plasmonic substrate when the protein rearrangement occurs during the interaction of DsRed with the solid surface of the substrate. Indeed, for the protein layer resulting from the lowest concentration the signal is likely given by DsRed isolated single proteins under monomer form, while for the DsRed layers deposited at higher concentrations either DsRed proteins under monomer and tetrameric form or closely situated monomers and/or dimers can contribute. The different morphologies of the protein layer can thus explain the different population distributions detected via the SERS signal. The optical dipolar coupling between adjacent chromophore sites, which is characteristic for the DsRed proteins, becomes stronger when packed monomers, dimers or tetramers are present, resulting



**Figure 7.** Experimentally recorded SERS spectra (upper spectra) and DFT-simulated Raman spectra (lower spectra) of DsRed dehydrated protein layers deposited from solution with (a)  $0.01\text{ g l}^{-1}$  ( $80\text{ nM}$ ), (b)  $0.05\text{ g l}^{-1}$  ( $400\text{ nM}$ ) and (c)  $0.1\text{ g l}^{-1}$  ( $800\text{ nM}$ ) DsRed concentrations. The Raman spectra were recorded with an accumulation time of  $30\text{ s}$ . In the insets, pie charts representing the DsRed population distributions in configurations A, B and C, for each protein concentration, are reported.

in stronger photo-induced interactions, highest optical absorption and thus increased modifications in the protein conformation.

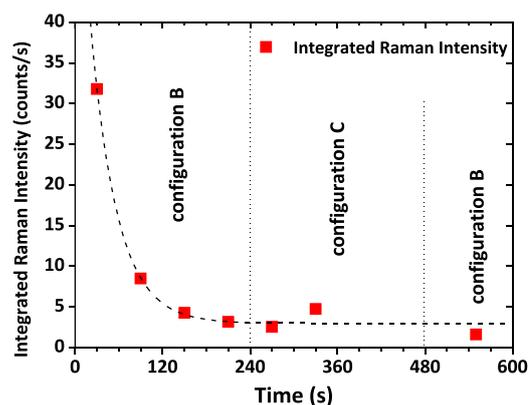
To complete our analysis and better support the above given findings, we have investigated the temporal evolution of the SERS intensity of the DsRed proteins on the time-scale of few minutes. As mentioned above, conformational fluctuations of the DsRed proteins and/or chemical processes altering their molecular structure can be at the origin of the blinking of Raman signal. Indeed, under laser irradiation, because of the plasmonic induced light absorption by HOMO-to-LUMO transitions, the DsRed proteins undergo some structural changes, losing temporary or permanently their conformation, which in turn results in fluctuations of



**Figure 8.** Time-dependent character of the conformational changes of DsRed proteins. Experimentally recorded SERS spectra (upper spectra) and DFT-simulated Raman spectra (lower spectra) of the DsRed chromophore in time: (a)  $t = 30$  s and 150 s, (b)  $t = 270$  s and 330 s and (c)  $t = 550$  s. The Raman spectra were recorded with an accumulation time of 30 s. For this study, the DsRed layer was deposited from the highest available DsRed concentration in solution ( $0.1 \text{ g l}^{-1}$  or 800 nM).

their Raman signatures. To illustrate the time-dependent character of the conformational changes of DsRed proteins, some of the most significant Raman spectra are reported in figure 8.

Shortly after illumination a strong decrease of the Raman spectrum intensity is observed (figure 8(a)). It is accompanied by change in the intensity of some of the characteristic Raman peaks. In time this event is followed by appearance of new Raman peaks at higher wavenumbers (figure 8(b)), which are ascribed to the stretching vibration of the broken C=N bonds in the DsRed chromophore's imidazolinone ring, already discussed above. It may appear that the experimental spectrum is a mixture of B and C configurations but the presence of a very intense peak at  $1950 \text{ cm}^{-1}$  determines the C



**Figure 9.** Temporal evolution of the spectrally integrated Raman intensities after subtraction of the background signal. The spectra were acquired with 30 s accumulation time. DsRed thin layer deposited from solution with DsRed concentration of  $0.1 \text{ g l}^{-1}$  (800 nM).

configuration as predominant. This observation reveals a time-dependent transition in the protein structure from configuration B to configuration C. Such processes can be photo-induced since the molecules are submitted to intense illumination by the probe light [92–94]. For larger elapsed time (after 8 min) the proteins are stabilized back to configuration B (figure 8(c)). An intense peak can be noticed at  $1595 \text{ cm}^{-1}$  in relation with the transitory state of the proteins, i.e. to the chemical transformations of the DsRed structure.

The temporal evolution of the spectrally integrated Raman intensities after subtraction of the background signal is reported in figure 9. One can notice the strong fourfold reduction of the Raman intensity during the first 60 s. This transient evolution is followed by stabilization of the DsRed proteins in configuration B. In the next four minutes, the observed Raman spectra point to protein stabilization in configuration C, followed by a return back to the initial configuration B.

Without loss of generality the temporal evolution of the SERS signal of DsRed proteins can be explained as follows: upon irradiation, and because of the large optical absorption of the DsRed proteins, the laser induced heating leads to desorption of some adhered DsRed proteins, thus causing the initial drop of the SERS signal (figure 8(a)). Then, the chromophore's structure of the still adsorbed proteins undergoes optically assisted chemical transformation processes which lead to the protein transient stabilization in configuration C (figure 8(b)). Finally, either some of the desorbed proteins re-adsorb on the plasmonic substrate or the still adhered ones flip back to their initial configuration, even though with a lower SERS intensity (figure 8(c)). Such photo-induced desorption/re-adsorption process have already been discussed in the literature [80]. Under non-resonant excitation the SERS signal and its blinking disappear (figure 4(b)). The observed SERS measurements here are resonant with the HOMO-LUMO transition of the proteins which means that a protein initially settled in configuration C or B, may relax back to a different metastable configuration thus leading to configuration fluctuations and SERS blinking. The photon

energy used for SERS measurements is 2.33 eV, so it is high enough to induce fluctuations from C (energetically more stable) to B configuration. Further studies are required to fully elucidate the origin of the SERS signal and its temporal fluctuations, a subject still highly debated in the SERS community. In our AgNPs-based plasmonic substrates, the 5.5 nm thick SiO<sub>2</sub> shell (figure 1(a)) acts as a barrier against charge tunneling and transfer between the metal AgNPs and the adhered DsRed proteins. However, excitation transfer due to the near-field interaction between the nanoparticle surface plasmons and the HOMO-to-LUMO transitions of the proteins is likely to take place. This mechanism leads to enhanced excitation of the proteins followed by conformational changes. The SERS blinking discussed here thus gives valuable information on the dynamics of the proteins adhered on the AgNPs plasmonic substrates. It reveals that the protein structure is essentially preserved although some alterations can be observed. This scenario endorses the dynamical character of the relationship between protein structure and function. It also confirms that, to some extent, the conformational changes of proteins with strong internal coherence, like DsRed proteins, are reversible.

#### 4. Conclusions

In this work we have investigated via SERS effect the response of wilde-type DsRed (an optically absorbing, naturally FP) thin protein layers after adsorption, interaction and dehydration of the proteins on the solid surface of AgNPs-based plasmonic substrate. To that end highly reproducible and sensitive AgNPs-based plasmonic substrates were realized on large scale by a plasma deposition process that successfully combines sputtering from a silver target, to realize the monolayer of AgNPs, with plasma polymerization to coat conformably the AgNPs with an ultra-thin silica layer. The monolayer of AgNPs is composed of smaller, rather spherical NPs (diameter of  $5.0 \pm 1.7$  nm) overlapped with larger, prolate spheroidal ones (major axis of  $19.9 \pm 10.0$  nm) and it is responsible of the plasmonic effect. The ultra-thin silica cover layer, intended to protect the metallic silver against quick oxidation or premature aging, also properly avoids the direct contact (i.e. chemisorption) of the proteins with the AgNPs-active surface and maximizes the SERS EM mechanism based on 'plasmon resonance'. After electrodynamic simulation, the EM near-field enhancement (SERS EM enhancement factor) was found to be localized in proximity of the plasmonic substrate's surface. It was found to reach values as high as  $10^5$  (surface averaged value of about  $2.0 \times 10^4$  per silver nanoparticle), thus guarantying the validity of our AgNPs-based substrates as plasmonic sensors. The plasmonic systems were coupled with DsRed proteins in the form of dehydrated, thin and discontinuous mono-layers realized by dip coating process starting from DsRed stock solution of concentrations varying between 80 and 800 nM. Intense SERS spectra for all the investigated DsRed thin layers were detected only in presence of the AgNPs-based plasmonic substrates. The Raman features were mostly ascribed to the DsRed

chromophore's vibrational modes, as evidenced by DFT calculations. However, it was evidenced that the spectral region 200–1000 cm<sup>-1</sup> holds information on the secondary structure of the DsRed proteins. The spectral range 1000–1800 cm<sup>-1</sup> containing the most intensive Raman features is mainly correlated with the DsRed chromophore structure. The 2800–3500 cm<sup>-1</sup> range is particularly sensitive to the DsRed chromophore chemical environment, i.e. the primary and secondary structure of DsRed proteins, because of the reactivity of the hydrogen atom. The temporal evolution of the SERS intensity of the DsRed proteins on the time-scale of few minutes was also investigated. It is shown that under laser irradiation the DsRed proteins can undergo optically assisted chemical transformations resulting in structural changes and in the temporary or permanently stabilization of the protein in different conformations, with an eventual flip back to their initial state. This mechanism is in part responsible of the observed fluctuations of the Raman signatures. Although further studies are required to fully elucidate the relationship between protein structure and function, which lays at the basis of the SERS signal and its temporal fluctuations, the results discussed here give valuable information on thin protein layers of DsRed monomers adhered on AgNPs-based plasmonic substrates. They reveal that the protein structure is essentially preserved, even though some alterations can be observed during irradiation, and endorse the dynamical character of the interaction between proteins, laser beam and plasmonic surfaces.

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