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Delphine Boudard, Valérie Forest, Jérémie Pourchez, Najih Boumahdi, Maura Tomatis, et al.. In vitro cellular responses to silicon carbide particles manufactured through the Acheson process: impact of physico-chemical features on pro-inflammatory and pro-oxidative effects.. *Toxicology in Vitro*, 2014, 28 (5), pp.856-865. 10.1016/j.tiv.2014.02.012 . hal-01021766

**HAL Id: hal-01021766**

**<https://hal.science/hal-01021766>**

Submitted on 9 Jul 2014

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***In vitro* cellular responses to silicon carbide particles manufactured through the Acheson process: impact of physico-chemical features on pro-inflammatory and pro-oxidative effects.**

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## **Abbreviations**

BET method: Brunauer-Emmet-Teller method

COO<sup>•</sup>: Carboxyl radical

DMEM: Dulbecco's Modified Eagle's Medium

EPR: Electron Paramagnetic Resonance

FCS: Fetal Calf Serum

HO<sup>•</sup>: Hydroxyl radical

H<sub>2</sub>O<sub>2</sub>: Hydrogen peroxide

ICP: Inductively Coupled Plasma spectrometry

ROS: Reactive Oxygen Species

SiC: Silicon carbide

SSA: Specific Surface Area

TNF $\alpha$ : Tumor Necrosis Factor alpha

XPS: X-ray Photoelectron Spectroscopy

## **Abstract**

Silicon carbide (SiC) an industrial-scale product manufactured through the Acheson process, is largely employed in various applications. Its toxicity has been poorly investigated. Our study aims at characterizing the physico-chemical features and the *in vitro* impact on biological activity of five manufactured SiC powders: two coarse powders (SiC C1/C2), two fine powders (SiC F1/F2) and a powder rich in iron impurities (SiC I). RAW 264.7 macrophages were exposed to the different SiC particles and the cellular responses were evaluated. Contrary to what happens with silica, no SiC cytotoxicity was observed but pro-oxidative and pro-inflammatory responses of variable intensity were evidenced. Oxidative stress ( $H_2O_2$  production) appeared related to SiC particle size, while iron level regulated pro-inflammatory response (TNF $\alpha$  production). To investigate the impact of surface reactivity on the biological responses, coarse SiC C1 and fine SiC F1 powders were submitted to different thermal treatments (650 to 1400°C) in order to alter the oxidation state of the particle surface. At 1400°C a decrease in TNF $\alpha$  production and an increase in HO $\cdot$ , COO $^{\cdot-}$  radicals production were observed in correlation with the formation of a surface layer of crystalline silica. Finally, a strong correlation was observed between surface oxidation state and *in vitro* toxicity.

**Keywords:** *silicon carbide powders, Acheson process, thermal post-treatment, physico-chemical characterization, biological toxicity, occupational exposure.*

## **Introduction**

Silicon carbide (SiC) was discovered in 1892 by Edward Goodrich Acheson who searched a diamond substitute material (Acheson, 1893). Today SiC denomination is a generic term that refers to a family of different materials sharing some common physico-chemical characteristics. The production of SiC, a well known material has significantly increased during the past fifty years mainly due to its remarkable properties such as high chemical inertness, elevated thermal stability and excellent mechanical properties. SiC particles are widely used for many different industrial purposes in the ceramic or composite material field, including particulate filters and abrasives (Pham-Huu et al., 1999).

SiC is industrially manufactured through the Acheson process. Reactants (petroleum coke and silica) are placed all around a graphite resistance in an electric furnace in order to enable the carbothermal reduction of  $\text{SiO}_2$  into SiC at high temperature. At the end of the firing and after several post-process operations (crushing, grinding, etc.) polydisperse SiC powders are obtained. At each step of this process, aerosolized SiC fractions as well as by-products, can be generated in the work environment and can potentially be inhaled by the workers. A health risk among SiC workers has been noticed since the beginning of the 19<sup>th</sup> century (Winslow et al., 1919; Bruusgaard, 1948). Occupational analyses focusing on the Acheson process showed that the airborne environment was charged with SiC microparticles, SiC fibers and impurities, especially crystalline silica and carbon (Hayashi and Kajita, 1988; Osterman et al., 1989). Moreover, analyses of lung tissue biopsies from workers exposed to these powders have revealed substantial amounts of SiC particles in alveolar spaces and interstitial fibrosis associated with an increased pneumoconiosis incidence (Funahashi et al., 1984; Hayashi and Kajita, 1988; Massé et al., 1988; Dufresne et al., 1992). Taken together, these observations were considered to be the result of a silicogenic (fibrogenic) effect (Bruch et al., 1993b) and

showed the importance of occupational risk evaluation on SiC exposure, through toxicological studies (Bruch et al., 1993a, 1993b; Bruch and Rehn, 1996).

Toxicological data available in the literature are mainly obtained from experiments conducted on micro-scaled SiC particles or fibers (called whiskers), but SiC toxicity has been poorly investigated and the few reported data are controversial, making it difficult to draw clear conclusions. For instance, it has been shown that SiC particles do not induce harmful effects on tissues, suggesting that SiC material is quite biologically inert (Bruch et al., 1993a, 1993b). Conversely, other studies have suggested potential adverse effects induced by SiC. *In vivo* exposure to whiskers triggers lung inflammation (Cullen et al., 1997), granulomas (Vaughan et al., 1993), bronchoalveolar hyperplasia and severe lung fibrotic changes (Akiyama et al., 2007), while micro-scaled SiC particles were associated to oxidative stress, genotoxic and carcinogenic effects (Cichy, 1989; Svensson et al., 1997; Allen et al., 1995). Moreover, *in vitro* responses are characterized by significant reactive oxygen species (ROS) generation (Svensson et al., 1997), cytotoxic and genotoxic effects (Svensson et al., 1997; Allen et al., 1995), and stimulation of pro-inflammatory cytokines production like TNF $\alpha$  (Allen et al., 1995; Cullen et al., 1997). These results mainly underline a potential impact of SiC particle shape on the biological activity, because SiC whiskers (*i.e.* long and rigid rods of SiC) induce more important biological activity than isotropic SiC particles (Svensson et al., 1997).

Recent *in vitro* studies, specifically devoted to SiC nanoparticles, highlighted an accumulation of particles in A549 lung epithelial cells, a major cell oxidation-reduction status disturbance and DNA damage (Barillet et al., 2010a; Barillet et al., 2010b). Another study clearly showed the impact of the nanoparticle surface area and the nature of crystalline phases ( $\alpha$ -SiC vs.  $\beta$ -SiC) on the TNF $\alpha$  production, the influence of the iron content at the nanoparticle surface on the free radical release, and the surface oxidation on the cellular H<sub>2</sub>O<sub>2</sub> production (Pourchez et al., 2012). Thus, these authors proposed to reconsider SiC nanoparticles biocompatibility

and to handle SiC nanoparticles with caution until more toxicological information is available.

In this context, it seems crucial to investigate more deeply the interactions between SiC industrial powders manufactured through the Acheson process and living cells. Consequently, we conducted a multidisciplinary study in order to examine the impact of the physico-chemical parameters of SiC industrial particles on the *in vitro* cellular responses. As a matter of fact, a main challenge is the lack of comprehensive data to assess the potential toxicity of a SiC industrial particle collection regarding different sizes, oxidation state of surfaces, crystallographic structure or chemical composition. These complementary physico-chemical and biological approaches may be particularly suitable for a safer by design development.

To reach this objective we studied 5 polydisperse SiC powders manufactured by the Acheson process in industrial plants: two coarse SiC C1/C2 powders; two fine SiC F1/F2 powders and a coarse impure powder SiC I with a high level of metallic impurities. Their physico-chemical features were first characterized: crystallographic structure, C/Si atomic ratio (*i.e.* silicon or carbon excess), surface oxidation state (*i.e.* the formation of a silica or oxycarbide layer around the SiC grain) and the presence of iron impurities on particle surface. *In vitro* toxicological assessment was then carried out using macrophages (RAW 264.7, a cultured murine macrophage cell line widely used in toxicological studies due to its phagocytic capacity). The cytotoxicity (LDH release), a pro-inflammatory effect (TNF $\alpha$  production), and the oxidative stress (H<sub>2</sub>O<sub>2</sub> specific production) were assessed. Finally, the particle potential to release free radical species was evaluated in cell free condition. Two radical-generating mechanisms have been examined: i) HO $\cdot$  radical generation in the presence of hydrogen peroxide. This test mimics the contact with lysosomal fluids where H<sub>2</sub>O<sub>2</sub> is released following particle phagocytosis by alveolar macrophages; and ii) COO $\cdot^-$  from the formate ion, used as a

model target molecule for homolytic cleavage of a carbon-hydrogen bond in several organic molecules and biomolecules.

Finally, to better investigate the impact of the surface nature of the particles on cellular responses, coarse SiC C1 and fine SiC F1 powders underwent an oxidative thermal post-treatment at different temperatures (650°C, 750°C, 850°C, 1400°C). Biological activity was then assessed.

## **Materials and methods**

### *Collection of manufactured SiC powders*

In this study, the 5 SiC industrial powders used (SiC C1/C2/F1/F2 and I) were produced by the Acheson process, and collected in industrial plants. SiC C1 and C2 particles correspond to coarse  $\alpha$ -SiC microparticles and are mainly used for abrasives and refractory applications. SiC F1 and F2 particles correspond to fine  $\alpha$ -SiC microparticles and are mainly used for particulate filters and technical ceramics. SiC I powder can be considered as a metallurgical impure powder with no particular industrial application, but this sample is representative of airborne dusts that can be disseminated and inhaled in the workplace environment. Only alveolar fractions of SiC powders have been studied using a vertical elutriator (Boumahdi, 2009). This fraction corresponds to particles lower than 10  $\mu\text{m}$  contained in raw powders.

### *Oxidative thermal post-treatment*

SiC C1 and F1 powders were submitted to increasing thermal treatments under air atmosphere. SiC grains monolayer bed was laid out in a crucible (AluSIK-99 ZA) in the middle of a tubular furnace (Nabertherm RHT08/17), and exposed for 2 hours at the following temperatures: 650°C, 750°C, 850°C and 1400°C.



### *SiC particles characterization*

SiC physico-chemical characteristics were investigated using the following methods. Particles morphology was observed using a field-emission scanning electron microscope (JEOL JSM-6500F). The specific surface area (SSA,  $\text{m}^2/\text{g}$ ) was determined by  $\text{N}_2$  adsorption at 77K after out-gassing 2h at 200°C (Micromeritics ASAP 2000), using the Brunauer-Emmet-Teller (BET) method. Particle size distribution and crystalline structure were determined respectively by laser granulometry (Malvern, Mastersizer 2000) and X-ray diffractometry with a semi-quantitative analysis by Rietveld Method (Siemens Kristalloflex diffractometer D8). Particle median diameter  $D_{50}$  (BET size,  $\mu\text{m}$ ) was calculated as  $\text{BET size} = 6000 / (\rho \times \text{SSA})$ . Concentration of constitutive elements (Si, C) and impurities (especially iron and aluminum) was deduced from elemental chemical analysis by inductively coupled plasma spectrometry (ICP, Jobin-Yvon Activa). The oxidation state of SiC powders (silica, quartz, cristobalite, oxycarbide layer around SiC grains) was characterized by surface analysis using X-ray photoelectron spectroscopy (XPS, Thermo VG Thetaprobe) and X-ray diffractometry.

### *Free radical release in cell free system*

Electron paramagnetic resonance (EPR) using the spin-trapping technique (Fubini et al., 1995b) was used to evaluate SiC particle potential to generate free radicals (hydroxyl radical  $\text{HO}^\bullet$ , carboxyl radical  $\text{COO}^\bullet$ ) in aqueous suspensions. Each powder (45 mg) was suspended in a buffered solution (0.5M potassium phosphate buffer, pH 7.4) 0.15M of DMPO (5-5'-dimethyl-1-pyrroline-N-oxide). The reaction was started by adding the substrate molecule respectively hydrogen peroxide (1.0M) or sodium formate (1.0M) to the SiC particle suspension. The radical yield was progressively measured in a 50  $\mu\text{l}$  aliquot of the suspension up to one hour. Radical species release was monitored in the suspension by EPR spectroscopy (Miniscope 100 EPR spectrometer, Magnettech). The instrument settings were as follows:

microwave power 10 mW; modulation 1000 mG; scan range 120 G; centre of field approximately 3345 G. The use of internal standard (Mn) enabled radical activity quantification. Each experiment was repeated independently three times for each powder and included controls: amorphous silica (radical negative control) and DQ12 quartz (toxicological positive control)(Bruch et al., 2004; Fubini et al., 2004).

#### *Cell line and culture conditions*

The RAW 264.7 cell line derived from murine peritoneal macrophages transformed by the AML Virus (Abelson Murine Leukemia Virus) was provided by the ATCC Cell Biology Collection (Promochem LGC, Molsheim). Cells were cultured in Dulbecco's Modified Eagle's Medium (DMEM, Invitrogen), complemented with 10% fetal calf serum (FCS, Invitrogen), 1% penicillin-streptomycin (penicillin 10 000 units/mL, streptomycin 10mg/mL; Sigma-Aldrich, Saint-Quentin Fallavier, France) and incubated at 37°C under a 5% carbon dioxide humidified atmosphere.

For each experiment, as described by Leclerc et al. (2010), cells were prepared in 96-well plates (100 000 cells/well for TNF $\alpha$  and LDH assays) in 25  $\mu$ L of complete DMEM (DMEMc). Suspensions of SiC powders were prepared in 75  $\mu$ L of DMEMc which were added to the culture and incubated either for 90 min or 24h at 37°C in a 5% CO<sub>2</sub> atmosphere, depending on the biological parameter studied (cytotoxicity, TNF $\alpha$  production or oxidative stress), as described below. Cell viability was determined by trypan blue dye exclusion (FDA, Sigma), after each contact between cells and particles.

Different doses were tested: 15, 30, 60 and 120  $\mu$ g of particles per mL of culture medium. Negative and positive controls of toxicity, corresponding to the cells incubated alone or incubated with DQ12 quartz respectively (Bruch et al., 2004) were included. Three independent experiments were performed for each condition.

### *Cytotoxicity assays*

The activity of the lactate dehydrogenase (LDH) released from cells with damaged membranes in the culture supernatant was assessed after a 24h incubation of cells with SiC particles. The CytoTox-ONE™ Homogeneous Membrane Integrity Assay (Promega, Charbonnières les bains, France) was used according to the manufacturer's instructions. Detection was performed using a fluorometer (Fluoroskan Ascent, Thermolabsystems), with excitation/emission wavelengths set at 530/590 nm. The activity of the released LDH was reported to that of total cellular LDH (measured after the lysis of control cells) and was expressed as a percentage of the control.

### *Pro-inflammatory TNF $\alpha$ production*

Tumor Necrosis Factor alpha (TNF $\alpha$ ) production was assessed in the culture supernatant after a 24h incubation of cells with SiC particles. A commercial ELISA Kit (Quantikine® Mouse TNF $\alpha$  Immunoassay, R&D Systems, Lille, France) was used according to the manufacturer's instructions. The optical density of each well was determined using a microplate reader (Multiskan RC, Thermolabsystems, Helsinki, Finland) set at 450 nm. A standard curve was established and results were expressed in pg/mL of TNF $\alpha$ .

### *Oxidative stress with H<sub>2</sub>O<sub>2</sub> production*

Acute oxidative stress was assessed by the production of H<sub>2</sub>O<sub>2</sub> after 90 min interaction between the cells and the different types of SiC powders. Hydrogen peroxide H<sub>2</sub>O<sub>2</sub> production was measured according to the protocol of De la Harpe and Nathan (1985). Briefly, KRPG (Krebs-Ringer phosphate glucose) buffer, containing a mixture of scopoletin (30  $\mu$ M), NaN<sub>3</sub> (1 mM) and horseradish peroxidase (1 unit pupurogallin/ml HPO) was added to cells. Over a 90 min period, fluorimetric determination (355/460 nm excitation/emission wavelengths) of

scopoletin oxidation, catalyzed by horseradish peroxidase was measured (Fluoroskan Multiskan). Results were expressed as the amount of H<sub>2</sub>O<sub>2</sub> released by cells (nmol H<sub>2</sub>O<sub>2</sub>/10<sup>6</sup> cells).

### *Statistical analysis*

For the several parameters of *in vitro* biological evaluation, a statistical analysis was carried out using a two-way analysis ANOVA test with Bonferroni post-test, in order to perform multiple comparisons between the different SiC particles against the same biological negative control (cells incubated alone, or amorphous silica for free radical HO<sup>•</sup> and COO<sup>-</sup> release). A one-way ANOVA test with Bonferroni post-test was used to compare the same powder SiC C1 / F1 either native (unoxidized, that serves as a control) or submitted to various temperatures. Analysis and graphics were performed on Prism 5.0 software (GraphPad, San Diego, CA). Only points with a test significance at p<0.001 (\*\*\*) were reported into the graphs. Results are expressed as means of three independent experiments.

A linear regression curve with the R<sup>2</sup> coefficient was also established for the H<sub>2</sub>O<sub>2</sub> production depending on the SiC particle surface (cm<sup>2</sup>), after adding a trendline to excel data base.

## **Results and discussion**

A comprehensive physico-chemical characterization of 5 industrial SiC powders was carried out, followed by the *in vitro* evaluation of the biological responses.

Physico-chemical data are presented in Table 1 with an illustration of the morphological aspect of SiC particles given by Figure 1. SiC powders were polydispersed and exhibited an irregular-shaped morphology characterized by a smooth surface with sharp ridges and the presence of submicronic particles fixed on larger particles which is a common feature of powders synthesized by the Acheson process (Figure 1).

They could be classified either as 2.5  $\mu\text{m}$  coarse particles (SiC C1 and C2) or 0.5  $\mu\text{m}$  fine particles (SiC F1 and F2). SiC I was kept apart because of a higher size (6  $\mu\text{m}$ ), the presence of crystallized silica and its very high metallic impurities content (iron about 20 000 ppm compared to 2500 ppm for other powders). Except SiC I showing a very high crystallized silica content and only 65% of  $\alpha$ -SiC phases, the other SiC powders correspond to pure  $\alpha$ -SiC phases (> 99%), with very similar features in terms of C/Si ratio around 1 and crystallographic structure (principally with SiC-6H polytype and SiC-4H and SiC-15R <10%). By contrast SiC I powder has a 1.66 C/Si ratio associated with high oxygen and free carbon levels (%O  $\approx$  6 %, %C<sub>Free</sub>  $\approx$  17.5 %) and the presence of crystallized silica (9% of quartz and 5% of cristobalite).

Biological effects of SiC powders concerning cytotoxicity, pro-inflammatory TNF $\alpha$  response and oxidative stress are reported in Figures 2, 3 and 4 respectively.

Surprisingly all the 5 SiC powders manufactured through the Acheson process were found to be globally not cytotoxic (Figure 2), contrary to nano-sized SiC particles synthesized by other routes as shown by Pourchez *et al.* (Pourchez et al, 2012). Only the positive control (DQ12 quartz) clearly showed a significantly enhanced and dose-dependent LDH release.

All particles induced a moderate pro-inflammatory response (Figure 3), except SiC I which generated a strong TNF $\alpha$  production (around 3000 pg/ml at 120  $\mu\text{g}$  dose for example), even higher than that induced by the DQ12 quartz (around 2400 pg/ml at the same dose). This SiC I atypical profile could be explained on the one hand by the presence of crystallized silica (quartz and cristobalite) with high free carbon levels, and on the other hand by its high content of iron impurities (Table 1) (Fubini et al., 1999; Governa et al., 2005; IARC, 1996).

It has been well described in the literature that there is a relationship between the presence of surface transition metal ions (especially iron) and cellular responses (Fubini et al., 1995b; Pritchard et al., 1996; Aust et al., 2000), especially for free radical generation (Fubini and

Hubbard, 2003; Fenoglio et al., 2001; van Maanen et al., 1999; Turci et al., 2011; Pourchez et al., 2012). Indeed iron is known to be a catalyst in the formation of several reactive oxygen species (Pierre and Fontecave, 1999), particularly the hydroxyl radical can be generated through the Fenton reaction ( $\text{Fe}^{2+} + \text{H}_2\text{O}_2 \rightarrow \text{Fe}^{3+} + \text{OH}^- + \text{HO}^\bullet$ ) when ferrous iron (Fe[II]) are converted into ferric iron (Fe[III]) (Halliwell and Gutteridge, 1992). Oxidative stress is not only the result of an over-production of oxygen reactive species, it also implies that physiological antioxidant defenses are overwhelmed. But this antioxidant aspect will not be evaluated in this study.

$\text{H}_2\text{O}_2$  cellular production and free radical generation in cell free test have been employed to assess the ability of SiC particles to induce oxidative stress.  $\text{H}_2\text{O}_2$  production induced by fine SiC F1 and F2 particles, regardless the dose was much higher than that triggered by the coarse SiC C1 / C2 or SiC I powders and even more elevated than that caused by the DQ12 quartz (Figure 4). This suggests that particle size may have a role in some cellular responses, particularly on ROS intracellular generation. A linear relationship is indeed detectable between  $\text{H}_2\text{O}_2$  production and the SSA parameter ( $y = 15.9x + 21.5$ , where  $y = \text{H}_2\text{O}_2$  production in  $\text{nmol}/10^6$  cells and  $x =$  particle surface in  $\text{cm}^2$ ;  $R^2 = 0.9$ , supplementary Figure 1). This is in agreement with a previous study which has shown a significant impact of nanosized SiC specific surface area on *in vitro* cellular responses (Pourchez et al., 2012) and also with results previously published in the literature for other particles like  $\text{TiO}_2$  and carbon black (Oberdörster et al., 1994; Oberdorster, 2000; Oberdörster et al., 2005; Brown et al., 2001; Höhr et al., 2002; Donaldson et al., 2002; Fubini, 2007).

To investigate the ability of SiC to generate particle-derived free radicals (not at the cellular level),  $\text{HO}^\bullet$  and  $\text{COO}^{\bullet-}$  production was assessed in cell free condition by EPR spectroscopy (Figure 5). All particles were able to release free radicals and were more effective in  $\text{COO}^{\bullet-}$  than in  $\text{HO}^\bullet$  radical generation. Free radical production increased with particle size, it was 3-5

folds higher for the coarse SiC C1/C2 particles than for fine SiC F1/F2 particles (maximal  $\text{COO}^\cdot$  production for SiC C2). The SiC I powder was characterized rather by a  $\text{HO}^\cdot$  radical profile, with a 5-fold production compared to SiC F1/F2. This behavior may be related to the large amount of iron (Table 1) in the coarse particles if compared to the fine ones, especially SiC I which exhibited also a partially crystallized surface silica layer. Note that  $\text{HO}^\cdot$  and  $\text{COO}^\cdot$  release did not parallel the  $\text{H}_2\text{O}_2$  production observed in macrophage cells (Figure 4), since these tests reflect different outcomes and depend upon different parameters.  $\text{H}_2\text{O}_2$  production in cellular test reflects macrophage activation, following particle phagocytosis. This is a complex process initiated by the interaction between the particle and the phagocyte, which may be affected by several physico-chemical features of the particle itself (size, shape, surface charge, hydrophilicity etc.). Conversely, free radical generation in cell free medium only depends on the intrinsic characteristics of the particle surface, e.g. presence of reactive sites (e.g. redox active metal ions) or crystalline state. Once inhaled, the particle is in contact with several organic molecules such as proteins, non enzymatic antioxidants, lipids. Carboxyl radical release reflects the potential of inhaled particles to react with these molecules promoting the cleavage of C-H bonds. This mechanism may take place in extracellular fluids before macrophage phagocytosis. Opposite to C-H cleavage,  $\text{HO}^\cdot$  release only occurs in  $\text{H}_2\text{O}_2$  rich-fluids such as phagolysosomal fluid, and reflects the ability of inhaled particle to react with  $\text{H}_2\text{O}_2$ . We therefore expect a consumption of  $\text{H}_2\text{O}_2$  following Fenton or Fenton-like reactions.

To investigate the role of surface oxidation state, two SiC powders (C1 and F1) were submitted to increasing thermal treatments (from 600 to 1400°C). Oxidative thermal treatments led to surface modifications characterized by an increase of the silica layer thickness at 1400°C, as illustrated in Figure 6 (Deal and Grove, 1965; Filipuzzi, 1991; Shi et al., 2001; Das et al., 2004). At this temperature  $\text{Fe}^{2+}$  is also converted into  $\text{Fe}^{3+}$ .

The physico-chemical characterization of the oxidized SiC C1 and SiC F1 powders revealed no significant changes in the morphology or specific surface area of the particles, except at 1400°C where the morphology was strongly modified presenting a grain aspect mainly characterized by less sharp ridges and more rounded edges. SiC particles were progressively covered with a surface amorphous SiO<sub>2</sub> layer which was transformed into cristobalite silica at 1400°C (Table 2 and Figure 6). This observation was correlated with an increased oxide layer, judging by the silica evolution and a silicon carbide peak decrement (data not shown). At 1400°C, oxidized SiC C1 and SiC F1 showed both a SSA and a C/Si ratio decrement (Table 2).

The biological activity assessment after thermal treatments is presented in Figures 7 to 10. A significant development of cytotoxicity was observed for oxidized SiC F1 compared to that of the original SiC F1 powder, whatever the temperature (Figure 7B), reaching values similar to that of the positive control DQ12. On the contrary, oxidative treatments had a more limited effect on the cytotoxicity of SiC C1, except for specific temperatures and dose particles (Figure 7A). At an equivalent dose, the LDH release for the fine oxidized SiC F1 powder was higher than for the coarse oxidized SiC C1 powder, suggesting that fine particles exhibiting a higher surface could be more easily oxidized, which resulted in a higher cytotoxicity.

Similarly, oxidized SiC C1 showed no significant production of TNF $\alpha$  compared to the negative control and unoxidized SiC C1 whereas oxidized SiC F1 (from 650-850°C) exhibited a TNF $\alpha$  production drastically higher than that induced by SiC F1 particles (Figure 8A and 8B). However, it is interesting to note that both oxidized SiC C1 and SiC F1 particles treated at 1400°C, despite the presence of a silica cristobalite layer around SiC grains, presented a TNF $\alpha$  production equivalent to that of the negative control and significantly lower than their original counterparts. Some studies indicate that cristobalite originated by heating quartz at high temperature (>1300°C), as well heated cristobalite, exhibits higher



hydrophobicity and lower amount of surface radicals (Fubini et al., 1995b, 1995a) if compared to other cristobalite samples, such as those originated from diatomaceous earth heated at 1000°C. Heated cristobalite also exhibits a lower toxicity in cell free tests (Fubini et al., 1999). This may partially explain the limited pro-inflammatory effect of industrial SiC powders treated at 1400°C.

Oxidation of SiC C1 did not influence the H<sub>2</sub>O<sub>2</sub> production (Figure 9A). Although oxidized SiC F1 exhibited a H<sub>2</sub>O<sub>2</sub> generation higher than that of the positive control (irrespective of the temperature), it remained in the same range as the original SiC F1 powder, except at 750°C with an H<sub>2</sub>O<sub>2</sub> production significantly higher than original SiC F1, whatever the dose. On the contrary H<sub>2</sub>O<sub>2</sub> production for SiC F1-650°C was significantly less than for original SiC F1, whatever the particles dose. We have finally calculated the R<sup>2</sup> coefficient between H<sub>2</sub>O<sub>2</sub> production and the particle surface for the different temperatures. For oxidized SiC C1, R<sup>2</sup> = 0.471 and for oxidized SiC F1, R<sup>2</sup> = 0.667 (data not shown). These results suggested that the production of H<sub>2</sub>O<sub>2</sub> was not dependent on the degree of oxidation and iron content (Table 3). The different behavior between oxidized SiC C1 and F1 could be once again explained by a particle size effect.

The increasing amorphous surface layer and progressive conversion of Fe<sup>2+</sup> into Fe<sup>3+</sup> following oxidation at low temperatures (<850°C) are likely responsible for the decrease in free radical generation (Figure 10). The decrease was more noticeable for carboxyl than for hydroxyl radicals. Although the mechanism of COO<sup>•-</sup> generation is not still fully clarified, the reduction of reactivity subsequent to oxidation of active surface sites has been observed also in other particulates (Tomatis et al., 2002). However, SiC C1 and F1 oxidized at 1400°C showed an increased capacity to generate an EPR signal, mainly for HO<sup>•</sup> but also for COO<sup>•-</sup> radicals even if for this latter the effect was much less pronounced (Figure 10). At this treatment temperature, two correlations can be established: between HO<sup>•</sup>, COO<sup>•-</sup> radicals and

crystallization on the one hand (cristobalite > amorphous SiO<sub>2</sub>) and between HO<sup>•</sup>, COO<sup>•-</sup> radicals and size on the other hand (coarse oxidized SiC C1 > fine oxidized SiC F1, Table 3). These observations were in agreement with previous literature studies describing specifically a more important toxicity associated with a higher radical potential for crystallized silica compared to amorphous SiO<sub>2</sub> (Fubini et al., 1999; Fubini and Hubbard, 2003). Finally, we have observed as for original SiC C1 and F1 powders an opposite trend between cellular oxidative stress (H<sub>2</sub>O<sub>2</sub> production) and free radical generation in cell free conditions. The EPR radical potential was temperature-dependent and directly related to the silica phase nature: amorphous SiO<sub>2</sub> at 650, 750 and 850°C compared to cristobalite SiO<sub>2</sub> at 1400°C (Table 2).

## **Conclusion**

Particle and fibre toxicology is known to be closely related to their physico-chemical properties (size, shape, surface area, chemical composition, etc.). In order to deepen such a relationship, a thorough physico-chemical characterization of different SiC powders manufactured through the Acheson process and collected at workplace was carried out, in association with an *in vitro* evaluation of their biological activity. Table 3 summarizes the relationships put in evidence in the present study.

We have thereby demonstrated that all types of industrial SiC particles tested did not induce any significant cytotoxic effect. Three parameters having an influence on the *in vitro* biological response were identified: the particle size, the presence of iron impurities at the particle surface and the oxidation state.

The particle size was found to have an impact on SiC powders related to H<sub>2</sub>O<sub>2</sub> production oxidative stress, with a significantly higher impact for fine SiC particles. Size of oxidized fine SiC F1 seems to have also an influence especially on cytotoxicity and to a lesser extent on

oxidative stress. The presence of iron metallic impurities at the surface of the particles mainly stimulated a pro-inflammatory TNF $\alpha$  response which was abolished when amorphous SiO<sub>2</sub> was transformed into cristobalite at 1400°C. The oxidation surface modifications by this 1400°C thermal treatment seemed to also have a deep impact on HO<sup>•</sup> and COO<sup>-</sup> radical generation.

Taken together these results support the conclusion that the various manufactured SiC powders collected from Acheson process workplace, do not induce similar levels of toxicity, underlining the need to systematically evaluate the biological activity in relation to the particles physico-chemical features through case by case studies. Furthermore, the modification of particles surface has clearly emphasized the major importance of surface oxidation state, in addition to more usual physico-chemical features such as size, SSA, shape or chemical composition.

This approach combining systematically physico-chemical characterization and biological assessment is particularly recommended in the evaluation of occupational risks in industrial environments or in the context of “safer by design” principles (Morose, 2010). By tightly controlling the physico-chemical features of the industrial SiC particles, pro-inflammatory effect and oxidative stress could be limited. A particularly interesting observation is that SiC toxicity manufactured through the Acheson process seems to be modulated by the oxidized external layer around SiC grains. It opens new perspectives in the preparation of industrial powders as the prevention of potential hazard seems easier at the design stage than during the manufacturing processes or at the customer use level.

**Funding information**

This work was supported by the French Ministry of Industry and an industrial partner.

**Supporting information available**

Supplementary Figure 1 representing the relationship between the H<sub>2</sub>O<sub>2</sub> production and the particle surface. This material is available online.

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## Figure legends

Figure 1 – Morphological aspect of SiC microparticles observed by scanning electron microscopy. A) SiC C1 representative of coarse particles, B) SiC F2 representative of fine particles.

Figure 2 – Cytotoxicity of the different SiC microparticles determined by the LDH release. Results are means of 3 independent experiments. Standard deviation and statistically significant differences from the negative control (cells incubated without particles) are also indicated: \*\*\*  $p < 0.001$  (two-way ANOVA test).

Figure 3 – Pro-inflammatory effect of the different SiC microparticles determined by the TNF $\alpha$  production. Results are means of 3 independent experiments. Standard deviation and statistically significant differences from the negative control (cells incubated without particles) are also indicated: \*\*\*  $p < 0.001$  (two-way ANOVA test).

Figure 4 – Acute oxidative stress induced by the different SiC microparticles as assessed by the H<sub>2</sub>O<sub>2</sub> production. Results are means of 3 independent experiments. Standard deviation and statistically significant differences from the negative control (cells incubated without particles) are also indicated: \*\*\*  $p < 0.001$  (two-way ANOVA test).

Figure 5 – Free radical release by the different SiC microparticles A) HO $\cdot$  and B) COO $\cdot^-$ , as determined by electron paramagnetic resonance. A negative control (amorphous silica) and a positive control (DQ12 quartz) were included. Results are means of 3 independent experiments. Standard deviation and statistically significant differences from the negative control (amorphous silica) are also indicated: \*\*\*  $p < 0.001$  (two-way ANOVA test). We should also note the significant difference of behavior between coarse (SiC C1 / C2) and fine particles (SiC F1 / F2), and between SiC I and coarse / fine particles ( $p < 0.001$ ).

Figure 6 – Development of the silica layer during oxidation. FEG-SEM images of SiC particles embedded in a resin (diallylpthalate): (a) non-oxidized particles, (b) particles oxidized at 1200°C/10h in air. Large particles are illustrated to emphasize the nature of the particle surface, they are not representative of the whole powder sample which was constituted by smaller particles (see Table 1).

Figure 7 – Influence of different thermal treatments on the cytotoxicity of two SiC microparticles SiC C1 (A) and SiC F1 (B) determined by the LDH release. Results are means of 3 independent experiments. Standard deviation and statistically significant differences from the original powder (SiC C1 and SiC F1 respectively) are also indicated: \*\*\*  $p < 0.001$  (one-way ANOVA test).

Figure 8 – Pro-inflammatory effect of the two SiC microparticles SiC C1 (A) and SiC F1 (B) after different thermal treatments determined by the TNF $\alpha$  production. Results are means of 3 independent experiments. Standard deviation and statistically significant differences from the original powder (SiC C1 and SiC F1 respectively) are also indicated: \*\*\* p<0.001 (one-way ANOVA test).

Figure 9 – Acute oxidative stress induced by the two SiC microparticles SiC C1 (A) and SiC F1 (B) after different thermal treatments as assessed by the H<sub>2</sub>O<sub>2</sub> production. Results are means of 3 independent experiments. Standard deviation and statistically significant differences from the original powder (SiC C1 and SiC F1 respectively) are also indicated: \*\*\* p<0.001 (one-way ANOVA test).

Figure 10 – Influence of different thermal treatments of two SiC microparticles (SiC C1 and SiC F1) on the free radical release A) HO $\cdot$  and B) COO $\cdot$ , as determined by electron paramagnetic resonance. Results are means of 3 independent experiments. Standard deviation and statistically significant differences from the original powder (SiC C1 and SiC F1 respectively) are also indicated: \*\*\* p<0.001 (one-way ANOVA test).

**Figure 1**

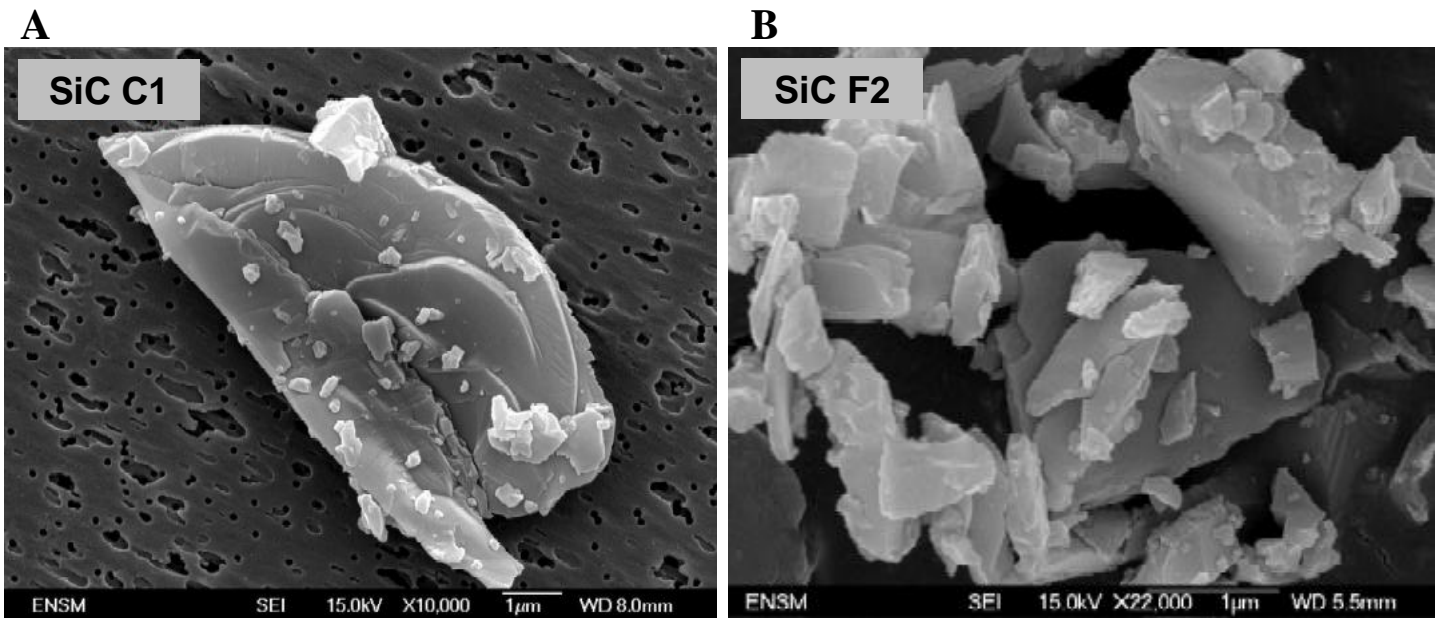
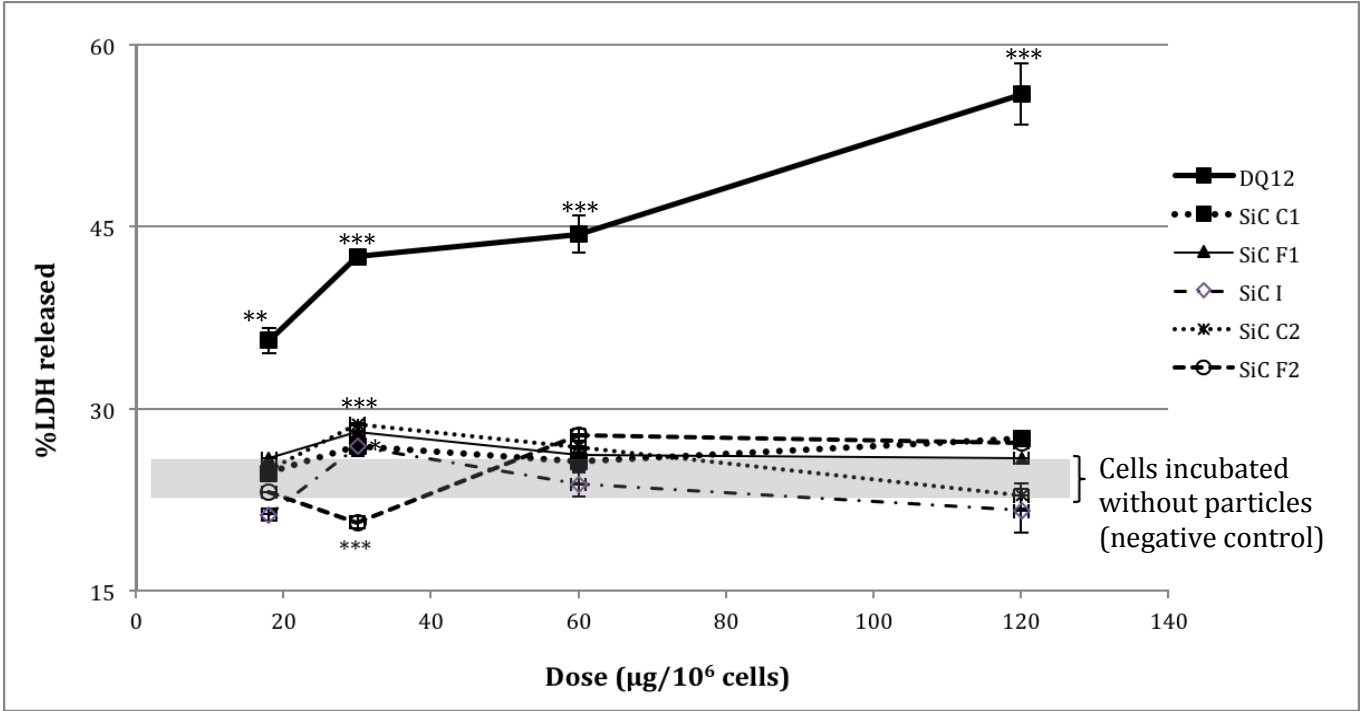
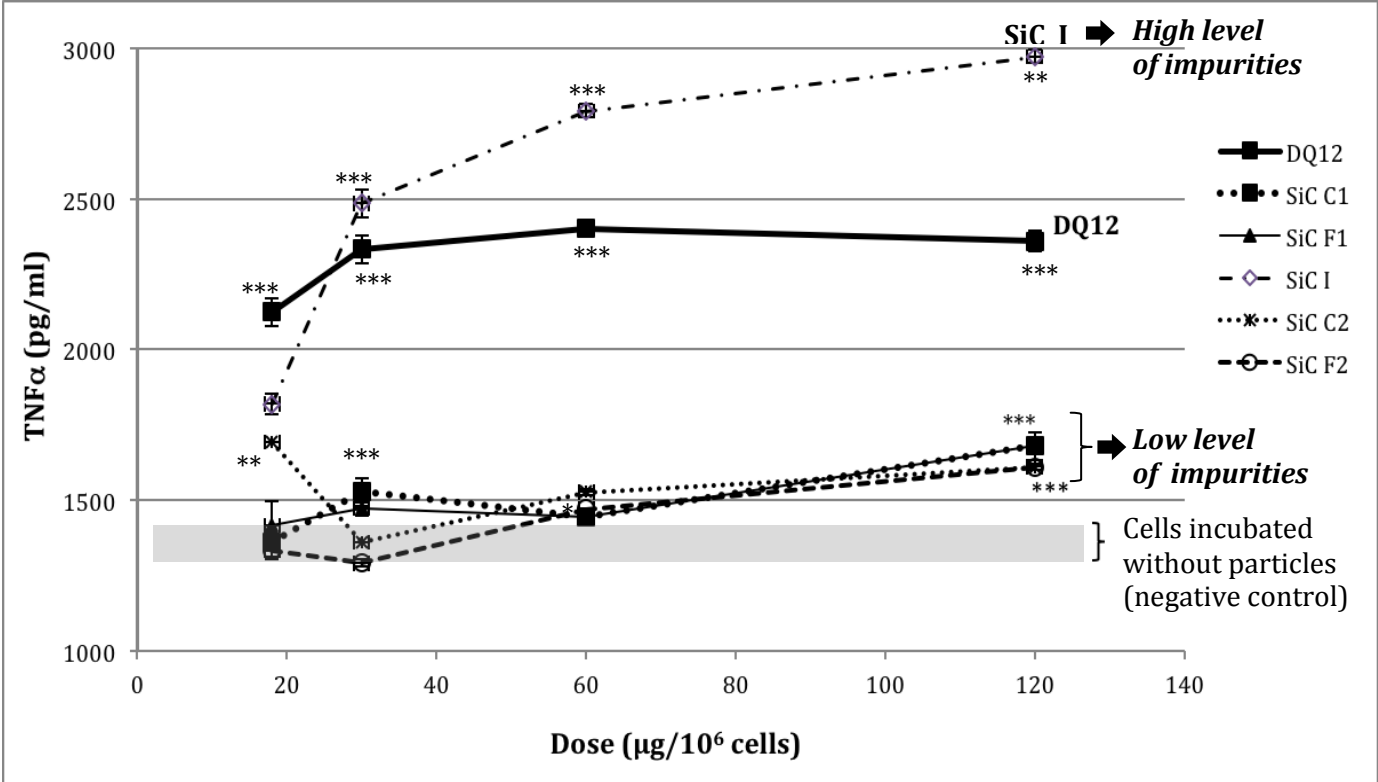


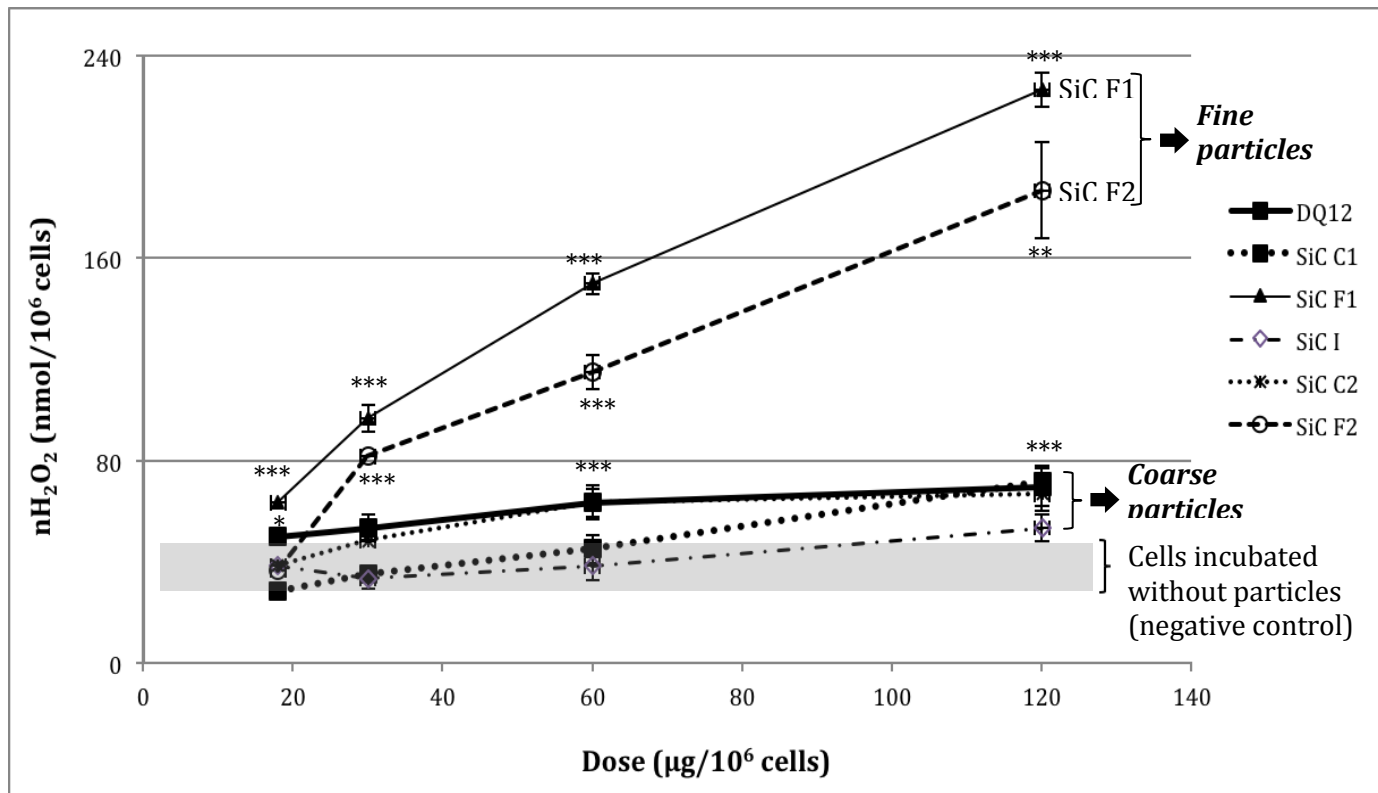
Figure 2



**Figure 3**

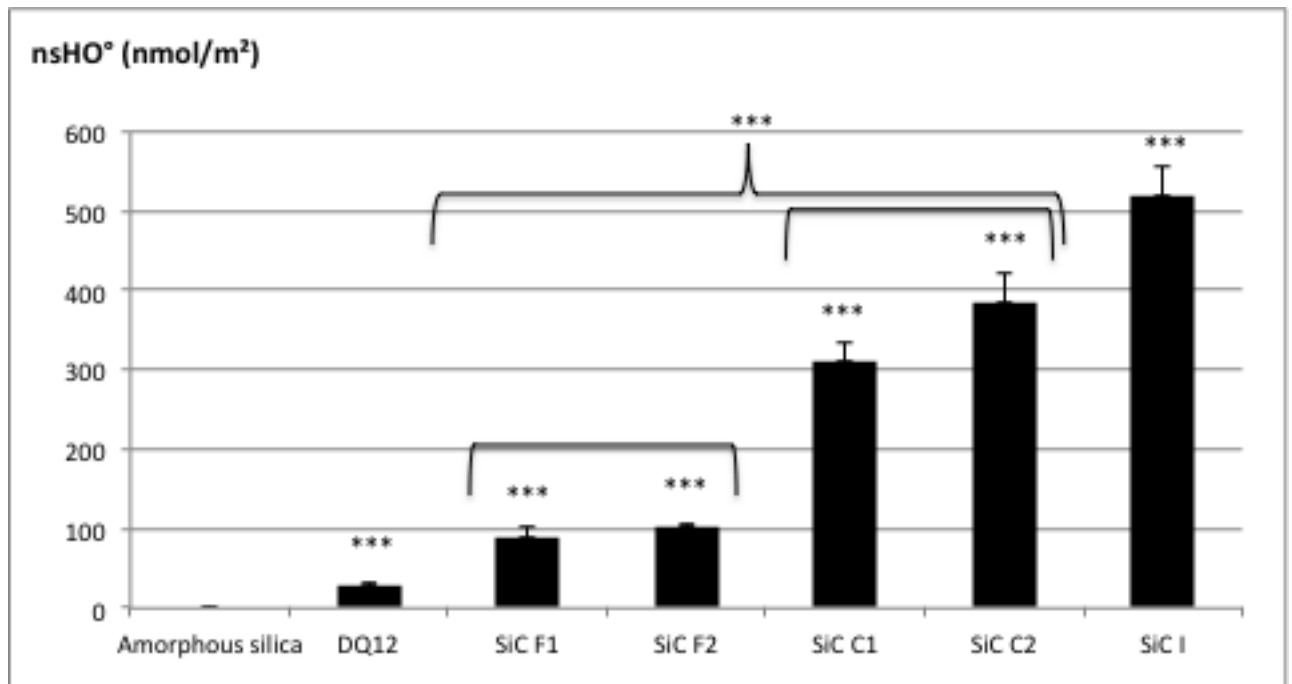


**Figure 4**



**Figure 5**

**A**



**B**

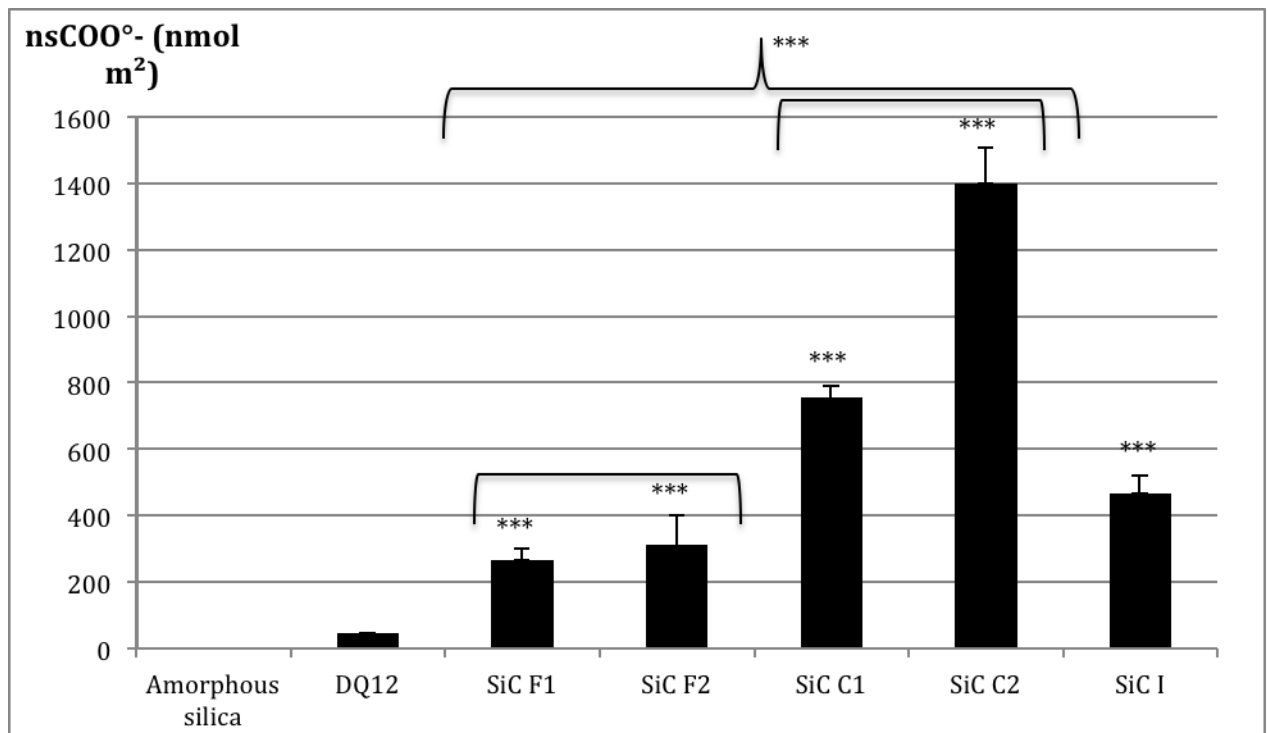




Figure 6

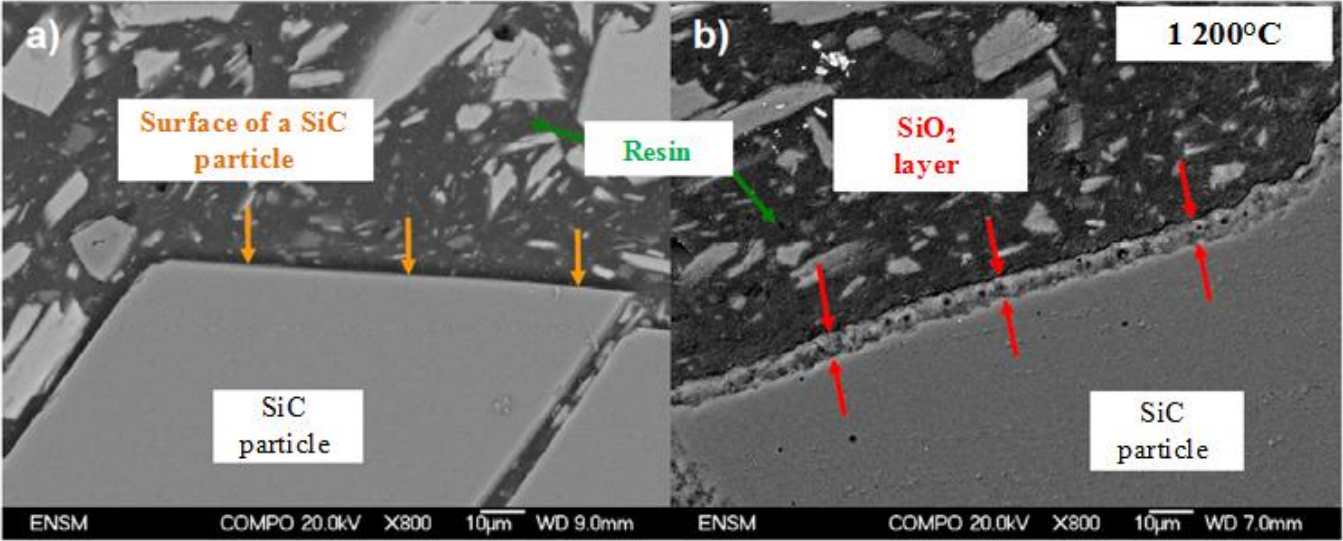
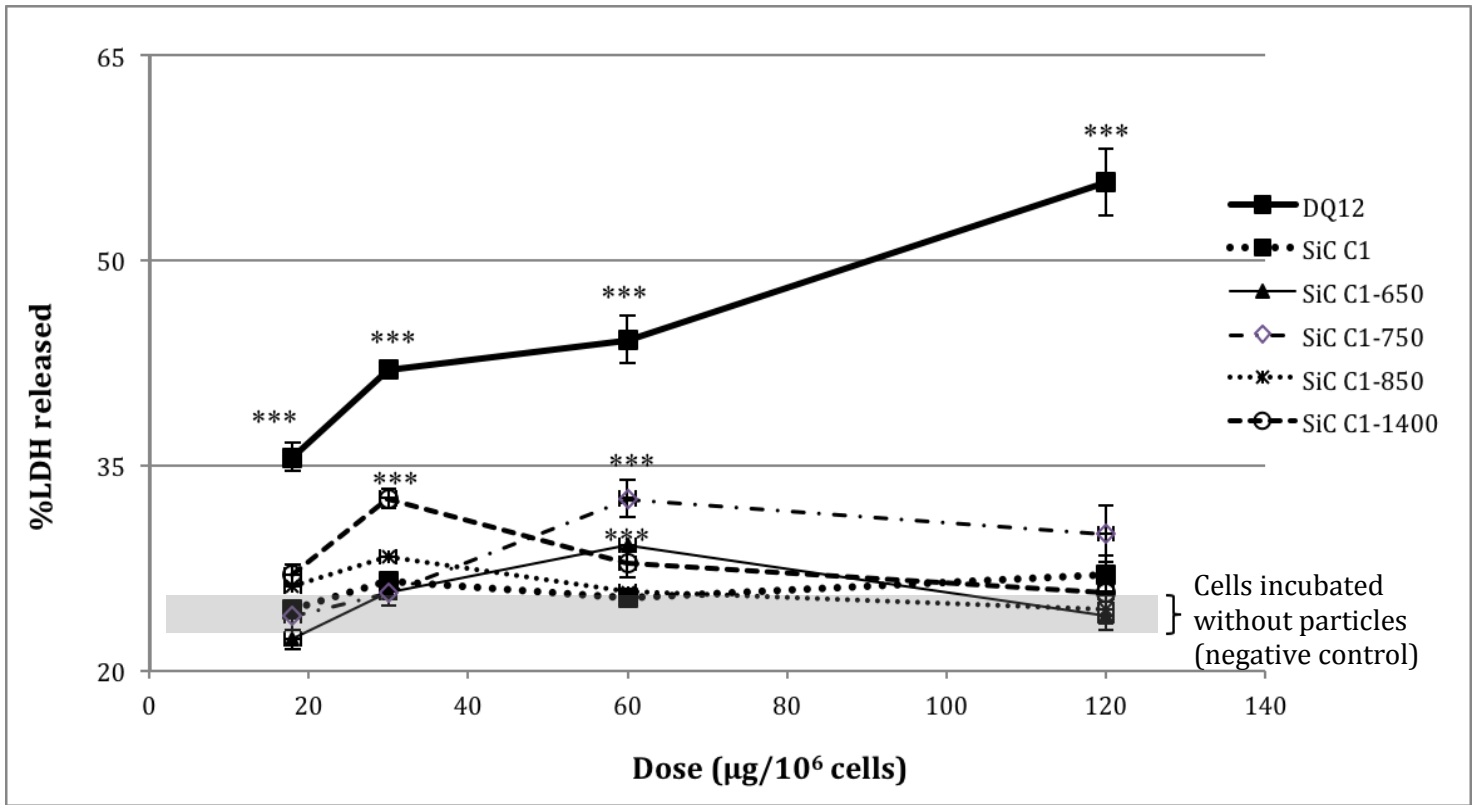
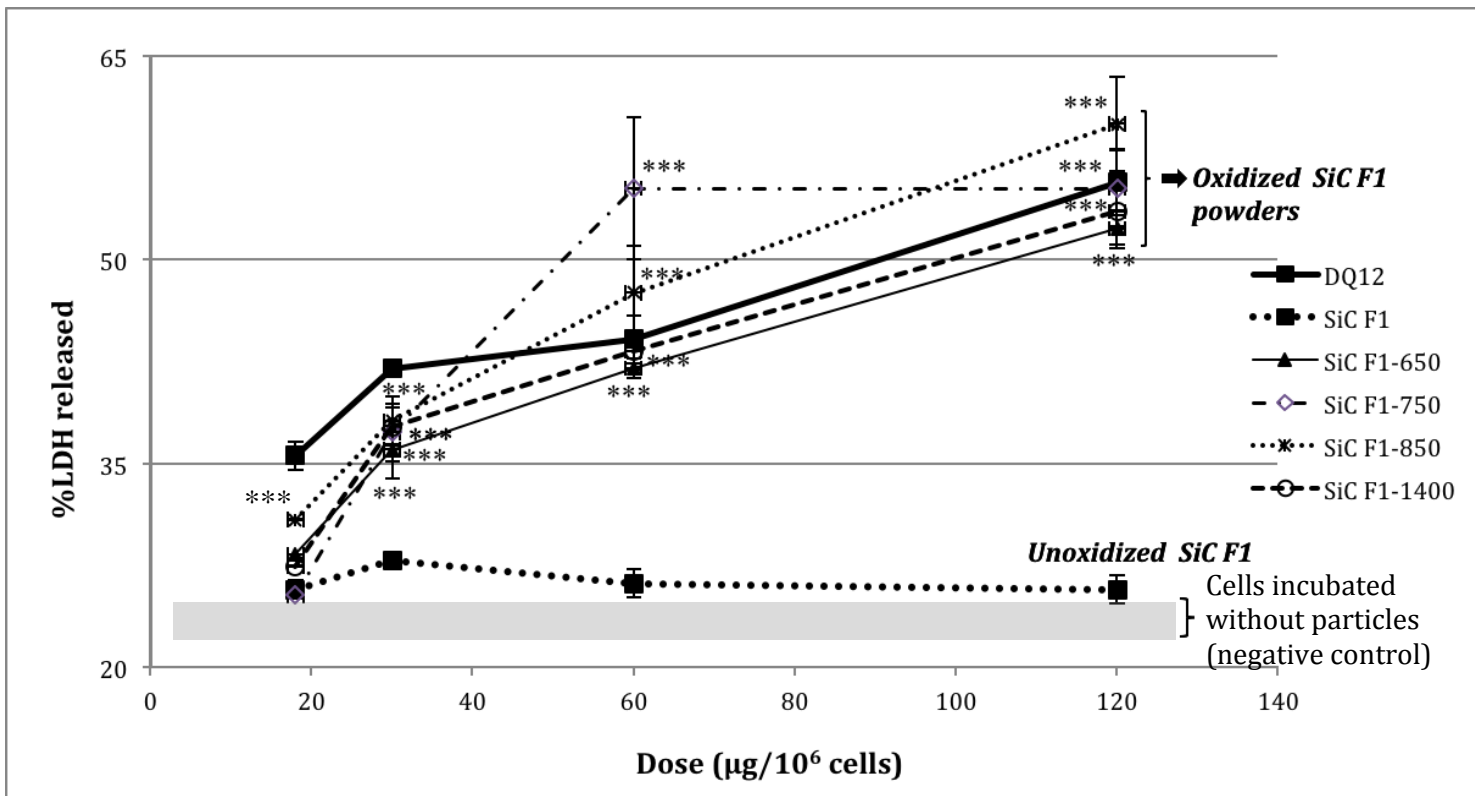


Figure 7

A

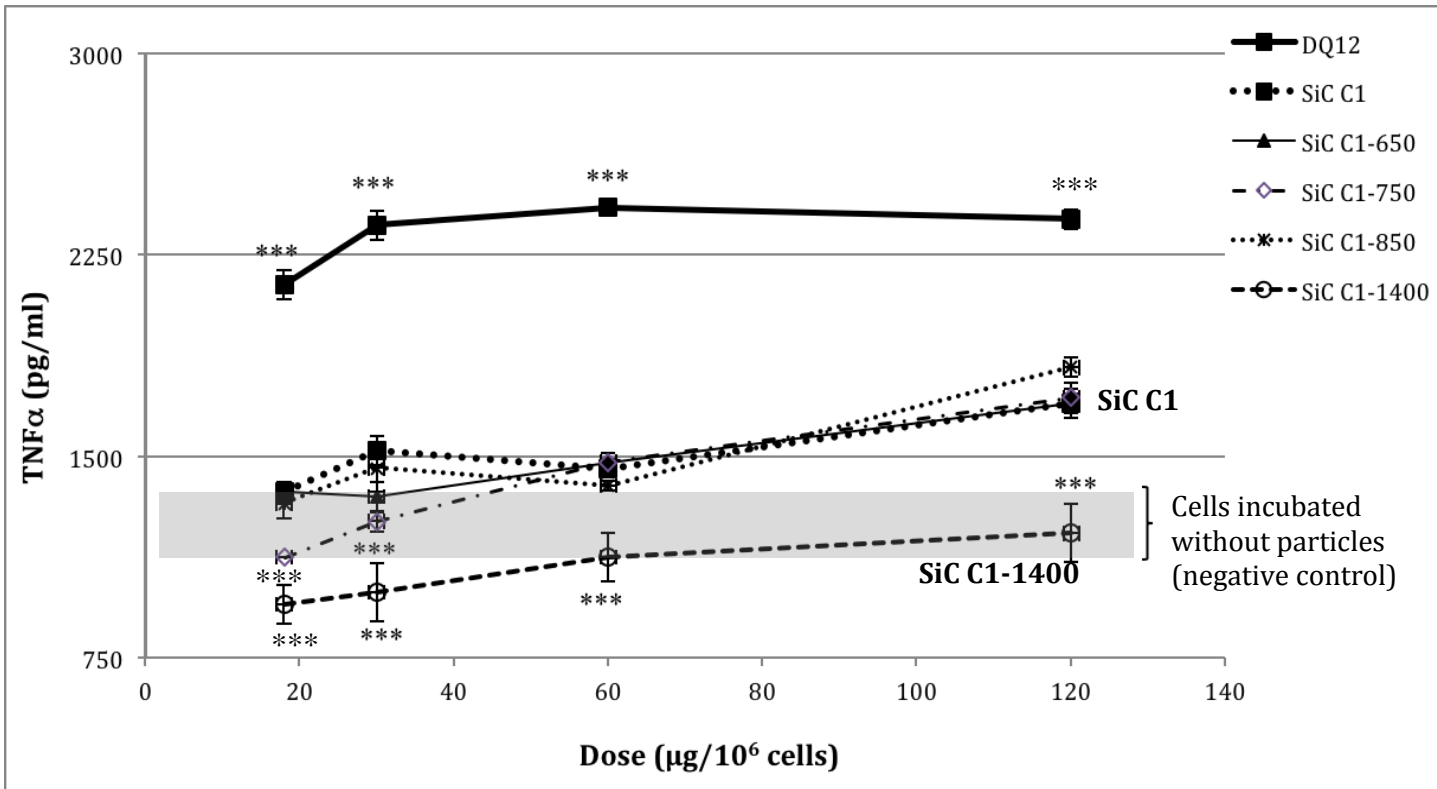


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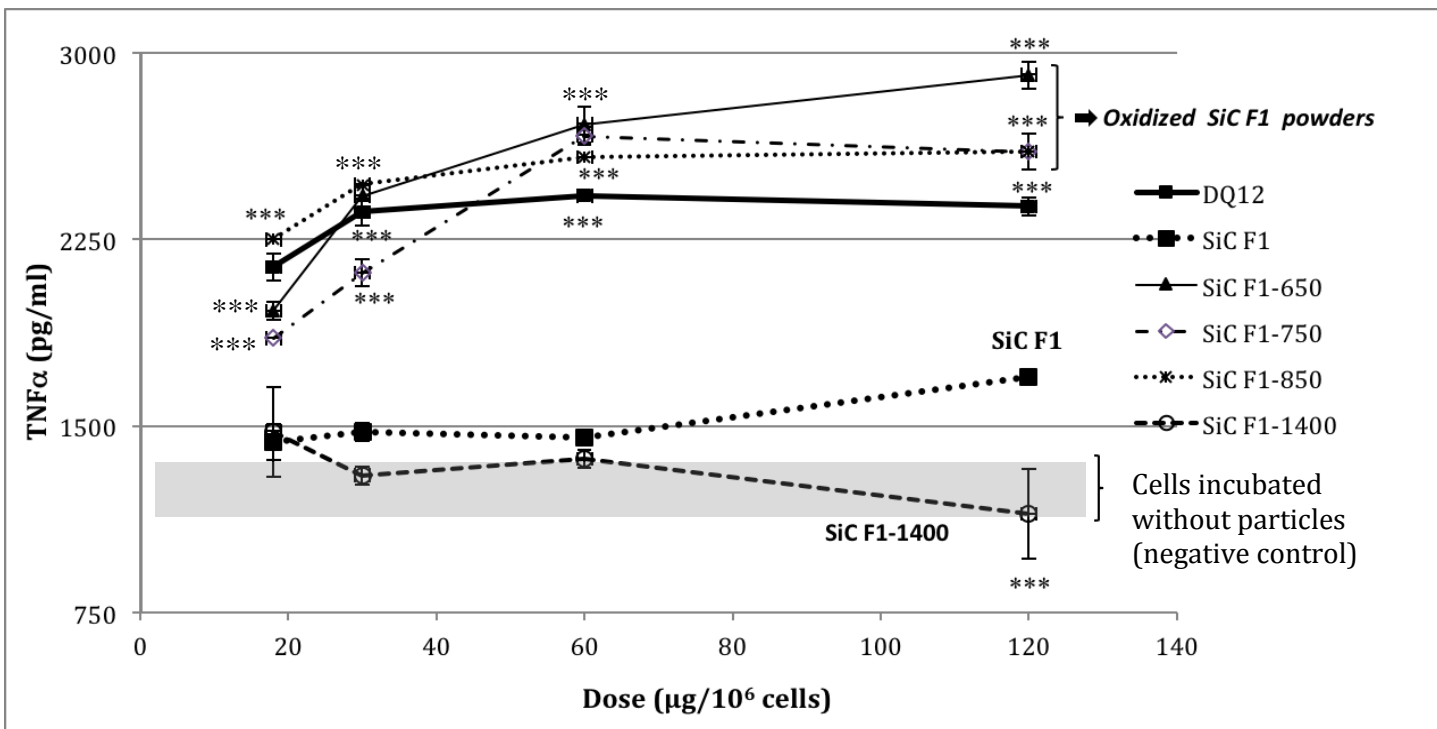


**Figure 8**

**A**

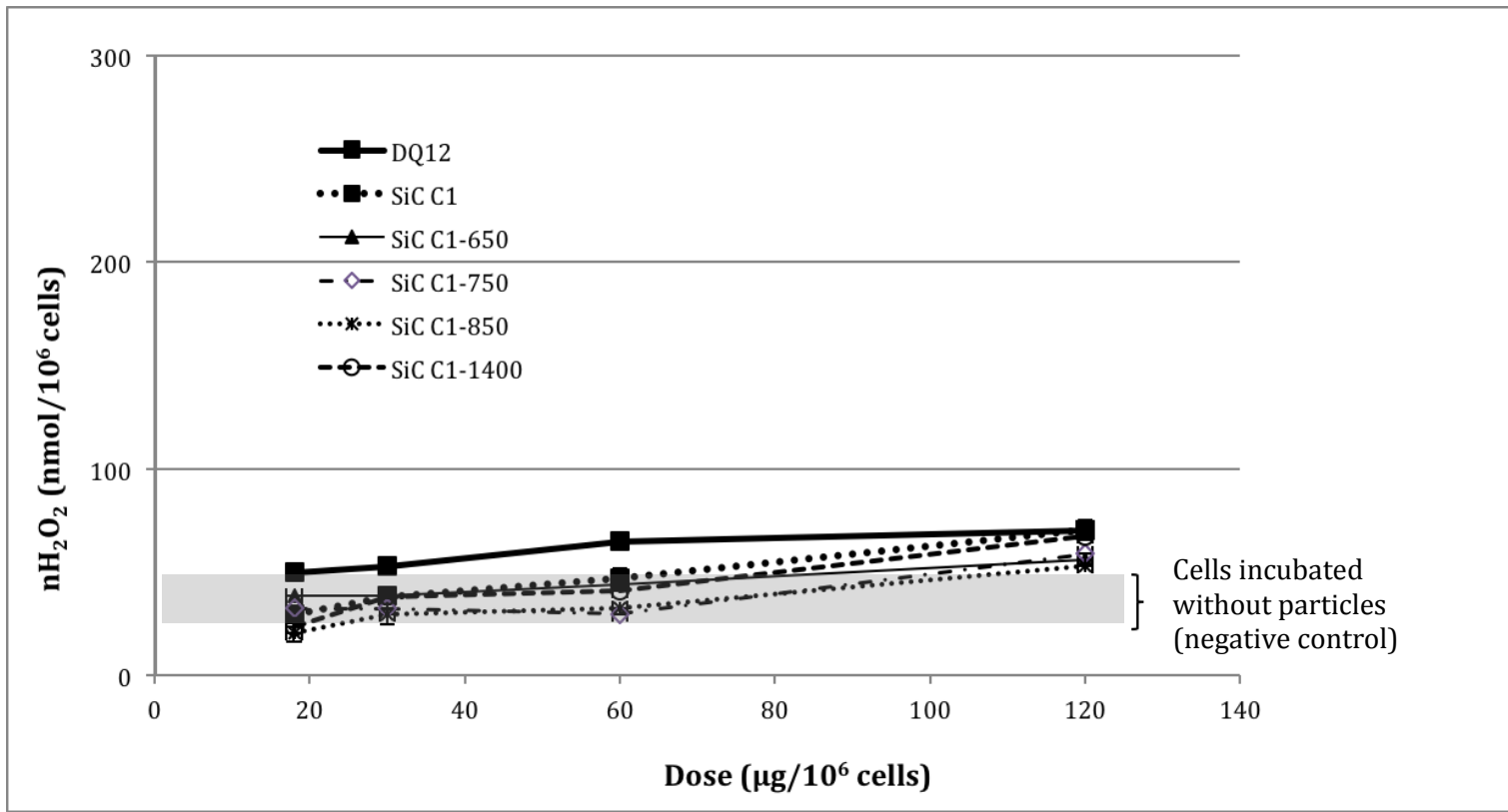


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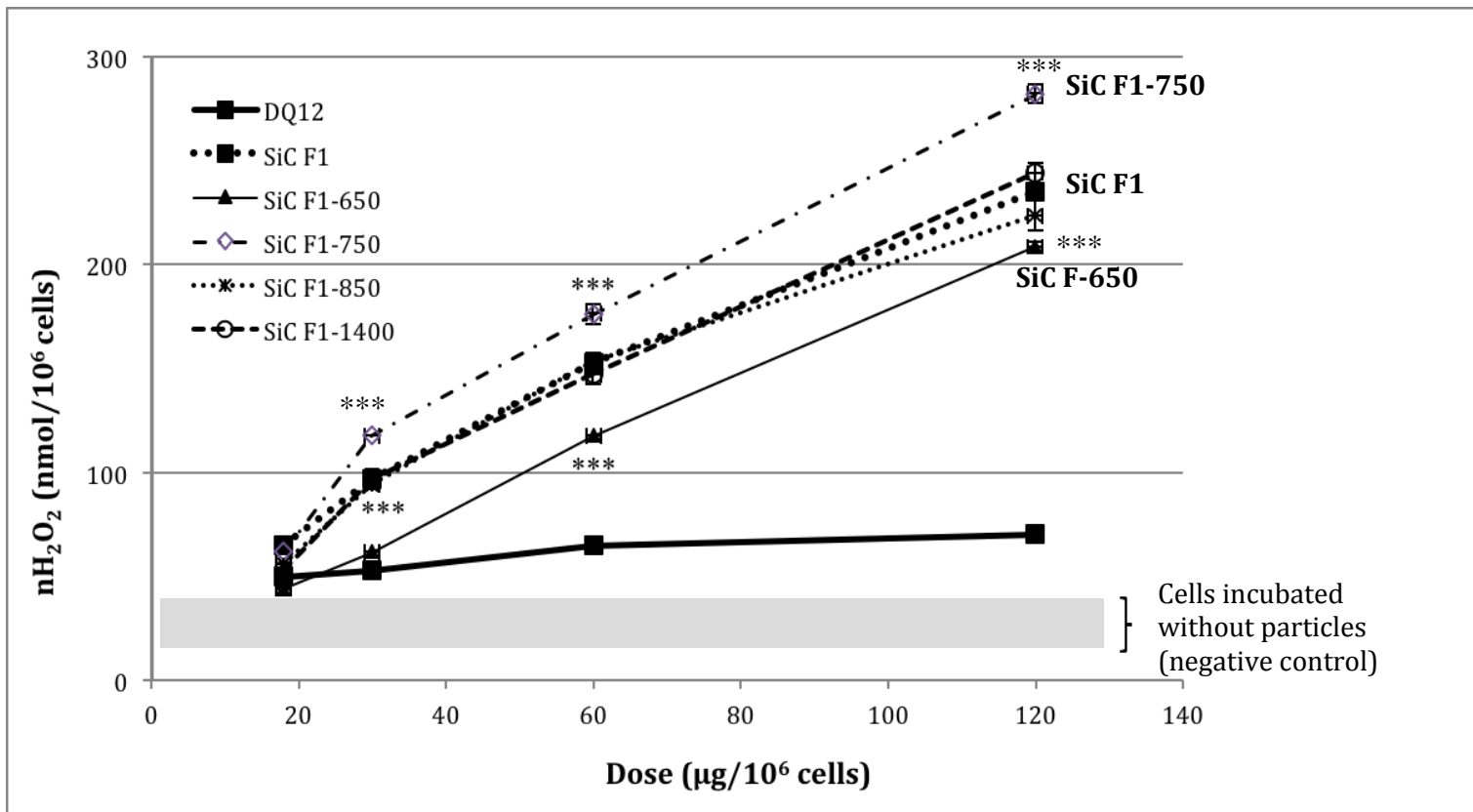


**Figure 9**

**A**

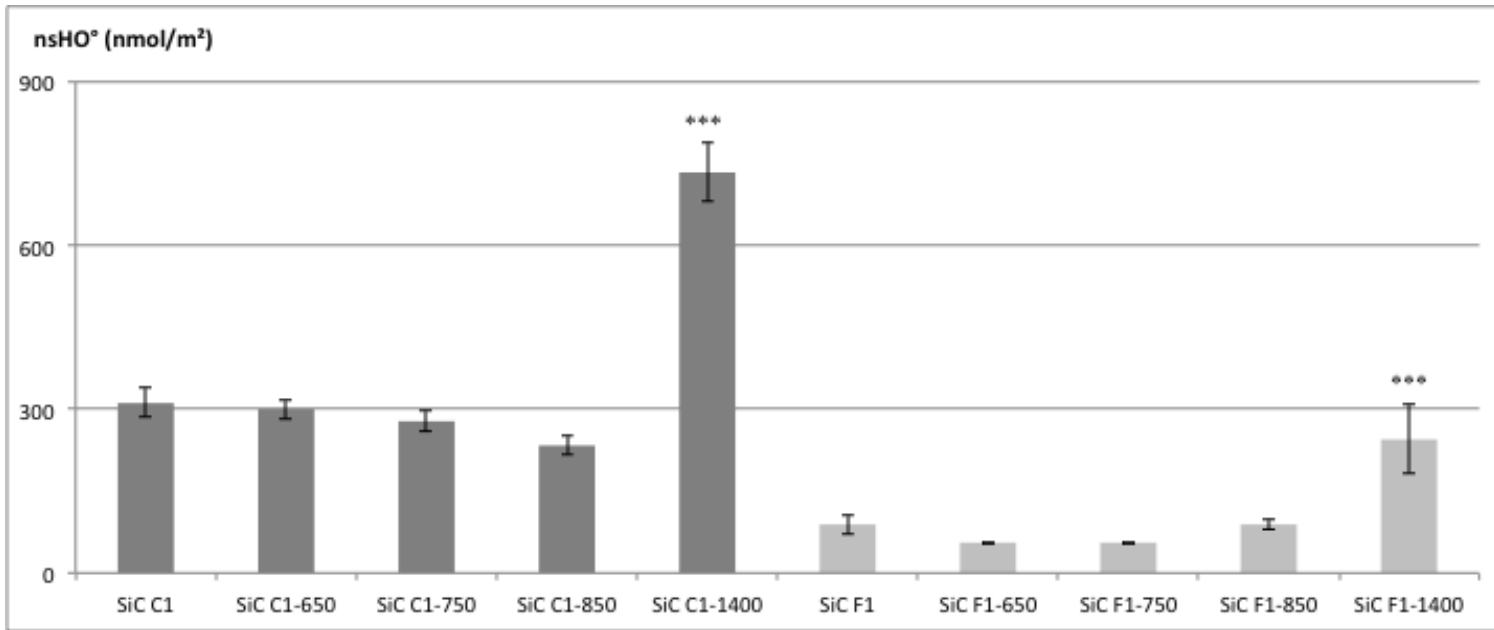


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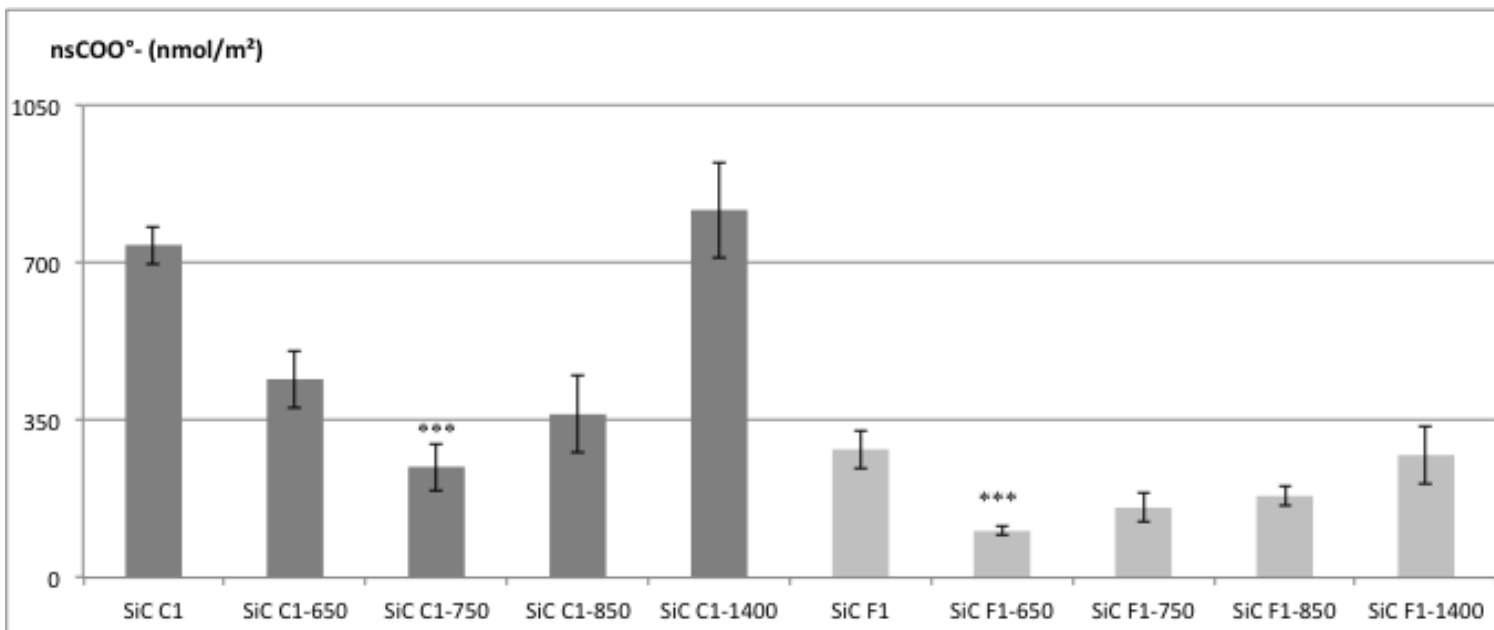


**Figure 10**

**A**



**B**



**Table 1** – Physico-chemical characteristics of different SiC microparticles

Sample	SSA (m <sup>2</sup> /g)	Median diameter D <sub>50</sub> (μm)	Cristallite phases	O1s (% atomic)	C/Si (atomic ratio)	Fe (ppm)	Al (ppm)	Schematic representation
SiC C1	4.0	2,5	SiC-6H (91%) SiC-4H (7%) SiC-15R (<1%)	17 (presence of a SiO <sub>2</sub> layer)	0,98	2370	350	
SiC F1	11.0	0,5	SiC-6H (91%) SiC-4H (7%) SiC-15R (2%)	22 (presence of a SiO <sub>2</sub> layer)	1	1570	560	
SiC I	3.0	6	SiC-6H (53%) SiC-4H (7%) SiC-15R (5%) SiO <sub>2</sub> quartz (9%) SiO <sub>2</sub> cristobalite (5%)	23 (presence of a SiO <sub>2</sub> layer)	1,66	20 000	1300	
SiC C2	3.5	2,5	SiC-6H (90%) SiC-4H (7%) SiC-15R (2%)	17 (presence of a SiO <sub>2</sub> layer)	0,99	2230	730	
SiC F2	8.5	0,8	SiC-6H (90%) SiC-4H (3%) SiC-15R (7%)	23 (presence of a SiO <sub>2</sub> layer)	0,98	1370	0	