

# Somatosensory Event-related Potentials from Orofacial Skin Stretch Stimulation

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1 **TITLE:**  
2 Somatosensory event-related potentials from orofacial skin stretch stimulation  
3

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41 **KEYWORDS:**

42 Cutaneous mechanoreceptors, speech perception, speech production, sensorimotor control,  
43 electroencephalography  
44

45 **SHORT ABSTRACT:**

46 This paper introduces a method for obtaining somatosensory event-related potentials following  
47 orofacial skin stretch stimulation. The current method can be used to evaluate the contribution  
48 of somatosensory afferents to both speech production and speech perception.

49

50 **LONG ABSTRACT:**

51 Cortical processing associated with orofacial somatosensory function in speech has received  
52 limited experimental attention due to the difficulty of providing precise and controlled  
53 stimulation. This article introduces a technique for recording somatosensory event-related  
54 potentials (ERP) that uses a novel mechanical stimulation method involving skin deformation  
55 using a robotic device. Controlled deformation of the facial skin is used to modulate kinesthetic  
56 inputs through excitation of cutaneous mechanoreceptors. By combining somatosensory  
57 stimulation with electroencephalographic recording, somatosensory evoked responses can be  
58 successfully measured at the level of the cortex. Somatosensory stimulation can be combined  
59 with the stimulation of other sensory modalities to assess multisensory interactions. For  
60 speech, orofacial stimulation is combined with speech sound stimulation to assess the  
61 contribution of multi-sensory processing including the effects of timing differences. The ability  
62 to precisely control orofacial somatosensory stimulation during speech perception and speech  
63 production with ERP recording is an important tool that provides new insight into the neural  
64 organization and neural representations for speech.

65

66 **INTRODUCTION:**

67 Speech production is dependent on both auditory and somatosensory information. The  
68 auditory and somatosensory feedback occur in combination from the earliest vocalizations  
69 produced by an infant and both are involved in speech motor learning. Recent results suggest  
70 that somatosensory processes contribute to perception as well as production. For example, the  
71 identification of speech sounds is altered when a robotic device stretches the facial skin as  
72 participants listen to auditory stimuli<sup>1</sup>. Air puffs to the cheek that coincide with auditory speech  
73 stimuli alter participants' perceptual judgments<sup>2</sup>.

74

75 These somatosensory effects involve the activation of cutaneous mechanoreceptors in  
76 response to skin deformation. The skin is deformed in various ways during movement, and  
77 cutaneous mechanoreceptors are known to contribute to kinesthetic sense<sup>3,4</sup>. The kinesthetic  
78 role of cutaneous mechanoreceptors is demonstrated by recent findings<sup>5-7</sup> that the movement-  
79 related skin strains are appropriately perceived as flexion or extension motion depending on  
80 the pattern of skin stretch<sup>6</sup>. Over the course of speech motor training, which is the repetition of  
81 specific speech utterance with concomitant facial skin stretch speech, articulatory patterns  
82 change in an adaptive manner<sup>7</sup>. These studies indicate that modulating skin stretch during  
83 action provides a method for assessing the contribution of cutaneous afferents to the  
84 kinesthetic function of the sensorimotor system.

85

86 The kinesthetic function of orofacial cutaneous mechanoreceptors has been studied mostly  
87 using psychophysiological methods<sup>7,8</sup> and microelectrode recoding from sensory nerves<sup>9,10</sup>.  
88 Here, the current protocol focuses on the combination of orofacial somatosensory stimulation

89 associated with facial skin deformation and event related potential (ERP) recording. This  
90 procedure has precise experimental control over the direction and timing of facial skin  
91 deformation using a computer-controlled robotic device. This allows us to test specific  
92 hypotheses about the somatosensory contribution to speech production and perception by  
93 selectively and precisely deforming facial skin in a wide range of orientations during both  
94 speech motor learning and directly in speech production and perception. ERP recording are  
95 used to noninvasively evaluate the temporal pattern and timing of the influence of  
96 somatosensory stimulation on orofacial behaviors. The current protocol then can evaluate the  
97 neural correlates of kinesthetic function and assess the contribution of the somatosensory  
98 system to both speech processing, speech production and speech perception.

99  
100 To show the utility of the application of skin stretch stimulation to ERP recording, the following  
101 protocol focuses on the interaction of somatosensory and auditory input in speech perception.  
102 The results highlight a potential method to assess somatosensory-auditory interaction in  
103 speech.

104

#### 105 **PROTOCOL:**

106

107 The current experimental protocol follows the guidelines of ethical conduct according to the  
108 Yale University Human Investigation Committee.

109

#### 110 **1. Electroencephalography (EEG) preparation**

111

112 1.1. Measure head size to determine the appropriate EEG cap.

113

114 1.2. Identify the location of the vertex by finding the mid-point between nasion and inion  
115 with a measuring tape.

116

117 1.3. Place the EEG cap on the head using the pre-determined vertex as Cz. Examine Cz again  
118 after placing the cap by using a measuring tape as done in 1.2. Note that the EEG cap is  
119 equipped with electrode holders and the placement of the 64 electrodes (or holders) is based  
120 on a modified 10-20 system with pre-specified coordinates system based on Cz<sup>11</sup>. This  
121 representative application uses a 64 electrode configuration to assess scalp distribution  
122 changes and for source analysis. For simpler applications (event-related potential changes in  
123 amplitude and latency) using fewer electrodes are possible. There are two additional electrodes  
124 for ground in the EEG system used here. Those electrode holders are also included in the cap.

125

126 1.4. Apply electrode gel in the electrode holders using a disposable syringe.

127

128 1.5. Attach EEG electrodes (including ground electrodes) into the electrodes holders  
129 matching the labels of the electrodes and to the electrode holders on the electrode cap.

130

131 1.6. Clean the skin surface with alcohol pads.

132

133 Note: For electrodes for detecting eye motion (electro-oculography), the skin locations are  
134 above and below the right eye (vertical eye motion), and lateral to the outer canthus of the  
135 both eyes (horizontal eye motion); for somatosensory stimulation the skin lateral to the oral  
136 angle is cleaned.

137

138 1.7. Fill the four electro-oculography electrodes with the electrode gel and secure the  
139 electrodes with double-sided tape to the sites noted in 1.6.

140

141 1.8. Secure all electrode cables using a Velcro strap. If required, tape the cables to  
142 participant's body or the other locations that do not introduce any additional electrical or  
143 mechanical noise.

144

145 1.9. Position the participant in front of the monitor and the robot for somatosensory  
146 stimulation. Secure all electrode cables again as in 1.8.

147

148 1.10. Connect the EEG and electro-oculography electrodes (including the ground electrodes)  
149 into the appropriate connectors (matching label and connector shape) on the amplifier box of  
150 EEG system.

151

152 1.11. Check to see that the EEG signals are artifact free and that the offset value is in an  
153 acceptable range ( $< 50 \mu\text{V}$  or smaller). If noisy signals or large offsets that are usually indicative  
154 of high impedance are found, correct those electrode signals by adding additional EEG gel  
155 and/or repositioning hair that is directly under the electrode.

156

157 1.12. Insert the EEG-compatible earphones and confirm that the sound level is in a  
158 comfortable range based on subject report.

159

## 160 **2. Somatosensory stimulation**

161

162 Note: The current protocol applies facial skin stretch for the purpose of somatosensory  
163 stimulation. The experimental setup with the EEG system is represented in Figure 1. The details  
164 of the somatosensory stimulation device have been described in the previous studies<sup>1,7,12-14</sup>.  
165 Briefly, two small plastic tabs (2 cm wide and 3 cm height) are attached with double-sided tape  
166 to the facial skin. The tabs are connected to the robotic device using string. The robot generates  
167 systematic skin stretch loads according to experimental designs. The setup protocol for ERP  
168 recording is as follows:

169

170 2.1. Place the participants head in the headrest in order to minimize head motion during  
171 stimulation. Remove carefully the electrode cables between the participant's head and  
172 headrest.

173

174 2.2. Ask the participant to hold the safety switch for the robot.

175

176 2.3. Attach plastic tabs to the target skin location using double-sided tape for somatosensory

177 stimulation. For the representative results<sup>12,13</sup>, in which the target is the skin lateral to the oral  
178 angle, place the center of the tabs on the modiolus, a few mm lateral to the oral angle with the  
179 center of the tabs at approximately the same height of the oral angle.  
180

181 2.4. Adjust the configuration of the string, string supports and the robot in order to avoid  
182 EEG electrodes and cables.

183  
184 2.5. Apply a few facial skin stretches (one cycle sinusoid at 3 Hz with a maximum force of 4  
185 N) to check for artifacts due to the stimulation (usually observed as relatively large amplitude  
186 and lower frequency compared with the electrophysiological response). If artifacts are  
187 observed in the EEG signals, go back to 2.4.

### 188 189 3. ERP recording

190  
191 3.1. Explain the experimental task to the subject and provide a few practice trials.

192  
193 Note: The experimental task and stimulus presentation for ERP recording are preprogramed in  
194 software for stimulus presentation.

195  
196 3.1.1. In the representative test with combined somatosensory and auditory stimulation<sup>12</sup>,  
197 apply the somatosensory stimulation associated with skin deformation to the skin lateral to the  
198 oral angle. The pattern of stretch is a one cycle sinusoid (3 Hz) with a maximum force of 4 N. A  
199 single synthesized speech utterance that is midway in a 10-step sound continuum between  
200 "head" and "had" is used for auditory stimulation.

201  
202 3.1.2. Present both stimulations separately or in combination. In the combined stimulation,  
203 test three onset timings (90 ms lead and lag, and simultaneous in somatosensory and auditory  
204 onsets: see Figure 3A).

205  
206 3.1.3. Randomize the presentation of five stimulations (somatosensory alone, auditory alone  
207 and three combined: lead, simult. and lag). Vary the inter-trial interval between 1000 and 2000  
208 ms in order to avoid anticipation and habituation. The experimental task is to identify whether  
209 the presented speech sound, which is the sound that is acoustically intermediate between  
210 "head" and "had", was "head" by pressing a key on a keyboard. In the somatosensory alone  
211 condition, in which there is no auditory stimulation, the participants are instructed to answer  
212 not "head".

213  
214 3.1.4. Record participant judgments and the reaction time from the stimulus onset to the key  
215 press using the software for stimulus presentation. Ask the participant to gaze a fixation point  
216 on the display screen in order to reduce artifacts due to eye-movement.

217  
218 3.1.5. Remove the fixation point every 10 stimulations for a short break. (See also other  
219 example of task and stimulus presentation<sup>12,13</sup>)

220

221 3.2. Start the software for ERP recording at 512 Hz sampling, which also records the onset  
222 time of stimulation in the timeline of ERP data. Note that the time stamps of the stimulation,  
223 which also includes the information about the type of the stimulation, are sent for every  
224 stimulus from the software for stimulus presentation. The two programs (for ERP recording and  
225 for the stimulus presentation) are running on two separate PCs that are connected through a  
226 parallel port.

227  
228 3.3. Set the software for the somatosensory stimulation to the trigger-waiting mode and  
229 then start stimulus presentation by activating the software for stimulus presentation. Note that  
230 the software for the somatosensory stimulation is also running on a separate PC from the other  
231 two PCs. A trigger signal for the somatosensory stimulation is received through an analog input  
232 device that is connected to a digital output device in the PC for sensory stimulation. Single  
233 somatosensory stimulation is produced per one trigger. Record 100 ERPs per condition.

234

### 235 **REPRESENTATIVE RESULTS:**

236 This section presents representative event-related potentials in response to somatosensory  
237 stimulation resulting from facial skin deformation. The experimental setup is represented in  
238 Figure 1. Sinusoidal stimulation was applied to the facial skin lateral to the oral angle (See  
239 Figure 3A as reference). One hundred stretch trials were recorded for each participant with 12  
240 participants tested in total. After removing the trials with blinks and eye movement artifacts  
241 offline on the basis of the horizontal and vertical electro-oculography signals (over  $\pm 150 \mu\text{V}$ ),  
242 more than 85% of trials were averaged. EEG signals were filtered with a 0.5– 50 Hz band-pass  
243 filter and re-referenced to the average across all electrodes. Figure 2 shows the average  
244 somatosensory ERP from selected representative electrodes. In frontal regions, peak negative  
245 potentials were induced at 100-200 ms post stimulus onset followed by a positive potential at  
246 200-300 ms. The largest response was observed in the midline electrodes. Different from the  
247 previous studies of somatosensory ERP<sup>15-18</sup>, there is no earlier latency ( $< 100\text{ms}$ ) potentials. This  
248 temporal pattern is rather similar to the typical N1-P2 sequence following auditory  
249 stimulation<sup>19</sup>. In comparison between the corresponding pair of electrodes in left and right  
250 hemisphere, the temporal pattern is quite similar probably due to the bilateral stimulation.

251

252 *[Place Figure 1 and 2 here]*

253

254 The first result shows how the timing of stimulation affects multisensory interaction during  
255 speech processing<sup>12</sup>. In this study, neural response interactions were found by comparing ERPs  
256 obtained using somatosensory–auditory stimulus pairs with the algebraic sum of ERPs to the  
257 unisensory stimuli presented separately. The pattern of auditory-somatosensory stimulations  
258 are represented in Figure 3A. Figure 3B shows the pattern of event-related potentials in  
259 response to somatosensory-auditory stimulus pairs (Red line). The black line represents the  
260 sum of individual unisensory auditory and somatosensory ERPs. The three panels correspond to  
261 the time lag between two stimulus onsets: 90 ms lead of the somatosensory onset (Left),  
262 simultaneous (Center) and 90 ms lag (Right). When somatosensory stimulation was presented  
263 90 ms before the auditory onset, there is a difference between paired and summed responses  
264 (the left panel in Figure 3B). This interaction effect gradually decreases as a function of the time

265 lag between the somatosensory and auditory inputs (see the change between the two dotted  
266 lines in Figure 3B). The results demonstrate that the somatosensory-auditory interaction is  
267 dynamically modified with the timing of stimulation.

268

269 *[Place Figure 3 here]*

270

271 The next result demonstrates that the amplitude of the somatosensory ERP increases in  
272 response to listening to speech<sup>13</sup>. The pattern of somatosensory stimulation is the same as  
273 noted above. Figure 4 shows somatosensory ERPs, which are converted into scalp current  
274 density<sup>20</sup> in off-line analysis, at electrodes (FC3, FC5, C3) over the left sensorimotor area.  
275 Somatosensory event-related potentials were recorded while participants listen to speech in  
276 the presence of continuous background sounds. The study tested four background conditions:  
277 speech, non-speech sounds, pink-noise and silent<sup>13</sup>. The results indicated the amplitude of  
278 somatosensory event-related potentials during listening to speech sounds was significantly  
279 greater than the other three conditions. There was no significant difference in amplitude for  
280 the other three conditions. Figure 4B shows normalized peak amplitudes in the different  
281 conditions. The result indicates that listening to speech sounds alters the somatosensory  
282 processing associated with facial skin deformation.

283

284 *[Place Figure 4 here]*

285

286 **Figure 1: Experimental setup.**

287

288 **Figure 2: Event related potentials in response to somatosensory stimulation produced by**  
289 **facial skin stretch.** The ERPs were obtained from representative electrodes.

290

291 **Figure 3: Event-related potentials reflect a somatosensory-auditory interaction in the context**  
292 **of speech perception.** This Figure has been modified from Ito, et al.<sup>12</sup> **A:** temporal pattern of  
293 somatosensory and auditory stimulations. **B:** Event-related potentials for combined  
294 somatosensory and auditory stimulation in three timing conditions (lead, simultaneous, and  
295 lag) at electrode Pz. The red line represents recorded responses to paired ERPs. The dashed line  
296 represents the sum of somatosensory and auditory ERPs. The vertical dotted lines define an  
297 interval 160–220 ms after somatosensory onset in which differences between “pair” and “sum”  
298 responses are assessed. Arrows represent auditory onset.

299

300 **Figure 4: Enhancement of somatosensory event-related potentials due to speech sounds.** The  
301 ERPs were recorded under four background sound conditions (Silent, Pink noise, Speech and  
302 Non-speech). This Figure has been modified from Ito, et al.<sup>13</sup> **A:** Temporal pattern of  
303 somatosensory event-related potentials in the area above left motor and premotor cortex. Each  
304 color corresponds to a different background sound condition. The ERPs were converted to scalp  
305 current density<sup>20</sup>. **B:** Differences in z-score magnitudes associated with the first peak of the  
306 somatosensory ERPs. Error bars are standard errors across participants. Each color corresponds  
307 to different background sound conditions, as in Panel A.

308



309 **DISCUSSION:**

310 The studies reported here provide evidence that precisely controlled somatosensory  
311 stimulation that is produced by facial skin deformation induces cortical ERPs. Cutaneous  
312 afferents are known as a rich source of kinesthetic information<sup>3,4</sup> in human limb movement<sup>5,6</sup>  
313 and speech movement<sup>7,8,21</sup>. Stretching the facial skin in a manner that reflects the actual  
314 movement direction during speaking induces a kinesthetic sense similar to the corresponding  
315 movement. The current method combining precisely controlled skin stretch and ERP recordings  
316 can be used to investigate the neural basis of orofacial function during a wide range of speech  
317 behaviors.

318  
319 Using mechanical stimulation and simultaneous EEG recording, it is important to monitor the  
320 ongoing signals for artifact. In particular, since the strings used to stretch the skin are located  
321 close to the EEG electrodes and cables, there is the possibility of electrical and motion artifacts  
322 being induced in the EEG signals. This artifact is distinguishable because of relatively large  
323 amplitude and lower frequency compared with the electrophysiological response. Before  
324 recording, the stimulation setup including the string configuration needs to be checked  
325 carefully to identify and eliminate any mechanical artifacts due to the stimulation. Although  
326 artifacts can be removed by post signal processing, such as filtering or independent component  
327 analysis<sup>22</sup> similar to eye movement and blinking, cleaner signals are always more desirable.

328  
329 The previous studies of somatosensory event-related potentials have mostly used brief  
330 somatosensory stimuli that were produced using mechanical<sup>23</sup>, electrical<sup>18</sup> or laser nociceptive  
331 stimulation<sup>15</sup>. Somatosensory inputs arising from these kinds of stimulation are not associated  
332 with any particular articulatory motion in speech, and hence, they may not be suitable for  
333 investigating speech-related cortical processing. Möttönen, et al.<sup>17</sup> had failed to show a change  
334 of magnetoencephalographic somatosensory potentials using simple lip tapping during listening  
335 to speech sounds. In contrast, deformation of the facial skin provides kinesthetic input similar  
336 to that which occurs in conjunction with speech articulatory motion<sup>21</sup> and sensorimotor  
337 adaption<sup>7</sup>. These stimuli also interact with speech perceptual processing<sup>1,14</sup>. The somatosensory  
338 ERP from the current skin stretch perturbation is more suitable for the investigation of speech-  
339 related cortical processing than the other methods currently available for somatosensory  
340 stimulation. Several different characteristics were found between the current skin stretch  
341 stimulation and the previous methods. Further investigation including the source location is  
342 required.

343  
344 Although deformation of the facial skin occurs to varying degrees during speech motion<sup>8</sup>, the  
345 skin lateral to the oral angle is densely innervated with cutaneous mechanoreceptors<sup>10,24</sup> and  
346 may be predominantly responsible for the detection of skin stretch during speech. The skin at  
347 the corners of the mouth may be especially important for speech motor control and speech  
348 motor learning. The current approach is somewhat limited because the stretch of the skin can  
349 only be done in one direction and at one location per EEG session. Using a more complex skin  
350 deformation and evaluating multiple directions and/or multiple locations in one EEG session  
351 will provide further insight into the specific role of somatosensation in speech processing.

352

353 There are long-standing interests in speech communication studies concerning the nature of  
354 representations and processing in speech production and perception<sup>25-27</sup>. The discovery of  
355 mirror neurons<sup>28,29</sup> reinforced the idea that motor functions are involved in speech perception.  
356 The involvement of the motor system (or the motor and premotor cortex) has also been  
357 investigated<sup>30-35</sup> in the perception of speech sounds. Nevertheless, the link between speech  
358 production and perception is still poorly understood. Exploring possible somatosensory  
359 influences on speech perception can help us understand the neural bases of speech perception  
360 and production, and whether they overlap or link. The current technique for modulating  
361 somatosensory function has provided a new tool to investigate this important area of inquiry.  
362 The current technique has the additional advantage that it can be used in investigations of  
363 somatosensory function more generally and how it interacts with other sensory modalities in  
364 neural processing.

365

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371

#### 372 **DISCLOSURES:**

373 The authors have nothing to disclose.

374

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