Poisson-Gaussian noise parameter estimation in fluorescence microscopy imaging
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In this paper, we propose a novel approach based on an Expectation-Maximization (EM) algorithm, following our previous work in [13]. We focus on fluorescence imaging systems, especially in the field of confocal microscopy and so-called macroscopy systems [14]. Similarly to [8, 12], as input data we use time lapse fluorescence images, which consist of repeated images of motionless specimens at given times. The considered problem is more challenging than the one investigated in [13] due to the nonstationarity of the acquired signal caused by photobleaching. This effect is a process of intensity decay in time usually modeled with an exponentially decreasing function [15, 3]. Although other photobleaching forms were also investigated [16], our analysis in this paper is based on the latter model, also known as three-parameter exponential model [17]. More specifically, in order to characterize the dependency between Poisson noise and photobleaching, we adopt the same model as the one presented in [6]. However, we relax the assumption of constant bleaching decay for the whole image, which is not realistic according to our experiments in the last section of this paper. Since the EM optimization framework is not guaranteed to converge to a global minimizer of the negative log-likelihood, its behavior can be improved by carefully setting its initialization. Usually the choice of a good starting value is discussed in the context of specific applications [18, 19, 20, 13]. We address this key problem for Poisson-Gaussian parameter estimation in the presence of photobleaching by proposing an adequate moment based initialization. Moreover, we provide an extension of the EM approach developed in [13] in order to allow us to jointly estimate Poisson-Gaussian noise parameters, to reconstruct the original signal and to estimate its photobleaching rates.

The paper is organized as follows. We provide a description of the noise identification problem from a time-series standpoint in Section 2. We then present the proposed iterative method in Section 3. Section 4 illustrates the algorithm performance on synthetic data and real confocal macroscopic image sequences obtained from biological samples. Section 5 concludes the paper.

2. NOISE MODEL

2.1. Adopted scheme

We consider data \((u_s)_{1 \leq s \leq S}\) where \(s\) corresponds to a location index (e.g. locating pixel \((x, y)\) in 2D or voxel \((x, y, z)\) in 3D), which are corrupted with a Poisson-Gaussian noise, and for which we observe \(T\) realizations. Each realization will be indexed by the time index \(t \in \{1, \ldots, T\}\). Such a framework leads us to the following model:

\[
(\forall s \in \{1, \ldots, S\}) (\forall t \in \{1, \ldots, T\}) \quad R_{s,t} = \alpha Q_{s,t} + W_{s,t} \quad (1)
\]
where \( \alpha \in \mathbb{R} \) is a scaling parameter and \( R_{s,t} \) is the observed random variable at time \( t \) and location \( s \). In the above model, the following auxiliary random variables intervene:

\[
Q_{s,t} \sim \mathcal{P}(u_s e^{-k_s t}) \\
W_{s,t} \sim \mathcal{N}(c, \sigma^2)
\]

where \((u_s)_{1 \leq s \leq S} \in [0, +\infty)^S\) is the “clean” image (possibly resulting from a blur of the original image and some offset), \((k_s)_{1 \leq s \leq S} \in (0, +\infty)^S\) denote the photobleaching rates, and \(c \in \mathbb{R}\) (resp. \( \sigma > 0 \)) is the mean value (resp. standard-deviation) of the Gaussian noise.

### 2.2. Considered problem

The problem is to estimate \( u = (u_s)_{1 \leq s \leq S}, k = (k_s)_{1 \leq s \leq S}, \alpha, c, \) and \( \sigma^2 \) from the available observation vector \( r = (r_{s,t})_{1 \leq s \leq S, 1 \leq t \leq T} \), which is a realization of the random field \( R = (R_{s,t})_{1 \leq s \leq S, 1 \leq t \leq T} \). We have thus \( 2S + 3 \) parameters to estimate. We define the vector of unknown parameters as \( \theta = (u, k, \alpha, c, \sigma^2) \).

In the following, it is assumed that \( u \) is deterministic and that \( Q = (Q_{s,t})_{1 \leq s \leq S, 1 \leq t \leq T} \) and \( W = (W_{s,t})_{1 \leq s \leq S, 1 \leq t \leq T} \) are mutually independent random fields. In addition, the components of \( W \) (resp. \( Q \)) are assumed to be independent. These assumptions let us define the cumulant of order \( n \) as \( \kappa_n[R_{s,t}] = \alpha^n \kappa_n[Q_{s,t}] + \kappa_n[W_{s,t}] \). This leads to the following results:

- mean value: \( \kappa_1[R_{s,t}] = \mathbb{E}[R_{s,t}] = \alpha e^{-k_s t} u_s + c \)
- variance: \( \kappa_2[R_{s,t}] = \text{Var}[R_{s,t}] = \alpha^2 e^{-2k_s t} u_s + \sigma^2 \)
- higher-order cumulants: \( n \geq 3, \kappa_n[R_{s,t}] = \alpha^n u_s e^{-k_s t} \)

### 3. NOISE ESTIMATION METHOD

#### 3.1. Moment based method

Several procedures may be derived from (4), (5), and (6) in order to estimate \( \theta \), but they are not equally reliable. For example, according to our observations, \( \kappa_1[R_{s,t}] / \kappa_2[R_{s,t}] \) does not provide a very accurate estimate of \( \alpha \). Thus, we propose to define preliminary estimates of \( (k_s)_{1 \leq s \leq S}, c \) and \( (a_s = \alpha u_s)_{1 \leq s \leq S} \) by noticing that (4) can be reexpressed as

\[
R_{s,t} = a_s e^{-k_s t} + c + E_{s,t}
\]

where \((E_{s,t})_{1 \leq s \leq S, 1 \leq t \leq T}\) are independent zero-mean random variables. This suggests to employ a nonlinear least squares approach to compute estimates \( \hat{\alpha} = (\hat{a}_s)_{1 \leq s \leq S}, \hat{k} = (k_s)_{1 \leq s \leq S}, \hat{c}\) of the parameters:

\[
(\hat{\alpha}, \hat{k}, \hat{c}) = \arg\min_{a, k, c} \sum_{s=1}^{S} \sum_{t=1}^{T} \omega_{s,t} \left( r_{s,t} - c - a_s e^{-k_s t} \right)^2
\]

where \((\omega_{s,t})_{1 \leq s \leq S, 1 \leq t \leq T}\) are positive weights. In order to efficiently solve the associated minimization problem, we propose to use an alternating optimization method (see Algorithm 1). For every \( s \in \{1, \ldots, S\} \), the minimization subproblem to be solved at each iteration reduces to a linear least squares one for a given value of \( k_s \). The minimization procedure thus reduces to a one-variable search (over \( k_s \)) which can be performed by standard numerical methods, e.g. the Nelder-Mead simplex method [21].

The estimates provided by this method are sufficiently stable, as only first order statistics are used. These results allow us to provide simple estimates of the remaining parameters. Indeed, by rewriting (5) as

\[
\mathbb{E}[(R_{s,t} - \mathbb{E}[R_{s,t}])^2] = \alpha a_s e^{-k_s t} + \sigma^2,
\]

the following least squares estimate for \( \alpha \) can be derived:

\[
\hat{\alpha} = \frac{\sum_{s=1}^{S} \sum_{t=1}^{T} \nu_{s,t} m_{s,t} - \sum_{s=1}^{S} \nu_{s,t} \sum_{t=1}^{T} \nu_{s,t} m_{s,t}}{\sum_{s=1}^{S} \nu_{s,t} m_{s,t}^2 - \sum_{s=1}^{S} \nu_{s,t}^2 m_{s,t}^2},
\]

where \((\nu_{s,t})_{1 \leq s \leq S}\) are positive weights, \( \nu = T \sum_{s=1}^{S} \nu_{s,t} \) and

\[
(\forall s \in \{1, \ldots, S\}) \quad m_{s,t} = \hat{\alpha}_s e^{-\hat{k}_s T} \frac{1 - e^{-\hat{k}_s T}}{1 - e^{-k_s T}}(12)
\]

with, for every \( t \in \{1, \ldots, T\}, v_{s,t} = (r_{s,t} - \hat{a}_s e^{-\hat{k}_s t} - \hat{c})^2 \). Then, the estimate of \( u \) is given by:

\[
(\forall s \in \{1, \ldots, S\}) \quad \hat{u}_s = \frac{\hat{\alpha}_s}{\hat{\alpha}}.
\]

Finally, the estimation process is completed by computing:

\[
\hat{\sigma}^2 = \frac{\sum_{(s,t) \in \mathcal{I}} v_{s,t}}{\sum_{(s,t) \in \mathcal{I}} v_{s,t}}
\]

where

\[
\mathcal{I} = \{(s,t) \in \{1, \ldots, S\} \times \{1, \ldots, T\} | v_{s,t} - \hat{\alpha} \hat{a}_s e^{-\hat{k}_s t} \geq 0\}
\]

#### 3.2. Refined estimation

The main limitation of the previous moment based method is that the unknown parameters are not jointly estimated. Due to this fact, we may face large error propagation with respect to the estimation of some parameters. Thus, similarly to the work in [13], we propose to improve the moment based method results by resorting to an EM approach. The proposed noise identification procedure is summarized in Fig. 1.

![Flowchart of the proposed noise identification method.](image-url)
necessary to include this effect into this framework. More precisely, in the \((n + 1)\)-th maximization step, it can be shown that, for every \(s \in \{1, \ldots, S\}\), the photobleaching effect \(k_s^{n+1} = -\ln x^{n+1}(s)\) where \(x^{n+1}(s)\) is the solution in (0, 1) of the polynomial equation:

\[
(1 + T x^{T+1} - (T + 1)x^T) \sum_{t=1}^{T} E_{Q|R=r,\theta(n)}[Q_{s,t}] = (1 - x - x^T + x^{T+1}) \sum_{t=1}^{T} t E_{Q|R=r,\theta(n)}[Q_{s,t}].
\]

We propose to compute \(x^{n+1}\) from (15) using Halley’s algorithm [22]. Then, \(u\) can be derived as follows

\[
(\forall s \in \{1, \ldots, S\}) \quad u_s^{n+1} = \frac{1 - x^{n+1}(s)}{x^{n+1}(s)(1 - [x^{n+1}(s)]^T)} \sum_{t=1}^{T} E_{Q|R=r,\theta(n)}[Q_{s,t}].
\]

Finally, the maximization step is completed by update formulas for \(\alpha^{n+1}(s,t), \eta^{n+1}(s,t), \) and \(\sigma^{n+1}(s,t), \) which are unchanged with respect to the stationary case described in [13]. In the \(n\)-th expectation step, taking into account the photobleaching effect yields the following expressions:

\[
E_{Q|R=r,\theta(n)}[Q_{s,t}] = \frac{\zeta_s^{(n)}}{\eta_s^{(n)}}
\]

\[
\zeta_s^{(n)}(s,t) = \sum_{q_s,t=1}^{\infty} e^{-\frac{(x_s,t-\alpha^{(n)}q_s,t-\alpha^{(n)}e^{(n)}q_s,t)}{2\sigma^2(n)}} \frac{(u_s^{(n)}q_s,t-\alpha^{(n)}q_s,t)}{(q_s,t-1)!} e^{-\alpha^{(n)}q_s,t}
\]

\[
\eta_s^{(n)}(s,t) = \sum_{q_s,t=0}^{\infty} e^{-\frac{(x_s,t-\alpha^{(n)}q_s,t-\alpha^{(n)}e^{(n)}q_s,t)}{2\sigma^2(n)}} \frac{(u_s^{(n)}q_s,t)}{q_s,t!} e^{-\alpha^{(n)}q_s,t}
\]

### 4. SIMULATION EXAMPLES

In this section, we present experiments on both synthetic and real data in order to demonstrate the performance of the proposed approach. In particular, the simulations on synthetic data allow us to evaluate the reliability of our algorithm (Section 4.1) and the real data case study illustrates its potentials in microscopy applications (Section 4.2).

#### 4.1. Synthetic data validation

We evaluate the proposed algorithms using \(S = 200\) randomly generated \(u_s\) values uniformly distributed over \([0, 150]\) and \(k_s\) values uniformly distributed over \([10^{-4}, 10^{-3}]\). Signal \((r_s,t)\leq s \leq 8, 1 \leq t \leq T\) is generated according to (1) for \(c = 10, \alpha = 30, \sigma^2 = 100\) and \(T = 180\). The algorithm performance is measured by the SNR defined as the average of \(10 \log_{10}(P)\) with

\[
P = \frac{(ST)^{-1} \sum_{(s,t)}(u_s e^{-k_s t})^2}{\sum_{(s,t)}(u_s e^{-k_s t} - \tilde{u}_s e^{-\tilde{k}_s t})^2}
\]

computed over 50 noise realizations, where the estimated values are designated with a hat. Moreover, we examine the estimator properties by presenting the bias and standard deviation of the resulting noise parameters \(\alpha, c, \text{ and } \sigma\).

The results presented in Table 1 indicate that in the first step of the algorithm (Fig. 1) a majority of the unknown parameters are identified accurately. As expected, the estimates are further improved in the second step by EM, achieving high accuracy, indicated by high SNR values, and low standard deviation of the estimated noise parameters.

#### 4.2. True data results

In the real data case, noise parameter identification and true image intensity reconstruction follow registration of time lapse series of images. Images were acquired using a macro confocal laser scanning microscope (Leica TCS-LSI) from a cross-section through the rhizome of Convallaria majalis (Lily of the Valley). Measurements were done on images taken with the following settings: pinhole 1.06 airy, 800 Hz scan speed, PMT Offset -4.3%, PMT Gain 848, excitation line 488nm, and emission range 499nm-690nm. The reported signal intensities at each location within the biological sample result from natural occurring autofluorescence caused by different compounds like lignin and other phenolics. As such, the process of bleaching and decrease in image intensity is complex and cannot be fitted with a mono-exponential decay [23].

The processed time lapse sequence consists of 180 images with 12-bit resolution of size \(128 \times 128\), which translates into \(T = 180\) and \(S = 16384\). The first and last images of the sequence are illustrated in Fig. 2 (a) and Fig. 2 (b), respectively. One can observe that, due to the photobleaching effect, some parts of the image \(r_s, t\) (Fig. 2 (a)) are not visible in the last image \(r_{s,180}\) (Fig. 2 (b)), e.g. quadrant 4. Weakly fluorescing components are lost when calculating the mean over all realizations (Fig. 2 (c)), while they are well preserved and less oversmoothed when applying our algorithm (Fig. 2 (d)). Besides these visual results, our algorithm also allows us to establish the parameters of the noise model (1), which are given as 25.8 \(P(\tilde{u}_s e^{-\tilde{k}_s t}) + N(8, 119)\). The plots in Fig. 3 illustrate the change of the measured and reconstructed signals along \(t\), while \(s\) is fixed. They show the variety of acquired signals. For instance, the signal presented in Fig. 3(b) corresponds to a weak photobleaching effect, while in Fig. 3(c), a strong photobleaching effect is identified. One can observe that the bleaching curves are a good fit for the series of measured data points. The identified bleaching rates \(k_s\) belong to the set \([0, 3.9 \times 10^{-6}]\) Hz, and \(\tilde{u}_s\) values lie in \([0, 147]\). This example illustrates the properties of our method applied to a fluorescence imaging system.

#### 5. CONCLUSIONS

The present study has addressed the problem of Poisson-Gaussian noise parameter identification from time lapse data, taking into account the photobleaching effect. We have proposed new, fully automated, two-step approach dealing with this problem. Our experiments illustrate that this approach leads to a very accurate image reconstruction as illustrated by Fig. 3(d). The proposed algorithm has a direct application in the calibration of fluorescence imaging systems like confocal microscopy and as a preliminary step in image restoration procedures. One should note that one limitation of our proposed approach is the requirement for a stationary specimen. To overcome this problem, a motion compensation scheme can be used.
6. REFERENCES


