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# A novel bacteriochlorin–styrylnaphthalimide conjugate for simultaneous photodynamic therapy and fluorescence imaging†

Pavel A. Panchenko,<sup>a</sup> Mikhail A. Grin,<sup>c</sup> Olga A. Fedorova,<sup>a,b</sup> Marina A. Zakharko,<sup>a</sup> Dmitriy A. Pritmov,<sup>c</sup> Andrey F. Mironov,<sup>c</sup> Antonina N. Arkhipova,<sup>a</sup> Yuri V. Fedorov,<sup>a</sup> Gediminas Jonusauskas,<sup>d</sup> Raisa I. Yakubovskaya,<sup>e</sup> Natalia B. Morozova,<sup>e</sup> Anastasia A. Ignatova<sup>f,g</sup> and Alexey V. Feofanov<sup>f,g</sup>

Propargyl-15<sup>2</sup>,17<sup>3</sup>-dimethoxy-13<sup>1</sup>-amide of bacteriochlorin e (**BChl**) and a 4-(4-*N,N*-dimethylaminostyryl)-*N*-alkyl-1,8-naphthalimide bearing azide group in the *N*-alkyl fragment were conjugated by the copper(I)-catalyzed 1,3-dipolar cycloaddition to produce a novel dyad compound **BChl–NI** for anticancer photodynamic therapy (PDT) combining the modalities of a photosensitizer (PS) and a fluorescence imaging agent. A precise photophysical investigation of the conjugate in solution using steady-state and time-resolved optical spectroscopy revealed that the presence of the naphthalimide (**NI**) fragment does not decrease the photosensitizing ability of the bacteriochlorin (**BChl**) core as compared with **BChl**; however, the fluorescence of naphthalimide is completely quenched due to resonance energy transfer (RET) to **BChl**. It has been shown that the **BChl–NI** conjugate penetrates into human lung adenocarcinoma A549 cells, and accumulates in the cytoplasm where it has a mixed granular-diffuse distribution. Both **NI** and **BChl** fluorescence *in vitro* provides registration of bright images showing perfectly intracellular distribution of **BChl–NI**. The ability of **NI** to emit light upon excitation in imaging experiments has been found to be due to hampering of RET as a result of photodestruction of the energy acceptor **BChl** unit. Phototoxicity studies have shown that the **BChl–NI** conjugate is not toxic for A549 cells at tested concentrations (<8 μM) without light-induced activation. At the same time, the concentration-dependent killing of cells is observed upon the excitation of the bacteriochlorin moiety with red light that occurs due to reactive oxygen species formation. The presented data demonstrate that the **BChl–NI** conjugate is a promising dual function agent for cancer diagnostics and therapy.

## 1. Introduction

Photodynamic therapy (PDT) has emerged as an important treatment modality for a variety of cancers in recent years.<sup>1,2</sup> PDT involves three necessary components: light, a photosensitizer (PS), and tissue molecular oxygen. Upon irradiation by light of appropriate wavelength, the PS is promoted to a short lived singlet state which rapidly converts to the excited triplet state (<sup>3</sup>PS\*) through the process of intersystem crossing. Then, <sup>3</sup>PS\* transfers its excess energy to nearby O<sub>2</sub> molecules to form reactive oxygen species such as singlet oxygen (<sup>1</sup>O<sub>2</sub>) and free radicals, which are toxic to malignant cells and tissues.<sup>3–6</sup>

Among various photosensitizing agents, porphyrin-based compounds possess unique advantages related to their ability to be retained in tumors and to produce cytotoxic singlet oxygen. Photofrin, a porphyrin-type PS of the first generation, has achieved some clinical efficacy, but at the same time it suffered from several drawbacks such as chemical heterogeneity, low

<sup>a</sup> A. N. Nesmeyanov Institute of Organoelement Compounds of Russian Academy of Sciences, 119991, Vavilova str. 28, Moscow, Russia. E mail: pavel@ineos.ac.ru;

Fax: +7 499 135 50 85; Tel: +7 499 135 80 98

<sup>b</sup> D. Mendeleev University of Chemical Technology of Russia, 125047, Miusskaya sq. 9, Moscow, Russia

<sup>c</sup> Moscow Technological University, Institute of Fine Chemical Technologies, 119571, Prospect Vernadskogo, 86, Moscow, Russia

<sup>d</sup> Laboratoire Ondes et Matière d'Aquitaine, UMR CNRS 5798, Bordeaux University, 33405, 351 Cours de la Libération, Talence, France

<sup>e</sup> P. Hertsen Moscow Oncology Research Institute – Branch of the National Medical Research Radiological Centre of the Ministry of Health of the Russian Federation, 125284, 2nd Botkinskiy pr. 3, Moscow, Russia

<sup>f</sup> Biological Faculty, Lomonosov Moscow State University, 119992, Leninskie Gory 1, Moscow, Russia

<sup>g</sup> Shemyakin Ovchinnikov Institute of Bioorganic Chemistry of Russian Academy of Sciences, 117997, 16/10, Miklukho Maklaya str., Moscow, Russia

depth of tissue treatment caused by limited light penetration due to the absorption wavelength (630 nm) laying outside the “phototherapeutic window” (650–1350 nm), a low molar extinction coefficient at 630 nm, and prolonged cutaneous photosensitivity caused by its slow elimination in normal tissue.<sup>7</sup> Compared to porphyrins, chlorin- and bacteriochlorin-type PSs in which one or two pyrrole units (diagonal to each other) are reduced respectively exhibit intense absorption in the near infrared region ( $\geq 650$  nm), relatively low dark toxicities, rapid clearance from normal tissue and low cutaneous phototoxicity.<sup>8–13</sup> Despite smaller synthetic availability, di- and tetrahydroporphyrins could be considered as some of the most promising candidates for creating efficient second-generation drugs for PDT of cancer.

An important characteristic of most of the porphyrin-based photosensitizers is their ability to fluoresce. This property has been extensively explored in pre-clinical and clinical studies for fluorescence-image guided PDT. Unfortunately, porphyrins, chlorins, and bacteriochlorins display a small Stokes shift between their longer wavelength absorption and emission bands<sup>14–16</sup> and, therefore, their fluorescence is difficult to filter out of the scattered excitation light. This property of the PS fluorescence complicates imaging of deeply seated and large tumors. On the other hand, excitation of the porphyrin-based photosensitizer ultimately leads to the production of reactive oxygen species and related toxicity.<sup>14–17</sup>

To overcome this difficulty a new approach which consists of the construction of bifunctional systems combining modalities of a PS and a diagnostic agent (so called theranostics) has been developed.<sup>18–22</sup> In such systems, a fluorescent moiety can be excited selectively and independently from the photosensitizer unit enabling fluorescence imaging without toxic effects. Thus, Pandey and coworkers have used cyanine dyes as fluorescent labels to prepare conjugates with PSs.<sup>18–20</sup> A distinct feature of the emission spectra of cyanine dyes is that their fluorescence can easily reach the near-infrared (NIR) region upon increasing the length of the polymethine chain.<sup>23</sup> However, polymethine cyanine dyes are not so easy to synthesize and to modify, their photo-stabilities are relatively low and their Stokes shift is usually less than 25 nm, which may cause self-quenching as well as the increase of measurement error due to detection of scattered excitation, thus decreasing the detection sensitivity to a great extent as it is in the case of using simple porphyrin sensitizers. Some examples of BODIPY-phthalocyanine<sup>24,25</sup> and rhodamine-phthalocyanine<sup>26,27</sup> conjugates have also been described in the literature. Despite the higher photostability of BODIPY and rhodamine derivatives as compared with cyanine dyes, these types of fluorophores also demonstrate a small difference between absorption and emission maxima. Therefore, NIR dyes with a larger Stokes shift are very promising for the development of bifunctional conjugates for simultaneous photodynamic therapy and fluorescence imaging.

1,8-Naphthalimide derivatives are famous organic fluorophores which generally exhibit high thermo- and photostability and are known to act as fluorescent brighteners and dyes for polymer fibers,<sup>28,29</sup> laser active media,<sup>30,31</sup> electroluminescent materials<sup>32–34</sup> and optical memory devices.<sup>35–37</sup> Because of its

intense fluorescence, large Stokes shifts along with the relative ease of synthetic operations for targeted modification of the molecular structure, these types of compounds have found application in the construction of fluorescent chemosensors for biologically relevant cations and anions,<sup>38–40</sup> labels or probes for proteins, cells, lysosomes and other acidic organelles.<sup>41–43</sup> In our recent papers,<sup>44–46</sup> we have described photophysical properties of naphthalimides containing a substituted styryl fragment as an electron releasing group at the 4<sup>th</sup> position of a naphthalene ring. It has been found that the presence of the 4-(*N,N*-dimethylamino)styryl group extends the  $\pi$ -system of the parent chromophore and results in the long wavelength intramolecular charge transfer (ICT) absorption and emission, which is preferable for fluorescence imaging. Herein, we report on the synthesis, spectroscopic investigation and evaluation of PDT activity of the novel conjugate of a bacteriochlorin photosensitizer and 4-(*N,N*-dimethylamino)styryl-1,8-naphthalimide (**BChI-NI**, Scheme 1). The results and experimental details of our study of optical properties of this molecular system in solution and in living cells are presented. We report on the distinct photo-induced cytotoxicity of **BChI-NI** for human adenocarcinoma A549 cells as well as magenta-to-red conversion of **BChI-NI** fluorescence that can be useful to control the integrity of the photosensitizer moiety during irradiation of cancer cells.

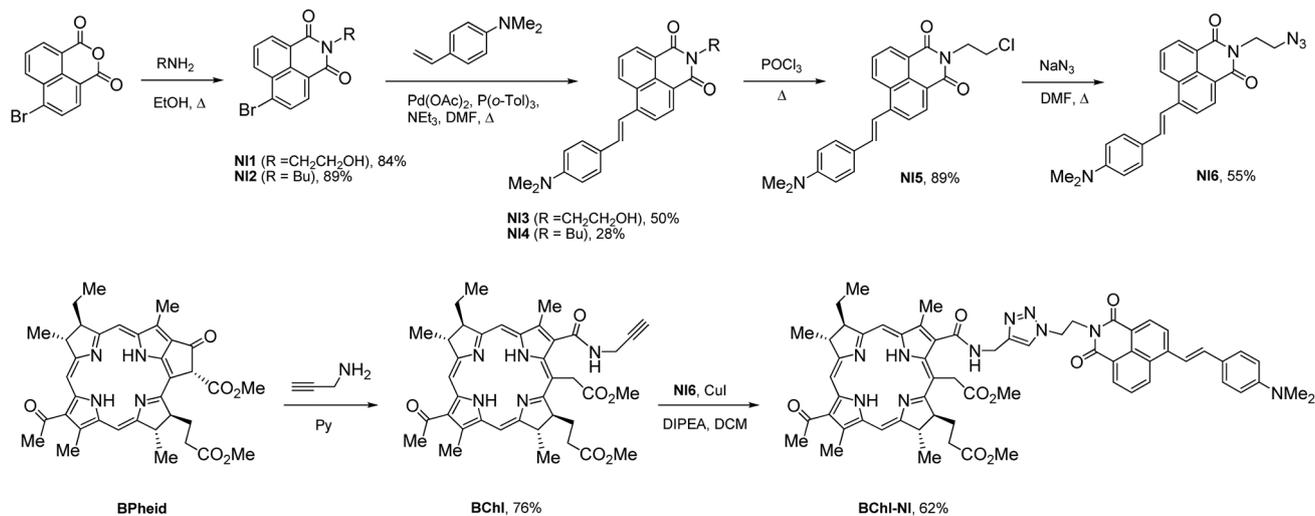
## 2. Experimental procedures

### Synthesis of the BChI-NI conjugate

For the synthesis of **BChI-NI**, we used the well-known copper(I)-catalyzed click reaction of 1,3-dipolar cycloaddition between naphthalimide-containing alkylazide **NI6** and the triple bond derivative of bacteriochlorin *e* **BChI** (Scheme 1). The latter was afforded from the methyl ester of bacteriopheophorbide *a* **BPheid** and propargylamine. Preparation of **BPheid** starting from biomass *Rhodobacter capsulatus* was carried out according to the described method.<sup>47,48</sup> The first step of the synthesis of naphthalimide **NI6**, in which the commercial starting material 4-bromo-1,8-naphthalic anhydride was reacted with ethanolamine, was performed conveniently in EtOH at reflux.<sup>49</sup> Next, 4-bromonaphthalimide **NI1** was subjected to the Heck coupling reaction with 4-*N,N*-dimethylaminostyrene under the catalyst Pd(OAc)<sub>2</sub><sup>50</sup> followed by the nucleophilic substitution of hydroxyl by the azide group in the hydroxyethyl fragment *via* subsequent treatment with POCl<sub>3</sub> and NaN<sub>3</sub>. Details of synthetic procedures and identifications are shown in the ESI.† The synthesis of *N*-butyl-4-styrylnaphthalimide **NI4** which was used for a comparative analysis of spectral characteristics has been described earlier.<sup>44</sup>

### Steady-state optical measurements

The absorption spectra were taken on a Varian-Cary 5G spectrophotometer. The fluorescence quantum yield measurements were performed using a Varian-Cary 5G spectrophotometer and a FluoroLog-3 spectrofluorometer. Spectral measurements were carried out in air-saturated acetonitrile solutions



Scheme 1 Synthesis of BChl, NI1–6 and BChl–NI.

(acetonitrile of spectrophotometric grade, water content < 0.005%, Aldrich) at  $20 \pm 1$  °C; the concentrations of the studied compounds were about  $0.5\text{--}2.0 \times 10^{-5}$  M. All measured fluorescence spectra were corrected for the nonuniformity of detector spectral sensitivity. Coumarin 481 in acetonitrile ( $\phi^{\text{fl}} = 0.08$ )<sup>51</sup> was used as a reference for the fluorescence quantum yield measurements. The fluorescence quantum yields were calculated by eqn (1),<sup>52</sup>

$$\phi^{\text{fl}} = \phi_{\text{R}}^{\text{fl}} \frac{S}{S_{\text{R}}} \cdot \frac{(1 - 10^{-A_{\text{R}}})n^2}{(1 - 10^{-A})n_{\text{R}}^2} \quad (1)$$

wherein  $\phi^{\text{fl}}$  and  $\phi_{\text{R}}^{\text{fl}}$  are the fluorescence quantum yields of the studied solution and the standard compound, respectively;  $A$  and  $A_{\text{R}}$  are the absorption of the studied solution and the standard respectively;  $S$  and  $S_{\text{R}}$  are the areas underneath the curves of the fluorescence spectra of the studied solution and the standard respectively; and  $n$  and  $n_{\text{R}}$  are the refraction indices of the solvents for the substance under study and the standard compound.

### Quantum yields of singlet oxygen generation

The quantum yields of singlet oxygen ( $\Phi_{\Delta}$ ) were estimated in acetone by using tetraphenylporphyrin (TPP) as a reference compound ( $\Phi_{\Delta}^{\text{TPP}} = 0.7$ )<sup>53,54</sup> and 1,3-diphenylisobenzofuran (DPBF) as an  $^1\text{O}_2$  trap. In a typical experiment, solutions (2.5 ml) containing both PSs (TPP and PS under study) and DPBF were placed into 1 cm rectangular spectroscopic cells and irradiated with monochromatic light (510 nm) using the excitation unit (a xenon lamp and excitation monochromator) of a FluoroLog-3 fluorometer. The initial concentration of DPBF corresponded to the absorption of about 1 at 414 nm ( $\sim 40$  mM). Identical initial DPBF concentrations were used for the reference solution of TPP and the samples. The change in DPBF absorption at 414 nm was recorded as a function of irradiation time *via* UV/Vis spectrometry. The values of  $\Phi_{\Delta}$  were calculated by eqn (2),

$$\Phi_{\Delta} = \Phi_{\Delta}^{\text{R}} \frac{V}{V_{\text{R}}} \cdot \frac{1 - 10^{-A_{\text{R}}}}{1 - 10^{-A}} \quad (2)$$

wherein  $V$  and  $V_{\text{R}}$  are the bleaching rates of the solutions containing PS under study ( $V$ ) and the reference compound ( $V_{\text{R}}$ ) which were found from the slopes of linear plots of absorption at 414 nm *versus* irradiation time;  $A$  and  $A_{\text{R}}$  are absorption values at an excitation wavelength (510 nm) of the solutions containing studied PS and the reference compound (TPP), respectively. The accuracy of  $\Phi_{\Delta}$  estimation was about 10%.

### Subpicosecond transient absorption setup

A Ti:sapphire laser system output (0.6 mJ and 30 fs at 800 nm and 1 kHz pulse repetition rate (Femtopower Compact Pro)) was split in two parts, producing the pump and the probe beams. 80% of pulses were used to pump an optical parametric generator (TOPAS (Light Conversion)) to generate the wavelength tuneable pump pulse. Following TOPAS, the harmonic generation or frequency mixing in a nonlinear crystal produced the excitation pulses in the range 250–2600 nm. The probe was a white light continuum pulse, extending from 390 nm to 900 nm, generated by focusing the 800 nm pulses ( $\sim 5$   $\mu\text{J}$  per pulse) into a 5 mm thick  $\text{D}_2\text{O}$  cell. The variable delay time between excitation and probe pulses was obtained by using a delay line with 0.1 mm resolution. The solutions were placed in a 1 mm circulating cell. A whitelight signal and reference spectra were recorded using a two-channel fiber spectrometer (Avantes Avaspec-2048-2). A home-written acquisition and experiment-control program in LabView made it possible to record transient spectra with an average error of less than  $10^{-3}$  of O.D. The temporal resolution of our setup was better than 60 fs. Temporal chirp of the probe pulse was corrected using a computer program with respect to a Lawrencian fit of a Kerr signal generated in a 0.2 mm glass plate used in place of the sample.

### Nanosecond transient absorption setup

A frequency tripled Nd:YAG amplified laser system (30 ps, 30 mJ@1064 nm, 20 Hz, Ekspla model PL 2143) output was used to pump an optical parametric generator (Ekspla model PG 401) producing tunable excitation pulses in the range 410–2300 nm.

The residual fundamental laser radiation was focused in a high pressure Xe filled breakdown cell where a white light pulse for sample probing was produced. All signals were analyzed using a spectrograph (Princeton Instruments Acton model SP2300) coupled with a high dynamic range streak camera (Hamamatsu C7700, 1 ns–1 ms). Accumulated sequences (sample emission, probe without and with excitation) of pulses were recorded and treated with HPDTA (Hamamatsu) software to produce two-dimensional maps (wavelength *versus* delay) of transient absorption intensity in the range 300–800 nm. The typical measurement error was better than  $10^{-3}$  O.D.

### Fluorescence imaging and procedure of photodynamic treatment of tumor cells

Human lung adenocarcinoma A549 cells were grown (37 °C, 5% CO<sub>2</sub>) in Eagle's minimum essential medium with phenol red, 8% fetal calf serum, 2 mM L-glutamine (so called complete medium). The cells were subcultured twice per week. On the day prior to an experiment, exponentially growing cells were plated on round cover glasses placed in 24-well plates (for microscopic experiments) or seeded directly in 96-well plates (for cytotoxicity measurements). The sowing density was  $5 \times 10^4$  cells per ml.

For microscopic experiments cells were incubated with 1–8  $\mu$ M of the **BChl-NI** conjugate for 1–3 h in a complete medium at 37 °C. Detailed intracellular distribution of the conjugate was studied using a Leica SP2 confocal laser scanning microscope (Leica, Germany). Conjugate fluorescence was excited with 488 nm (fits well to the absorption band of the **NI** chromophore) and 514 nm (fits well to the absorption band of the **BChl** chromophore) light. An emission in the 500–600 nm spectral range corresponding to the **NI** unit was registered using a photomultiplier. An emission in the range 730–1000 nm corresponding to PS was registered using a highly sensitive avalanche photodiode.

Intracellular formation of photoinduced reactive oxygen species (ROS) was measured using 2',7'-dichlorofluorescein diacetate (DCFDA). Cells were incubated with 1  $\mu$ M **BChl-NI** for 3 h and during last 30 min with 25  $\mu$ M DCFDA. Then cells were irradiated ( $22 \pm 2$  mW cm<sup>-2</sup>) with a halogen lamp (500 W) through a water filter (thickness of 5 cm) and a band-pass filter (transmission 660–1000 nm) for 15 min and analyzed by confocal microscopy. Fluorescence was excited with 488 nm and registered in the 500–540 nm (DCFDA) and 600–650 nm (**NI**) regions. Cells incubated with DCFDA and **BChl-NI** without irradiation as well as cells incubated with **BChl-NI** and irradiated without DCFDA were used as control.

To clarify the cellular mechanisms of **BChl-NI** transport, cells were thoroughly washed with a warm medium (37 °C) without serum, pre-incubated with chlorpromazine (30  $\mu$ M for 30 min), or methyl- $\beta$ -cyclodextrin (4 mM for 30 min) in a serum-deprived medium (37 °C) and further incubated in the presence of **BChl-NI** (4  $\mu$ M for 70 min) at 37 °C. To study the influence of temperature, cells were incubated with **BChl-NI** (4  $\mu$ M for 70 min) at 8 °C.

In the confocal microscopy measurements, lateral and axial resolutions were *ca.* 0.2 and 1.5  $\mu$ m, respectively. Confocal microspectroscopy studies were performed at 488 nm excitation using an experimental setup described elsewhere.<sup>55</sup>

For cell survival studies, the **BChl-NI** conjugate was added to cells (0.04–8  $\mu$ M with a two-fold increment). Control cells were incubated with equivalent concentrations of Cremophor EL. The cytotoxicity was estimated after incubation of cells with the conjugate or Cremophor EL alone for 6 h in the dark. The photoinduced cytotoxicity was measured on cells incubated with the conjugate or Cremophor EL alone for 3 h and irradiated as described above. After irradiation the cells were further incubated for 3 h and examined for viability. All the experiments were performed in duplicate. To evaluate cell viability, cells were stained with Hoechst 33342 (stains all cells) and propidium iodide (stains dead cells) and analyzed using a fluorescence microscope as described elsewhere.<sup>56,57</sup> Irradiation of control cells without **BChl-NI** did not induce any cytotoxicity under the irradiation conditions used.

## 3. Results and discussion

### Steady-state spectroscopic properties

Absorption and emission characteristics of the **BChl-NI** conjugate and monochromophoric derivatives **BChl** and **NI4** are presented in Fig. 1 and Table 1. As can be seen from Fig. 1a and c, the absorption spectrum of **BChl-NI** shows the presence of four bands with maxima at 354, 481, 515 and 747 nm corresponding to the electronic transitions in naphthalimide (481 nm) and bacteriochlorin (354, 515 and 747 nm) moieties. Although the position and intensity of characteristic Q and Soret bands of the bacteriochlorin core in the conjugate are essentially the same as those in the equimolar mixture of **BChl** and **NI4** (Fig. 1c), naphthalimide ICT absorption is observed at slightly higher wavelengths. This red shift could be attributed to the incorporation of an electron withdrawing triazole group in the *N*-butyl substituent of compound **NI4**, which enhances the ICT.

Fluorescence emission maxima of **BChl** and **NI4** appear at close  $\lambda$  values, however, the naphthalimide spectrum is much more broad and substantially drops into the IR region (Fig. 1b). In the case of equimolar mixture, excitation with 460 nm light which is mostly absorbed by **NI4** results in the emission band having the same feature as that of the individual naphthalimide dye but interfered with to some extent by the sharp collateral peak of the **BChl** fluorescence (Fig. 1d). Interestingly, the spectrum of the **BChl-NI** conjugate where two photoactive units are covalently linked is found to be different (Fig. 1d). Under excitation at 460 nm, **BChl-NI** demonstrates only the characteristic band of bacteriochlorin, whereas naphthalimide fluorescence is completely quenched. This observation implies that in the conjugate, efficient energy transfer from the naphthalimide to bacteriochlorin fragment may occur. To obtain deeper insight into the nature of processes in the excited state of the **BChl-NI** molecule we further studied transient absorption (TRABS) spectra of this system.

### Transient absorption spectroscopy

A representative result of a pump-probe experiment for **BChl-NI**, *i.e.* a map of absorbance changes after the laser pulse in delay-wavelength coordinates is displayed in Fig. 2a. The excitation of

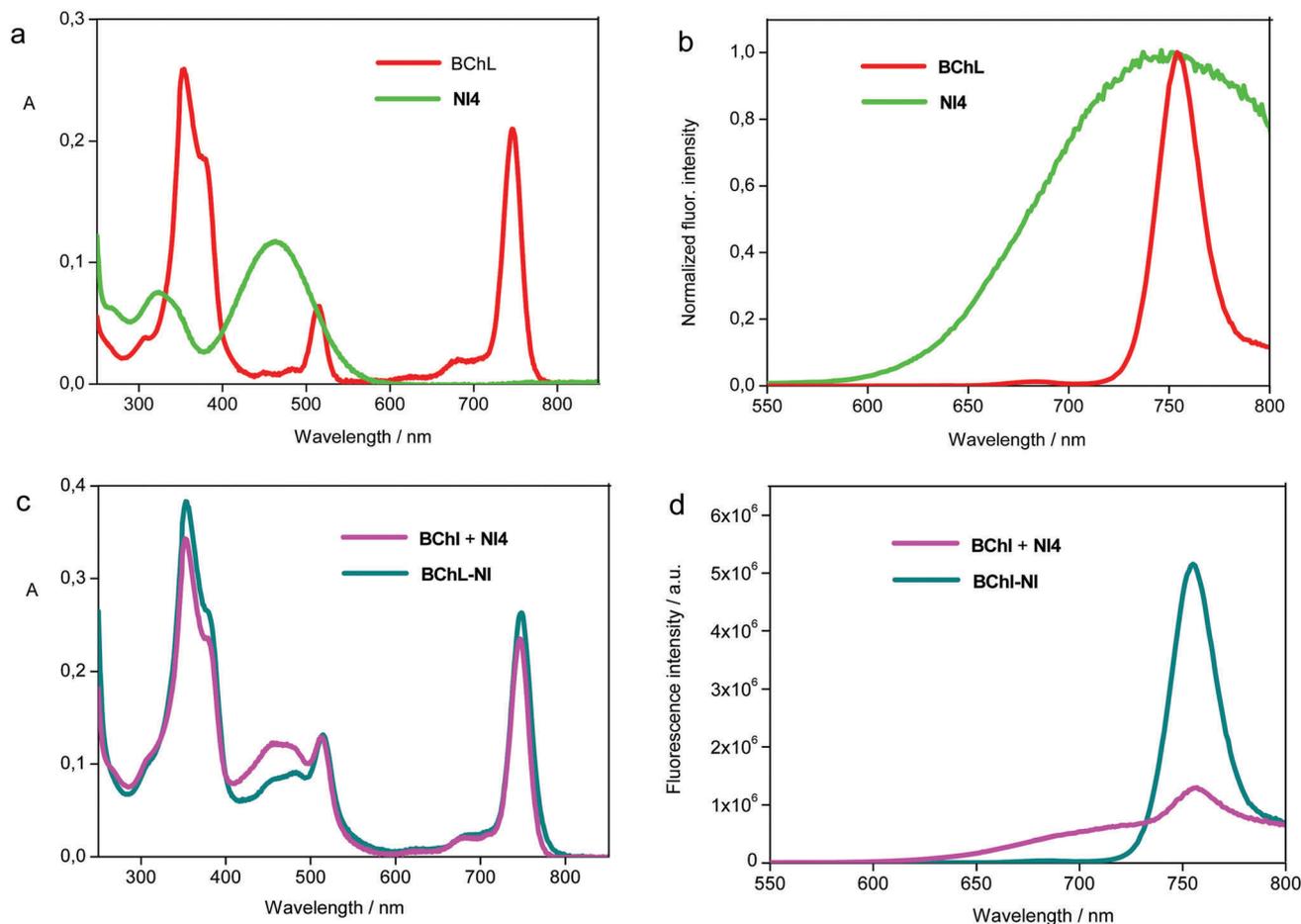


Fig. 1 UV/Vis absorption (a and c) and fluorescence emission (b and d) spectra of compounds **BChl**, **NI4**, **BChl-NI** and an equimolar mixture of **BChl** and **NI4** (denoted as “**BChl + NI4**”) in acetonitrile. The excitation wavelength is 460 nm for **NI4**, **BChl-NI**, **BChl + NI4** and 515 nm for **BChl**. Concentration of all compounds  $4.7 \times 10^{-6}$  M.

Table 1 Photophysical characteristics of compounds **BChl**, **NI** and **BChl-NI** in acetonitrile<sup>a</sup>

	$\lambda_{\max}^{\text{abs}}/\text{nm}$	$\lambda_{\max}^{\text{fl}}(\lambda_{\text{ex}})/\text{nm}$	$\varphi^{\text{fl}}$	Intramolecular RET in <b>BChl NI</b>					
				Förster theory		Experiment			
				$k_{\text{RET1}}/\text{s}^{-1}$	$\Phi_{\text{RET1}}$	$k_{\text{RET1}}/\text{s}^{-1}$	$\Phi_{\text{RET1}}$	$\Phi_{\text{RET2}}$	$\Phi_{\Delta}(\lambda_{\text{ex}}/\text{nm})$
<b>NI4</b>	462	743 (460)	0.032						
<b>BChl</b>	353; 515; 746	755 (515)	0.016						0.79 (510)
<b>BChl NI</b>	354; 481; 515; 747	755 (460)	0.023	$0.57 \times 10^{12}$	0.995	$1.89 \times 10^{12}$	0.999	0.981	0.82 (510)

<sup>a</sup> Quantum yield of generation of singlet oxygen ( $\Phi_{\Delta}$ ) is measured in acetone.

the naphthalimide chromophore with 470 nm light produced a negative signal at 750 nm. In accordance with the position of the long wavelength absorption band of **BChl** (Fig. 1a), this signal can be ascribed to the ground state bleaching of bacteriochlorin in the conjugate.‡ Another feature of the TRABS map shown in Fig. 1a is a broad positive band stretching from 500 to 680 nm.

‡ Apparently, the contribution of stimulated emission to the negative signal at 750 nm is relatively small, because of a high value of radiative lifetime ( $\tau_r$ ) of bacteriochlorin. Radiative lifetime is known to be the ratio of excited singlet state lifetime to the fluorescence quantum yield. From the data presented in Fig. 2 and Table 1,  $\tau_r = 2 \text{ ns}/0.016 = 125 \text{ ns}$ . Such a high  $\tau_r$  value explains low radiative rate constant ( $k_r = 1/\tau_r$ ) and low probability of stimulated emission as a result.

Probably, this spectral region covers the area where absorption signals of singlet ( $S_1$ ) states of both chromophores are located. One can also see that the appearance of a negative band on a time scale occurs not immediately after the excitation pulse and proceeds with a characteristic time of 0.53 ps as obtained from the TRABS time profile (Fig. 2b).§ Hence, the initially formed

§ Characteristic time  $\tau_2 = 4.1 \text{ ps}$  shown in Fig. 2b describes the relaxation of the singlet excited state of bacteriochlorin. Probably, the positive signal of  $S_1 \rightarrow S_n$  absorption has non zero intensity at around 750 nm which tends to decrease upon increasing time delay. Thus, the negative signal at 750 nm is becoming more and more negative even after the fast process with  $\tau_1 = 0.53 \text{ ps}$  is completed.

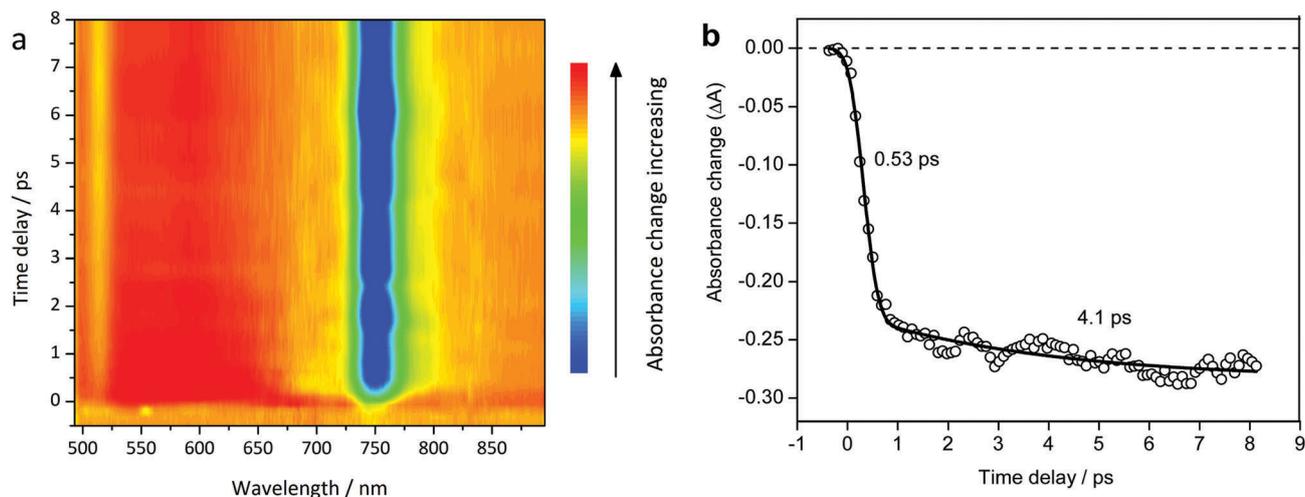


Fig. 2 TRABS spectral map with subpicosecond time resolution (a) and TRABS kinetics at 750 nm (b) of **BChl-NI** in acetonitrile. Excitation wavelength 470 nm.

naphthalimide excited state should participate in a kind of fast non-radiative process more likely to be the resonance energy transfer (RET). The rate constant of RET ( $k_{\text{RET1}}$ ) can be estimated from the known characteristic time as  $1/0.53 \times 10^{-12}$  s (see Table 1 for the value of  $k_{\text{RET1}}$ ). Quantum efficiency of intramolecular RET ( $\Phi_{\text{RET1}}$ ) is expressed as the ratio of  $k_{\text{RET1}}$  to the sum of rate constants of all other possible processes in the  $S_1$  state of a donor:

$$\Phi_{\text{RET1}} = \frac{k_{\text{RET1}}}{k_{\text{RET1}} + k_r + k_{\text{nr}}} = \frac{k_{\text{RET1}}}{k_{\text{RET1}} + \tau_{\text{D},0}^{-1}} \quad (3)$$

In eqn (3)  $k_r$  is the radiative rate constant of the naphthalimide chromophore, and  $k_{\text{nr}}$  describes its non-radiative relaxation which is not related to energy transfer. To estimate the sum ( $k_r + k_{\text{nr}}$ ) we used the value inversely proportional to the fluorescence lifetime of compound **NI4** ( $\tau_{\text{D},0} = 0.38$  ns),<sup>44</sup> where the RET process is not realized. The obtained value of  $\Phi_{\text{RET1}}$  was found to be close to unity (Table 1) indicating a highly efficient RET in the **BChl-NI** conjugate. Additionally, calculations of  $k_{\text{RET1}}$  and  $\Phi_{\text{RET1}}$  by the Förster model<sup>58</sup> testify to the same result. The details of these calculations are shown in the ESI.†

Further evolution of TRABS signals of the bacteriochlorin unit in **BChl-NI** can be followed by using the spectral map with nanosecond resolution (Fig. 3a). The horizontal cuts of this map at a given time delay give us the TRABS spectra at these delays. The spectrum immediately after excitation is shown in blue in Fig. 3b. In this spectrum, we can see a broad absorption band of the bacteriochlorin singlet state (several  $S_1 \rightarrow S_n$  transitions could contribute) in the range of 400–650 nm formed as a result of energy transfer¶ and negative features at 515 and 700 nm corresponding to the ground state bleaching. Kinetics of absorption at 600 nm (Fig. 3c) clearly shows that the  $S_1$  state relaxes within 2 ns at which it converts to some long-lived species presumably regarded as triplets. Thus, the

¶ Energy transfer process is not visible in this map; it can be perceived with the aid of the subpicosecond experiment described above.

spectrum after 40 ns (Fig. 3b, red line) shows us the absorption of the  $T_1$  state.

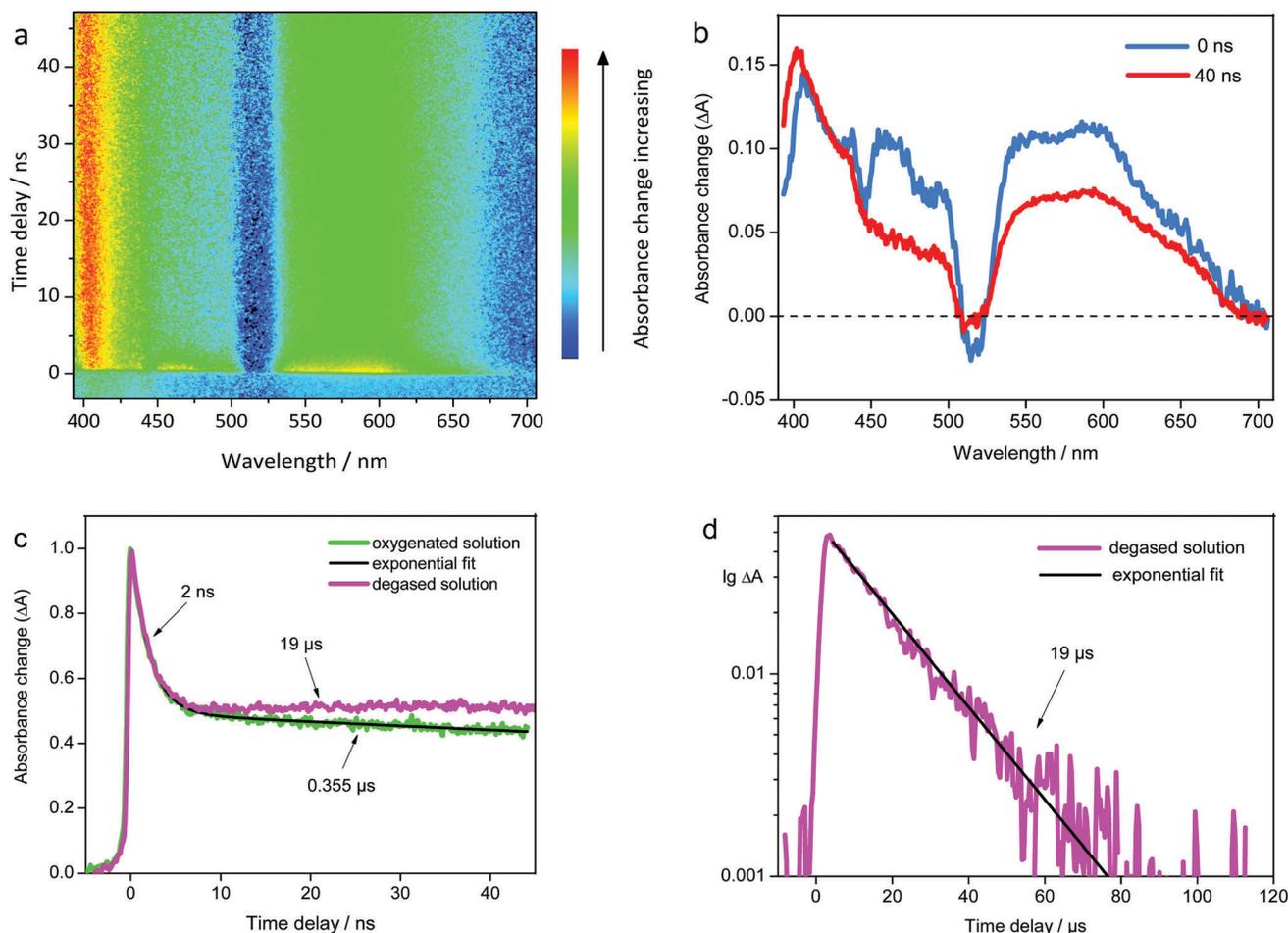
The lifetime of the bacteriochlorin triplet state was found to be dramatically affected by the presence of oxygen. Whereas the degassed solution exhibited single exponential decay with a time constant of 19  $\mu\text{s}$  ( $\tau_T$ ), in the case of an air saturated sample, the observed lifetime was 0.355  $\mu\text{s}$  ( $\tau_T^{\text{O}_2}$ ) (Fig. 3c and d). Considering the difference in  $\tau_T$  and  $\tau_T^{\text{O}_2}$  values, one can conclude that the excitation energy is transferred from the PS unit to molecular oxygen upon collisions which leads to the formation of  $^1\text{O}_2$  and PS in the ground state. The efficiency of this process given as  $\Phi_{\text{RET2}}$  was calculated by eqn (4).

$$\Phi_{\text{RET2}} = 1 - \frac{\tau_T^{\text{O}_2}}{\tau_T} \quad (4)$$

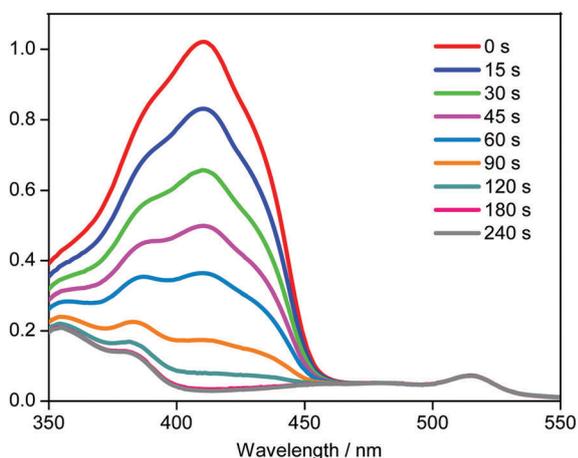
As evident from the obtained value of  $\Phi_{\text{RET2}}$  (0.981, see Table 1), bacteriochlorin in **BChl-NI** works as an excellent photosensitizer allowing the generation of  $^1\text{O}_2$  with a high quantum yield.

### Photosensitizing activity

Singlet oxygen ( $^1\text{O}_2$ ) is thought to be a key cytotoxic agent in the photodynamic inactivation of living cells.<sup>59,60</sup> It is formed as a result of energy transfer from the photosensitizer triplet state to molecular oxygen. Photosensitized  $^1\text{O}_2$  formation was studied using 1,3-diphenylisobenzofuran (DPBF) as a singlet oxygen trap. Interaction of DPBF with  $^1\text{O}_2$  is known to be purely chemical, resulting in the formation of colorless endoperoxides.<sup>53,54</sup> This process causes bleaching of the main maximum of DPBF at 414 nm. Fig. 4 illustrates one of the experiments on photosensitized bleaching of DPBF in a solution of the **BChl-NI** conjugate in acetone under illumination with green (510 nm) light which is absorbed by both chromophores. Rapid photobleaching of DPBF was also detected in the solution of free bacteriochlorin **BChl** (Fig. S24, ESI†). This observation is consistent with the results of previous studies which showed that metal-free bacteriochlorins efficiently photosensitized



**Fig. 3** TRABS spectral map (a) with nanosecond time resolution, TRABS spectra at different time delays (b) and TRABS kinetic curves at 600 nm in the presence and absence of oxygen (c and d) of **BChl-NI** in acetonitrile. Excitation wavelength = 440 nm. Spectral map has a negative perturbed signal at 440 nm induced by the filter rejecting this wavelength.



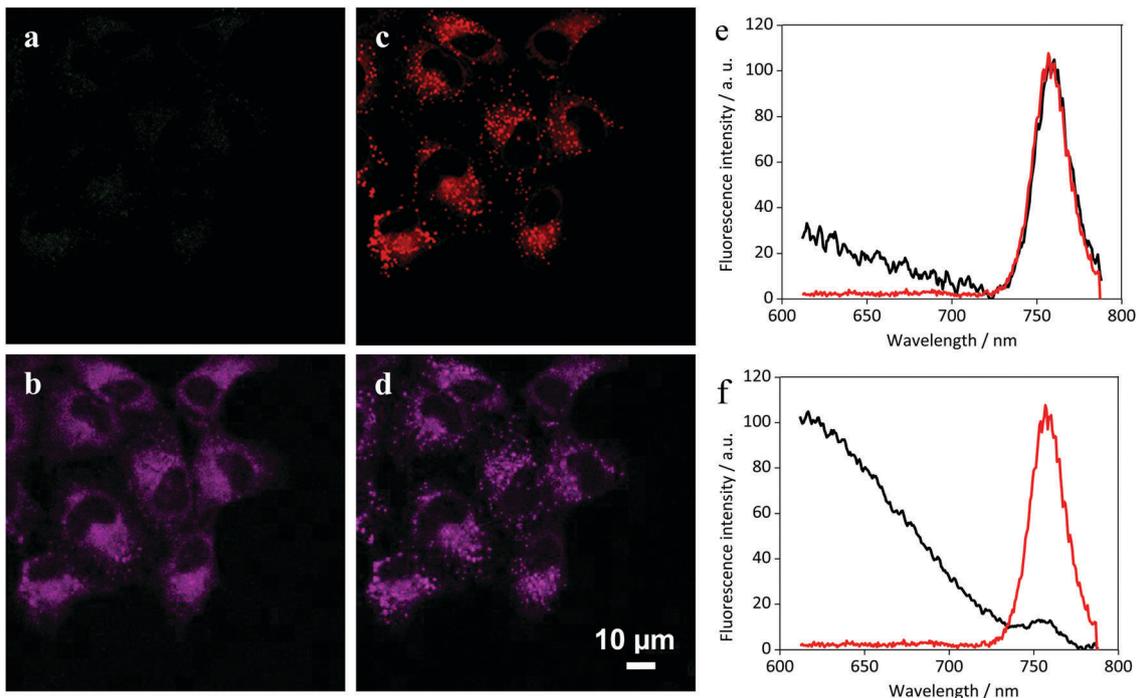
**Fig. 4** Changes in the UV/Vis absorption spectrum of a mixed solution containing the **BChl-NI** conjugate ( $2.6 \times 10^{-6}$  M) and DPBF ( $4.0 \times 10^{-5}$  M) in acetone upon irradiation at 510 nm.

singlet oxygen formation in air saturated solutions.<sup>61,62</sup> In solution of the free naphthalimide dye, photobleaching of the trap was not

found (Fig. S25, ESI<sup>†</sup>). The quantum yields of singlet oxygen production of **BChl** and **BChl-NI** under excitation at 510 nm were found to be 0.79 and 0.82, respectively (Table 1). Such close values indicate that photosensitizing activity of the naphthalimide dye in the conjugate is, apparently, caused by efficient energy transfer from the dye to the bacteriochlorin, which is in good agreement with the above time-resolved studies of **BChl-NI**, and the presence of the naphthalimide fragment in **BChl-NI** does not decrease the ability of the PS core to generate  $^1\text{O}_2$ .

#### ***In vitro* studies of the BChl-NI conjugate**

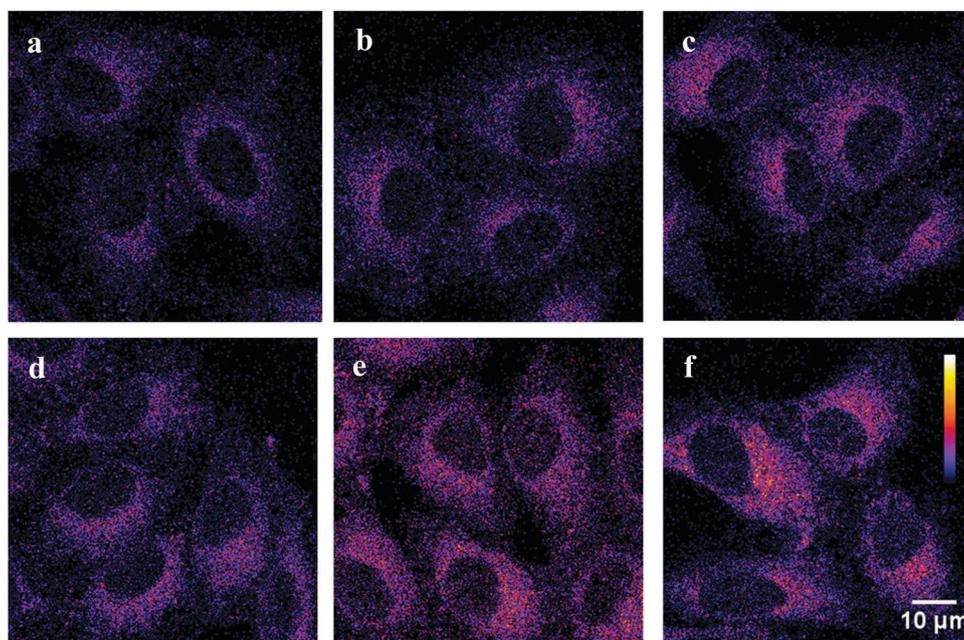
As confirmed by confocal microspectroscopy and confocal laser scanning microscopy, the conjugate penetrates into cancer A549 cells (Fig. 5 and 6). Intracellular fluorescence spectra of **BChl-NI** were recorded by confocal microspectroscopy with the 488 nm excitation wavelength, which fitted well to the absorption band of the **NI** moiety of the conjugate. A typical intracellular emission spectrum of **BChl-NI** is shown in Fig. 5e. Its shape and long-wavelength maximum (757 nm) correspond to the fluorescence of the bacteriochlorin moiety. Intense illumination of a cell with the 488 nm light leads to the changes in the



**Fig. 5** Intracellular distribution of **BChl-NI** fluorescence in A549 cells. Distribution of fluorescence in the 550–650 nm (a and c) and >730 nm (b and d) ranges at the low power 488 nm excitation before (a and b) and after (c and d) the high power prolonged illumination (photobleaching) of cells with the 488 nm wavelength. (e and f) Examples of intracellular fluorescence spectra of **BChl-NI** (black line) at the 488 nm excitation before (e) and after (f) the high power prolonged illumination (photobleaching) of cells. Red line—fluorescence spectrum of **Bchl** in 1% Chremophor EL solution. Spectra are normalized to the highest intensity. Cells were incubated with 2  $\mu\text{M}$  of **BChl-NI** for 3 h.

intracellular fluorescence spectra of **BChl-NI**: a band with the 757 nm maximum disappears due to photobleaching of the acceptor (**BChl**), and donor (**NI**) fluorescence is restored, which

has a maximum at *ca.* 600 nm (Fig. 5f). These changes confirm RET between **NI** and **BChl** chromophores in cells and show that the polarity of the cellular microenvironment is similar to the



**Fig. 6** Intracellular accumulation of **BChl-NI** in A549 cells. Confocal fluorescent images describing the intracellular distribution of the conjugate based on the bacteriochlorin fluorescence (excitation 514 nm, emission >730 nm). Cells were incubated with 2 (a and d), 4 (b and e), 8 (c and f)  $\mu\text{M}$  conjugate for 1 h (a–c) or 3 h (d–f).

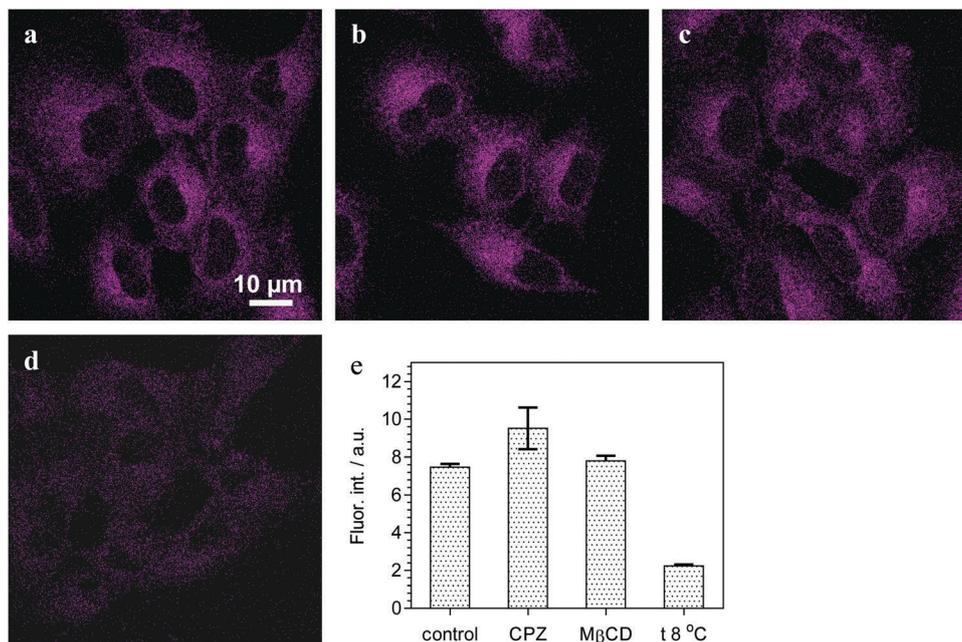


Fig. 7 Study of mechanisms of intracellular penetration of **BChl-NI**. (a-d) Confocal fluorescent images showing the intracellular distribution of **BChl-NI** in control cells (a), cells pre incubated with 30  $\mu\text{M}$  chlorpromazine (b) or 4 mM methyl  $\beta$  cyclodextrin for 30 min (c) or in the cells at 8  $^{\circ}\text{C}$  (d). (e) Comparison of average intracellular fluorescence intensities of **BChl-NI** in incubation regimes depicted in (a-d): CPZ, M $\beta$ CD treatment with chlorpromazine or methyl  $\beta$  cyclodextrin, respectively. Cells were incubated with 4  $\mu\text{M}$  **BChl-NI** for 70 min at 37  $^{\circ}\text{C}$  (a-c) or 8  $^{\circ}\text{C}$  (d).

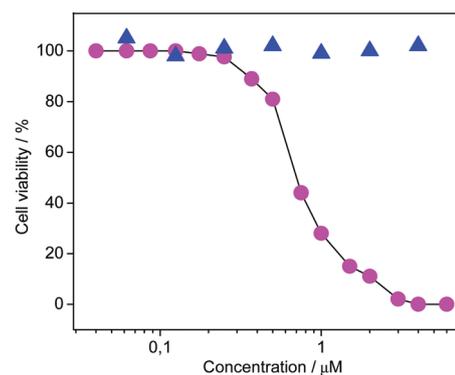
polarity of diethyl ether solution ( $\epsilon = 4.3$ ), where the **NI** chromophore has a fluorescence maximum at 608 nm.<sup>44</sup>

In agreement with microspectroscopy studies, confocal laser scanning microscopy reveals intracellular fluorescence of **BChl-NI** in the range of 730 nm and longer wavelengths (at the excitation of 488 or 514 nm) and the absence of fluorescence in the 500–650 nm range (Fig. 5a and b). As clearly seen (Fig. 5b and 6), the conjugate accumulates in the cytoplasm of A549 cells and does not penetrate into the nucleus. In the cytoplasm, **BChl-NI** has diffuse distribution. The pattern of intracellular distribution is similar at different extracellular concentrations of **BChl-NI** and different incubation times of cells with the conjugate (Fig. 6). An increase in the extracellular concentration of the conjugate from 2 to 8  $\mu\text{M}$  and incubation time from 1 to 3 h increases moderately intracellular fluorescence that indicates saturation of intracellular accumulation of **BChl-NI** at concentrations higher than 4  $\mu\text{M}$  and an incubation time of 3 h.

Intense prolonged illumination of cells with 488 nm or 514 nm light leads to the appearance of fluorescence in the 500–650 nm range due to photobleaching of the **BChl** chromophore. In the course of photobleaching, the distribution of

intracellular fluorescence becomes granular (Fig. 5c and d) as a result of photodynamic (phototoxic) processes induced in cells.

To study the mechanism of **BChl-NI** penetration into cells, the known inhibitors of clathrin-dependent (chlorpromazine) and caveolae-dependent (methyl- $\beta$ -cyclodextrin) endocytosis<sup>63</sup> were used. It was found that intracellular penetration of **BChl-NI** was not inhibited, when cells were pre-treated with chlorpromazine (an inhibitor, which induces dissociation of clathrin from a cell surface) (Fig. 7b) or with methyl- $\beta$ -cyclodextrin (a compound that depletes plasma membrane cholesterol) (Fig. 7c). Therefore, clathrin-dependent or caveolae-dependent endocytosis



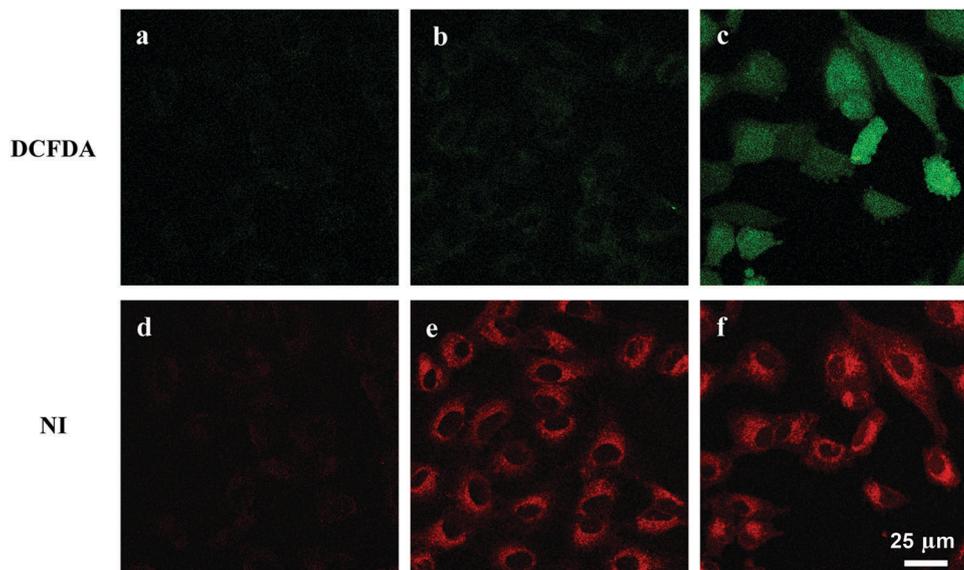


Fig. 9 Verification of light induced ROS formation in cells using DCFDA. Confocal fluorescence images show distribution of DCFDA (a c) and **NI** moiety (d f) fluorescence in the irradiated A549 cells. Fluorescence was excited at 488 nm and registered in the 500–540 nm (DCFDA, green) and 600–650 nm (**NI**, red). (a and d) Cells were incubated with DCFDA but without **BChl-NI** and irradiated with red light. (b and e) Cells were incubated with **BChl-NI** but without DCFDA and irradiated. (c and f) Cells were incubated with **BChl-NI** and DCFDA and irradiated.

pathways are not noticeably involved in **BChl-NI** uptake into A549 cells. A decrease in incubation temperature from 37 to 8 °C led to a threefold decrease in **BChl-NI** intracellular accumulation (Fig. 7d and e). This effect can be explained by a passive diffusion of **BChl-NI** through the plasma membrane, which is affected by a decrease in membrane fluidity at a low temperature.

The studies showed that the **BChl-NI** conjugate was not toxic for A549 cells at tested concentrations ( $<8 \mu\text{M}$ , Fig. 8) without light-induced activation. At the same time, the concentration-dependent killing of cells (Fig. 8) was observed upon irradiation with red light. Under the used conditions, the photodynamic effect was achieved through the excitation of the bacteriochlorin moiety. Conjugate concentrations that provide 90% and 50% photoinduced cell death are  $0.70 \pm 0.05$  and  $0.33 \pm 0.05 \mu\text{M}$ , respectively. These data indicate that the conjugate is an active photosensitizer, and its further investigation for anticancer photodynamic therapy is warranted.

To confirm the formation of reactive oxygen species (ROS) in cells under irradiation, cells were incubated with both DCFDA and **BChl-NI** and irradiated with red light (Fig. 9). In viable cells, DCFDA undergoes deacetylation to non-fluorescent 2',7'-dichlorofluorescein. This compound reacts quantitatively with ROS in cells and produces the fluorescent dye 2',7'-dichlorofluorescein. DCFDA is known to be very reactive with peroxides but can also be oxidized by other ROS.<sup>64</sup> Bright fluorescence of DCFDA and the **NI**-moiety was observed in the cytoplasm after irradiation (Fig. 9c and f). The appearance of DCFDA fluorescence indicates ROS generation during irradiation of cells. No fluorescence of DCFDA and **NI** was detected in control cells without irradiation (data not shown). No fluorescence of DCFDA was observed in cells incubated with DCFDA but without **BChl-NI** and irradiated (Fig. 9a) thus confirming

again that **BChl-NI** does produce ROS during irradiation with red light.

## 4. Conclusions

In summary, we have prepared a novel bacteriochlorin-naphthalimide conjugate **BChl-NI**. A steady-state and time-resolved spectroscopic study of **BChl-NI** in solution has shown that the presence of the **NI** fragment does not decrease the photosensitizing activity of **BChl**; however the fluorescence of naphthalimide is quenched due to efficient resonance energy transfer. *In vitro* results revealed high photoinduced cytotoxicity and fluorescence imaging capability that can be realized using both chromophores. Far-red absorption and fluorescence of the **BChl** moiety make this conjugate suitable for photodynamic treatment of deeply located tumors as well as for fluorescence imaging and navigation *in vivo*. At the same time far-red fluorescence of the conjugate is poorly detectable in cellular studies, since conventional confocal microscopes equipped with photomultiplier-based detection systems have low sensitivity in the 700–900 nm spectral range. Accordingly, photoinduced magenta-to-red\*\* conversion of fluorescence can facilitate

\*\* We used confocal laser scanning microscopy to visualize the intracellular distribution of the **BChl-NI** conjugate. Fluorescence was registered using a highly sensitive avalanche photodiode or a photomultiplier. Both detectors record the intensity of emitted light in each point of a scanned specimen and do not recognize color (wavelength) of detected photons. Color of the image is selected by a scientist using palettes, which are available in software. In order to provide better color reproduction, we chose red color for **NI** emission in Fig. 5c. Fluorescence of the **BChl** moiety has wavelengths that are not visible to the human eye. We decided to use dark magenta color for this fluorescence in the presented images.

visualization of the conjugate in cellular studies. Moreover, this color conversion of **BChI-NI** fluorescence could be a useful indicator of integrity of the photosensitizer moiety during irradiation of cancer cells and can help in optimizing the power and dose of light during photodynamic treatment. Thus, the newly synthesized conjugate **BChI-NI** is a good candidate for the next-generation “bifunctional” photosensitizer allowing PDT and fluorescence diagnostics to be performed.

## Conflicts of interest

There are no conflicts to declare.

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