Thermocapillary valve for droplet production and sorting
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Microfluidic droplets have been proposed as microreactors with the aim to provide high performance tools for biochemistry. Individual drops may be viewed as containing one digital bit of information and the manipulation of a large number of slightly differing drops would allow the testing of a large library of genes rapidly and with a small total quantity of material [1]. In microchannels, drops are produced and transported using a carrier fluid [2] and typical channel sizes allow the manipulation of volumes in the picoliter range. Surfactant in the carrier fluid prevents cross-contamination of the drops through wall contact or fusion [3, 4]. However, while the geometry of the microchannel may be used to determine the evolution of drops and their contents [3–5], the implementation of real lab-on-a-chip devices hinges on the active control of drop formation and its evolution, which remains elusive.

In this letter, we remedy the situation by demonstrating experimentally how a focused laser can provide precise control over droplets through the generation of a thermocapillary flow. In doing so, we develop the first theoretical model of a droplet subjected to localized heating, yielding a general understanding of the forces acting on the drop and a scaling law which favors miniaturization. A carrier fluid is still used for the formation and transport of drops but the effects of geometry are augmented with a local thermal gradient produced by the laser beam, focused through a microscope objective inside the microchannel.

Indeed, moving drops with heat has been a preoccupation of fluid mechanicians since the initial work of Young et al [6]. Although originally motivated by microgravity conditions where surface effects are dominant [6, 7], microfluidics has opened up a new area where bulk phenomena are negligible compared to surface effects. Recently, thermal manipulation of drops or thin films resting on a solid substrate has received the attention of the microfluidics community either through the embedding of electrodes in the solid [8, 9] or through optical techniques [10–12]. However, the physical mechanisms in the transmission of forces when the liquid touches a solid wall are fundamentally different from the case of drops suspended in a carrier fluid, away from the boundaries [13]. The latter case has received little attention despite the advantages that microchannels offer over open geometries.

Our experimental setup consists of a microchannel fabricated using soft lithography techniques [14]. Water and oil (Hexadecane + 2% w/w Span 80, a surfactant) are pumped into the channel at constant flowrates, \( Q_{\text{water}} \) and \( Q_{\text{oil}} \), using glass syringes and syringe pumps. Channel widths are in the range 100 – 500 \( \mu \text{m} \) and the height \( h \) is in the range 25 – 50 \( \mu \text{m} \). Local heating is produced by a continuous Argon-Ion laser (wavelength in vacuum \( \lambda_{\text{Ar+}} = 514 \text{ nm} \)), in the TEM\(_{00}\) mode, focused inside the channel through a \( \times5 \) or \( \times10 \) microscope objective to a beam waist \( \omega_0 = 5.2 \) or 2.6 \( \mu \text{m} \), respectively. The optical approach can be reconfigured in real-time and it allows the manipulation inside small microchannels with no special micro-fabrication. The absorption of the laser radiation by the aqueous phase is induced by adding 0.1% w/w of fluorescein in the water.

A surprising effect is observed when the water-oil interface reaches the laser spot: In the cross-shaped microchannel of Fig. 1, we produce water drops in oil through the hydrodynamic focusing technique in which two oil flows pinch off water droplets at the intersection of the channels. In the absence of the laser, drops of water are produced in a steady fashion and are transported along with the oil down the drain channel, as shown in Figs. 1(a)-(c). When the laser is illuminated, however, the oil-water interface is blocked in place as soon as it crosses the beam. While the typical drop pinching time is \( \tau_d \sim 100 \text{ ms} \) in the absence of the laser, we find that we can block the interface for a time \( \tau_b \) which may be of several seconds, as shown in Figs. 1(d)-(f) (see Ref. [15] for video sequences). During the time \( \tau_b \), the drop shed-
FIG. 1: Microfluidic valve: In a cross-shaped microchannel, the oil flows from the lateral channels and the water enters through the central channel. (a)-(c) In the absence of laser forcing, drops are shed with a typical break-off time [(b) to (c)] of 0.1 s. (d)-(f) When the laser is applied, the interface is blocked for several seconds, producing a larger drop. In image (e), the evolution of the neck shape is shown through a superposition of 100 images (2 s). Exit channel width is 200 μm. Operating conditions are: \( Q_{\text{oil}} = 0.08 \mu\text{L/min}, Q_{\text{water}} = 0.90 \mu\text{L/min}, \) beam power \( P = 80 \text{ mW} \) and beam waist \( \omega_0 = 5.2 \mu\text{m} \).

The drop thus produced is larger, since it has been “inflated” by the laser flow.

In the microchannel shown in Fig. 2, we measured the variation of the blocking time \( \tau_b \) with respect to laser power and forcing position. We observe that \( \tau_b \) increases approximately linearly with the power, above an initial threshold, showing a weak position-dependence of the laser spot. Furthermore, the inset of Fig. 2 shows that the droplet length \( L \) varies linearly with \( \tau_b \), as expected from mass conservation at constant water flowrate \( L = L_0 + \tau_b Q_{\text{water}} / S \), \( L_0 \) being the droplet length without laser and \( S \approx (125 \times 30) \mu\text{m}^2 \) the channel cross section. The best linear fit to the data gives an effective water flowrate \( Q_{\text{water}} = 0.028 \mu\text{L/min} \), close to the nominal value 0.03 \( \mu\text{L/min} \), showing that the water flowrate remains controlled even in presence of the laser forcing. Thus, the optical forcing provides a tunable valve which provides control over droplet timing and size. Similar blocking is observed in a T geometry or if the flows are driven at constant pressure. However, the blocking is only obtained when the light is absorbed, here by using a dye.

We visualize the convection rolls produced by the heating by placing tracer particles in both fluids, as shown in Fig. 3(a) for a drop that is blocked in a straight channel. For pure liquids, the direction of Marangoni flow along the interface is directed from the hot (low surface tension) to the cold (high surface tension) regions. However, the flows in our experiments point towards the laser along the interface, indicating an increase of surface tension with temperature. This is consistent with previous studies that have shown a linear increase of surface tension with temperature in the presence of surfactants [16–18].

One important constraint for practical applications is the amplitude of the temperature rise. Since the materials used in this study have similar thermal properties (thermal diffusivity \( D_{th} \sim 10^{-7} \text{m}^2\text{s}^{-1} \), thermal conduc-

\[ \Delta T \sim 0.5 \text{ Wm}^{-1}\text{K}^{-1} \], we estimate the maximum temperature in the flow by modeling the heating produced by a laser absorbed in a single fluid phase [19], assuming thermal diffusion as the only energy transport mechanism. Considering the measured optical absorption of our water/dye solution \( \alpha_{th} = 117.9 \text{ m}^{-1} \), and assuming that the temperature 100 \( \mu\text{m} \) away is fixed by the flowing oil at room temperature, we find \( \Delta T \approx 12 \text{ K} \) for the temperature rise at the laser focus for a beam power \( P = 100 \text{ mW} \). The temperature gradient is steep near the focus, with the temperature dropping to 5 K at 20 \( \mu\text{m} \) from the beam spot. However, note that given the typical

FIG. 2: (color online) Dependence of the blocking time \( \tau_b \) on laser power and position (indicated in the picture) for \( Q_{\text{water}} = 0.03 \mu\text{L/min} \) and \( Q_{\text{dye}} = 0.1 \mu\text{L/min} \), \( \omega_0 = 2.6 \mu\text{m} \). Inset: Rescaled droplet length \( L / L_0 \) vs. the blocking time (laser position •), where \( L_0 \) is the droplet length without the laser. The dashed line is a linear fit, ignoring the outlier at \( \tau_b = 0.75 \text{ s} \).

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flow velocity \((U \sim 1 \text{ mm/s})\) and the characteristic length scale over which thermal diffusion occurs \((L = 100 \mu \text{m})\), the thermal Peclet number \(Pe = UL/D_{th}\) is comparable to unity. Thus, our calculation overestimates the actual overheating.

The force generated by the convective flow on a droplet is investigated through the depth-averaged Stokes equations, since our channels have a large width/height aspect ratio [20]. The detailed modeling will be discussed in a subsequent publication; here we limit ourselves to the main features: a circular drop of radius \(R\) is considered in an infinite domain and the flow due to the Marangoni stresses is evaluated. Assuming a parabolic profile in the small dimension \((h)\) and introducing a streamfunction for the mean velocities in the plane of the channel, the depth averaged equations, valid in each fluid, are

\[
\left( \frac{1}{r} \frac{\partial}{\partial r} \left( \frac{r}{\partial \psi} \right) \right) + \left( \frac{\partial^2}{\partial \theta^2} \right) \left( \frac{1}{r} \frac{\partial}{\partial r} \frac{r}{\partial \psi} \right) + \left( \frac{\partial^2}{\partial \theta^2} \right) - \frac{12}{\bar{h}^2} \psi = 0, \tag{1}
\]

where the depth-averaged velocities may be retrieved from \(u_\theta = -\partial \psi / \partial r\) and \(u_r = 1/r(\partial \psi / \partial \theta)\). The kinematic boundary conditions at the drop interface \((r = R)\) are zero normal velocity and the continuity of the tangential velocity. The normal dynamic boundary condition is not imposed since the drop is assumed to remain circular, which is consistent with our experimental observations, Fig. 3a. Finally, the tangential dynamic boundary condition, which accounts for the optically-induced Marangoni stress, is

\[
\mu_1 \frac{\partial}{\partial r} \left( \frac{u^1_r}{r} \right) - \mu_2 \frac{\partial}{\partial r} \left( \frac{u^2_r}{r} \right) = -\frac{\gamma'}{r} \frac{dT}{d \theta}, \tag{2}
\]

where \(\mu_{1,2}\) are the dynamic viscosities and \(u^{1,2}_{\theta}\) are the velocities in the drop and the carrier fluid, respectively. \(\gamma' = \partial \gamma / \partial T\) is the surface tension to temperature gradient, which is positive in our case.

For simplicity, we approximate the steady state temperature distribution using a Gaussian form \(T(x, y) = \Delta T \exp[-(x - R)^2 + y^2)/w^2]\), where \(\Delta T\) is the maximum temperature difference between the hot spot and the far field and \(w\) corresponds to the size of the diffused hot spot, which is significantly larger than \(\omega_0\) [19]. The equations are nondimensionalized using \(\Delta T\) as temperature scale, \(R\) as length scale, \(R \gamma' \Delta T\) as force scale and \(\frac{R(\mu_1 + \mu_2)}{\Delta T} \) as time scale, the remaining nondimensional groups being the aspect ratio \(h/R\), the nondimensional hot spot size \(w/R\) and the viscosity ratio \(\bar{\mu} = \mu_2 / (\mu_1 + \mu_2)\).

A typical predicted flow field solving the above numerical formulation is shown in Fig. 3(b), in which the four recirculation regions are clearly visible. The velocity gradients display a separation of scales in the normal and tangential directions, as observed from the distance between the streamlines in the two directions. Indeed, it may be verified that the velocities vary over a typical length scale \(h/R\) in the normal direction, while the tangential length scale is given by \(w/R\).

Along with this flow field, we compute the pressure force, as well as the normal \((\bar{\sigma}_{F\theta} = 2\bar{\mu} \frac{\partial u_\theta}{\partial r})\) and tangential \((\bar{\sigma}_{F\theta} = \bar{\mu} \left( \frac{\partial u_r}{\partial \theta} + \frac{\partial u_\theta}{\partial r} - \frac{u_\theta}{r} \right))\) viscous shear stresses in the external flow. Their projections on the \(x\) axis, shown in the inset of Fig. 3(c), are then summed and integrated along \(\theta\) to yield the total dimensionless force \((\bar{F})\) on the drop. Note that the global \(x\) component of the force is negative and therefore opposes the transport of the drop by the external flow. The \(y\) component vanishes by symmetry and the integral of the wall friction may be shown to be zero since the drop is stationary. Numerically computed values of \(\bar{F}R/h\) are shown by the isolated
points in Fig. 3(c) as a function of $w/R$, for different values of the aspect ratio $h/R$. The points all collapse on a single master curve, displaying a nondimensional scaling law $F \sim wh/R^2$, for small $w/R$.

The dimensional form of the force can be obtained, for small $h/R$ and $w/R$, by considering the three contributions separately and noting that the velocity scale in this problem is imposed by the Marangoni stress. Using the separation of scales along the azimuthal and radial directions, Eq. 2 becomes $(\mu_1 + \mu_2) \frac{U}{h} \sim \frac{\Delta \gamma}{\sigma'} \frac{h}{R}$, where the ‘$\sim$’ is understood as an order-of-magnitude scaling. This yields the characteristic tangential velocity scale

$$U \sim \frac{\Delta \gamma'}{\mu_1 + \mu_2} \frac{h}{w}.$$  
(3)

The force due to the tangential viscous shear is then obtained by multiplying $\sigma \rho_0 \sim \mu_2 U/h$ by $\sin \theta \approx w/R$ and integrating on the portion $w \times h$ of the interface,

$$F_t \sim \mu_2 \frac{U}{h} \frac{w}{R} w h = \frac{\mu_2}{\mu_1 + \mu_2} \frac{\Delta \gamma}{\sigma'} \frac{h w}{R}.$$  
(4)

The force due to the normal viscous shear can be shown to scale like $F_n \sim \frac{\mu_1}{h} F_t$ and is therefore negligible. The pressure force, on the other hand, derives from a balance between the pressure gradient and the radial second derivative of velocity. In the present circular geometry, similar scaling arguments yield a law for the contribution of the pressure force $F_p$, which follows the same scaling as $F_t$, resulting in the same scaling law for the total force $F$. A rigorous derivation (to be published elsewhere) yields the final form of the force including the prefactor:

$$F = -2 \pi \frac{\mu_2}{\mu_1 + \mu_2} \frac{\Delta \gamma}{\sigma'} \frac{h w}{R}.$$  
(5)

This expression is represented (once nondimensionalized) by the straight line on Fig. 3(c) and agrees very well with the numerically computed values.

The physical value of the force for a typical experiment is estimated by taking $\mu_1 = 10^{-3}$ Nm$^{-2}$s (water), $\mu_2 = 3 \mu_1$ (hexadecane), and extracting $\gamma' \sim 1$ mN$^{-1}$K$^{-1}$ from Ref. [17]. This yields a force on the order of 0.1 $\mu$N, which is of the same order as the drag force on a drop in a large aspect ratio channel [21], thus confirming that thermocapillary forcing can indeed account for the blocking. Note that the force we calculate is several orders of magnitude larger those generated from electric fields [22] or optical tweezers [23].

This blocking force may be applied at different locations in a microchannel by displacing the laser spot. In particular, we demonstrate the sorting of drops, a fundamental operation in the implementation of lab-on-a-chip devices. Drops are formed, as above, in a cross-junction continuous phase. In the absence of laser forcing, the drops arriving at the bifurcation divide into two equal parts [5], Fig. 4(a). When the laser is applied, the water-oil interface is asymmetrically blocked on the right hand side while the left hand side continues to flow, Fig. 4(b). Above a critical laser power (approximately 100 mW for the present configuration), the drop is blocked long enough that it is completely diverted through the left hand channel [15]. Drops may therefore be sorted by accordingly selecting the laser position.

In summary, we have experimentally and theoretically demonstrated the efficiency of laser-driven blocking of water-in-oil drops. The theoretical treatment brings out two length scales, $h/R$ and $w/R$. While $h$ and $w$ can be thought of as determining the typical scales for velocity variations in the radial and azimuthal directions, $R$ enters the force scaling as a local radius of curvature rather than the actual size of the drop. It is therefore not surprising that the blocking force should increase as $R$ decreases. On the other hand, the drag force due to the external flow scales as $R^2$ [21], implying that the laser power necessary to counterbalance the drag quickly decreases with the drop size. This, along with the rapidity of viscous and thermal diffusion while thermal inertia is reduced, all lead to laws favorable to miniaturization. The generality of the process provides a practical new way for acting on individual droplets, at any location, while working inside the robust environment of the microchannel.

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[15] See EPAPS Document No. [number will be inserted by publisher] for movie sequences from the experiments. For more information on EPAPS, see http://www.aip.org/pubservs/epaps.html.
[18] A reduction the surfactant concentration reduced the efficiency of the blocking; a detailed exploration of surfactant effects will be addressed in a future study.